

QIBA Profile: Ultrasound Measurement of Shear Wave Speed for Estimation of Liver Fibrosis

Stage: 2. Consensus

15 Table of Contents 1. Executive Summary4 20 2.2 Discussion.......9 25 30 35 40 45 50 55 4.1.1 OBTAINING AND MAINTAINING THE IMAGING PHANTOMS.......26 4.1.2 ASSESSING IMAGING PERFORMANCE.......29 60 4.2.1 SITE ASSESSMENT TOOLS AND TESTS.30

Commented [OK1]: GUIDANCE:

Please do not change the Level 1 headings or numbering. Also, do not make gratuitous changes to fonts, sizes, formatting, numbering etc.

"Safe Pasting" (i.e. always paste Text Only) will avoid cluttering the document with random paragraph styles and anomalous formatting.

Line Numbers are very helpful during group reviews ("There's a word missing in line 169.") but you can turn them off (under Page Layout) if you find them distracting.

Commented [BG2]: Change log to be deleted—may incorporate old version in an appendix if anyone thinks it is useful. It was distracting and wasted reveiwers time reviewing the log and making corrections to that.

	4.2.2 ASSESSING SWS CONSISTENCY COMPARED WITH PHANTOM SPECIFICATIONS	
	TOPIC IN SECTION 3.4.1	34
	4.2.3 INDIVIDUAL ACTOR TOOLS AND TESTS	34
	4.3. Assessment Procedure: SWS Measurement Concordance	<u>35</u> 34
65	5. Conformance	35
	Appendix A: Acknowledgements and Attributions	37
	Appendix B: Background Information	40
	Appendix C: Conventions and Definitions	40
	Appendix D: Model-specific Instructions and Parameters	40
70	D.1 Canon	<u>41</u> 40
	D.2 ESAOTE	
	D.3 General Electric	45
	D.4 Hitachi	46
	D.5 Philips	<u>48</u> 47
75	D.6 Samsung	<u>49</u> 48
	D.7 Siemens	
	D.8 Supersonic Imagine	53
	Appendix E: Primary Checklists for Profile Execution and Conformance	<u>56</u> 55
	Appendix F: Secondary Checklists for Profile Execution and Conformance	
80	Appendix G: Patient information sheet and Data collection	56
	References	59 58

1. Executive Summary

90

105

110

115

120

The goal of a QIBA Profile is to help achieve a useful level of performance for a given biomarker.

Profile development is an evolutionary, phased process; this Profile is in the <u>consensus</u> stage. The performance claims represent expert consensus and will be empirically demonstrated at a subsequent stage. Users of this Profile are encouraged to refer to the following site to understand the document's context: http://qibawiki.rsna.org/index.php/QIBA_Profile_Stages.

The Claim (Section 2) describes the biomarker performance.

The **Activities** (Section 3) contribute to generating the biomarker. Requirements are placed on the **Actors** that participate in those activities as necessary to achieve the Claim.

Assessment Procedures (Section 4) for evaluating specific requirements are defined as needed.

Conformance (Section 5) regroups Section 3 requirements by Actor to conveniently check Conformance.

This QIBA Profile (Ultrasound Measurement of Shear Wave Speed for Estimation of Liver Fibrosis) addresses estimation of liver fibrosis, which is often used to determine when and how to treat patients with diffuse liver disease, and also monitor progression or response to treatment. It places requirements on ultrasound scanners (acquisition devices), Scanner Manufacturer/Vendor, Technologists/Sonographers, QA (Quality Assurance) Manager, Radiologists, and Image Analysis Tools involved in pre-delivery steps, scanner installation, site QA procedures, subject selection and handling, image data acquisition, image and other QA and image analysis. The requirements are focused on achieving sufficient accuracy and avoiding unnecessary variability of the estimation of liver fibrosis. Estimates of liver fibrosis are based on the stiffness of the liver tissue which in turn is based on a measurement of shear wave speed (SWS) in the tissue using ultrasound.

The clinical performance target is to achieve SWS measurements with a bias of the mean value of $\leq 5\%$ and an overall coefficient of variation of 5% (SD/mean). The standard against which to measure bias has not yet been fully defined, so currently there is no bias claim. At the present time, bias is determined by comparison to the measured shear wave speed and stiffness using a Verasonics ultrasound system in a calibrated QIBA SWS phantom. Currently bias and precision vary depending on the magnitude of measured shear wave speed (as determined in phantom studies) so bias and variance claims are given for three ranges of measured shear wave speed values. Also, bias and precision vary depending on the conditions under which the measurements are made. Bias and precision claims are therefore also given for various measurement conditions.

This document is intended to help clinicians basing decisions on this biomarker, imaging staff generating this biomarker, vendor staff developing related products, purchasers of such products and investigators designing trials with imaging endpoints.

Note that this document only states requirements to achieve the claim, not "requirements on standard of care." Conformance to this Profile is secondary to properly caring for the patient.

QIBA Profiles addressing other imaging biomarkers using CT, MRI, PET and Ultrasound can be found at qibawiki.rsna.org.

Commented [OK3]: KOD – based on your claims "The requirements are focused on achieving sufficient accuracy and avoiding unnecessary variability in the measurement of shear wave

The use of SWS to estimate liver fibrosis is what you explain in the Clinical Context and already mentioned in the first sentence in this paragraph.

2. Clinical Context and Claims

Elastography is a technique for measuring tissue stiffness or elasticity. Stiffness or elasticity of all materials including tissue is defined by a parameter known as the elastic (or Young's) modulus typically given in units of pressure (Pascals or kilopascals). The elastic modulus may be measured directly by mechanical testing where pressure is applied to a sample of material and the deformation (loss of height or thickness) is measured. The slope of the plot of thickness change vs. pressure is the elastic modulus. For a given amount of pressure, the change in thickness of the overall block of material, or at any 130 location in the material, is defined as the "strain". Samples of tissue are not usually available for mechanical testing, so elastography was developed as a means to estimate tissue elasticity noninvasively. Tissue elasticity may be calculated in two ways: 1) From an image of the strain of a region of tissue in response to external or internal compression force (known as strain elastography), and 2) by measuring the speed of propagation of a shear wave as it traverses a region of tissue (known as shear wave elastography). For the second technique, the shear wave speed (SWS) may be used as a surrogate for tissue stiffness which serves as a biomarker for level of fibrosis since it has been shown that fibrosis is the major cause of increased liver stiffness.

Clinical Context

125

145

150

160

140 Shear wave speed (SWS) is a biomarker to identify patients with moderate but significant liver fibrosis, defined as ≥ F2 fibrosis in the METAVIR system (or equivalent for other scoring systems) of staging liver fibrosis. This might be used to monitor progression of fibrosis or to monitor regression of fibrosis during anti-fibrosis therapy.

SWS also serves as a biomarker for the evaluation of cirrhosis, defined as F4 stage of fibrosis of the METAVIR system of staging liver fibrosis. As noted in the discussion below, the SWS biomarker may be referred to as the "measurand" elsewhere in this document.

Intended Clinical Application: SWS is measured in the liver of patients with suspected diffuse liver disease, with or without fatty infiltration of the liver and with suspected fibrosis or cirrhosis.

Multiple Claims: Ground work studies conducted by the QIBA SWS Biomarker Committee have indicated that the key measures of biomarker performance, Bias and Precision, depend on the level of fibrosis present and upon other variables such as whether or not the measurements are taken with a single machine at a single site (hospital or clinic) or not. Accordingly, several claims for bias and precision are made depending on the situation and estimated level of fibrosis. Strictly speaking, the claims of the profile only apply to purely elastic materials and phantoms. This is because visco-elastic phantoms are generally not available for sites to verify the profile claims and the committee must further verify the profile claims for a clinically relevant range of visco-elastic materials. Claims for viscoelastic phantoms and tissues will appear in the next version of the profile. The claims are presented below.

In the claims presented below, the term "imaging system" refers to both the ultrasound scanner (machine) and the operator using the machine to perform SWS measurements. Changing either the operator or ultrasound scanner therefore results in a different imaging system.

Conformance to this Profile by all relevant staff and equipment supports the following claim(s):

Claim 1 (technical performance claim): A shear wave speed measurement has a within-

Commented [OK4]: GUIDANCE:

Describe one or more clinical practice utilities or clinical trial endpoints this Profile could serve. E.g.

- · Determining eligibility of subjects in a clinical trial.
- · Triaging eligible subjects into cohorts based on stage or severity of disease.
- Assessing response to treatment
- Establishing the presence of progression of disease.
- Monitoring for adverse events.
- Establishing a database for the development, optimization, and validation of imaging biomarkers.

subject coefficient of variation (wCV) depending on the measured SWS and depth of acquisition according to Table 2-1.

Table 2-1 Coefficient of Variation (wCV)

rubic 2 1 coefficient of variation (wev)		
Measured SWS (m/s)	Depth=4.5cm*	Depth=7.0cm
0.9 < SWS <= 1.2	5%	8%
1.2 < SWS <= 2.2	4%	5%
2.2 < SWS <= 5.0	10%	12%

^{*}For measurements taken at depths other than the two listed, the SWS Committee has determined that linear interpolation of the Coefficients of Variation is appropriate.

Claim 2 (cross-sectional claim): A 95% confidence interval for the true SWS is Y \pm (1.96 \times Y \times wCV/100), where Y is the measured SWS and wCV is the within-subject coefficient of variation from Table 2-1.

Claim 3a (longitudinal claim): A true change in SWS measurements (Y1 and Y2) over two time points has occurred with 95% confidence if the measured % change, defined as $\frac{|Y_2-Y_1|}{(Y_1+Y_2)/2} \times 100$, is equal to or greater than the repeatability coefficient (RC) given in Table 2-2.

Table 2-2 Repeatability Coefficient (RC)

•	•	· •
Measured SWS (m/s)	Depth=4.5cm*	Depth=7.0cm
0.9 < SWS <= 1.2	14%	22%
1.2 < SWS <= 2.2	11%	14%
2.2 < SWS <= 5.0	28%	33%

^{*}For measurements taken at depths other than the two listed, the SWS Committee has determined that linear interpolation of the Repeatability Coefficient is appropriate.

Claim 3b (longitudinal claim): A 95% confidence interval for the true change over two time points (Y1 and Y2) is:

$$(Y_2-Y_1)\pm~1.96\times\sqrt{(Y_1\times wCV/100)^2+(Y_2\times wCV/100)^2}$$
, where wCV is based on Table 2-1.

185 Claims 3a and 3b hold when the same technologist and same ultrasound scanner are used at the two time points.

Claim 4a (longitudinal claim): A true change in SWS measurements (Y1 and Y2) over two time points has occurred with 95% confidence if the measured % change, defined as $\frac{|Y_2-Y_1|}{(Y_1+Y_2)/2} \times 100$, is equal to or greater than the reproducibility coefficient (RDC) given

Commented [OK5]: KOD Technical Issue

Do you want to consider taking the same approach for speed as you took for depth? I.e. making point claims and recommending linear interpolation?

Currently users are told to expect that at SWS 2.2m/s, wCV will be 4%, and at SWS 2.21m/s, it will jump to 10%...

Commented [OK6]: KOD Technical Issue "the interpolated wCV based on Table 2-1"?

Commented [OK7]: Y1 and Y2 are the two measurements (i.e. SWS=Y1), not the two timepoints (i.e. t=Y1)

180

in Table 2-3.

200

205

210

Table 2-3 Reproducibility Coefficient (RDC)

Measured SWS (m/s)	Depth=4.5cm	Depth=7.0cm
0.9 < SWS <= 1.2	19%	25%
1.2 < SWS <= 2.2	14%	17%
2.2 < SWS <= 5.0	33%	39%

^{*}For measurements taken at depths other than the two listed, the SWS Committee has determined that linear interpolation of the Reproducibility Coefficient is appropriate.

Claim 4b (longitudinal claim): A 95% confidence interval for the true change over two time points (Y1 and Y2) is

$$(Y_2 - Y_1) \pm 1.96 \times \sqrt{(Y_1 \times U/100)^2 + (Y_2 \times U/100)^2}$$
, where U is from Table 2-3b.

Table 2-3b Values of U (wCV from different technologist and/or scanner at same site)

Measured SWS (m/s)	Depth=4.5cm	Depth=7.0cm
0.9 < SWS <= 1.2	7%	9%
1.2 < SWS <= 2.2	5%	6%
2.2 < SWS <= 5.0	12%	14%

^{*}For measurements taken at depths other than the two listed, the SWS Committee has determined that linear interpolation of U is appropriate.

Claims 4a and 4b hold when a different technologist and/or a different ultrasound scanner is used at the <u>same site</u> at the two time points.

Claim 5a (longitudinal claim): A true change in SWS measurements (Y1 and Y2) over two time points has occurred with 95% confidence if the measured % change, defined as $\frac{|Y_2-Y_1|}{(Y_1+Y_2)/2} \times 100$, is equal to or greater than the reproducibility coefficient (RDC) given in Table 2-4.

Table 2-4 Reproducibility Coefficient (RDC)

		- \ - /
Measured SWS (m/s)	Depth=4.5cm	Depth=7.0cm
0.9 < SWS <= 1.2	22%	28%
1.2 < SWS <= 2.2	17%	19%
2.2 < SWS <= 5.0	33%	39%

Claim 5b (longitudinal claim): A 95% confidence interval for the true change (in m/sec) over two time points (Y1 and Y2) is

$$(Y_2 - Y_1) \pm \ 1.96 \times \sqrt{(Y_1 \times H/100)^2 + (Y_2 \times H/100)^2}$$
, where H is from Table 2-4b.

Table 2-4b Values of H (wCV from different technologist and/or scanner at different sites)

Measured SWS (m/s)	Depth=4.5cm	Depth=7.0cm
0.9 < SWS <= 1.2	8%	10%
1.2 < SWS <= 2.2	6%	7%
2.2 < SWS <= 5.0	12%	14%

Claims 5a and 5b hold when a different technologist and/or a different ultrasound scanner is used at different sites at the two time points.

The above claims were developed based on phantom studies conducted by the Ultrasound Shear Wave Speed Biomarker Committee and may not accurately reflect performance in patients. The expectation is that during the Claim Confirmation and Clinical Confirmation stages, data on the actual field performance will be collected and changes made to the claims or the details accordingly. At that point, this caveat may be removed or re-stated.

2.1 Clinical Interpretation

215

225

230

235

QIBA Claims describe the technical performance of quantitative measurements. The clinical significance and interpretation of those measurements is left to the clinician. Some considerations are presented in the following text.

Currently the only consensus standard for interpretation in the United States is that formulated by the Society of Radiologists in Ultrasound in October 2014¹. According to that standard, measurements are used to classify a patient into one of the three categories below:

Example Table of Liver Fibrosis Categories and Corresponding Representative Shear Wave Speed Values. *

Ultrasound System	No Fibrosis or Minimal Fibrosis	Moderate Fibrosis	Severe Fibrosis/Cirrhosis
	(METAVIR F0-F1)	(METAVIR F2 i and F3 ii)	(METAVIR F3 – F4)
System A	SWS < 1.37 m/s	1.37 < SWS < 2.2 m/s	SWS > 2.2 m/s
	(< 5.7kPa) [™]	(> 5.7 kPa, < 15 kPa)	(> 15 kPa) iv
System B	SWS < 1.66 m/s	1.66 ≤ SWS < 1.88 m/s	SWS ≥1.88 m/s
	(<8.29 kPa)	(≥8.29 kPa, < 10.60 kPa)	(≥10.60 kPa)

^{*}Considerable changes have been adopted by the clinical community since this table was developed. Some of the changes are described below:

Commented [OK8]: GUIDANCE:

This section should speak to the clinicians and clinical trialists who will apply the profile. This is where you explain how the technical performance in the claims could be applied to interpretation and clinical decision making. In some Profiles this may include pointing to measurement value cut-points that discriminate groups of subjects (e.g. those with vs. without a particular disease, or those at different stages of disease) and providing estimates of the sensitivity and specificity associated with each cut-point. Supporting analysis work should be referenced.

Commented [OK9]: KOD Editorial Issue Did you want to include the article title in the reference below?

Metavir F2 currently is often classified as "significant fibrosis" and is no longer grouped with F3.

ii. F3 is no longer classified as moderate cirrhosis but instead both F3 and F4 are classified as "Compensated advanced chronic liver disease" for clinical management.

iii. After acquisition of additional data with newer software, the values for this system have been revised upward. Currently the cutoff value for F2 is approximately 7kPa for both ARFI systems such as this one and Fibroscan.

iv. This value is high for the F4 cutoff and carries a significant risk of misclassification of F4 patients as F3. This value was used as it was associated with a nearly 100% specificity which was considered desirable by the consensus panel. It may be revised in the next

¹ Richard G. Barr, Giovanna Ferraioli, Mark L. Palmeri, Zachary D. Goodman, Guadalupe Garcia-Tsao, Jonathan Rubin, Brian Garra, Robert P. Myers, Stephanie R. Wilson, Deborah Rubens, and Deborah Levine. Radiology 2015 276:3, 845-861

consensus panel statement.

240

250

255

260

265

270

275

Further guidance regarding interpretation of shear wave speed values for chronic diffuse liver disease may be found in the updated guidelines for liver ultrasound elastography published in September 2018 by the World Federation of Ultrasound in Medicine and Biology²

245 For cutoff values for some specific ultrasound systems, please refer to the Manufacturer Specific Protocols in Appendix D.

Tests (see References (Inflammation affects SWS)) have shown that active inflammation in the liver affects SWS measurements. When a patient has severe acute/chronic active hepatitis (including short-term flare-ups), SWS may OVERESTIMATE the degree of fibrosis (increased positive bias). Similarly, SWS may OVERESTIMATE the degree of fibrosis in conditions that cause congestion of the liver, such as congestive heart failure, renal failure with volume overload, etc.

Clinical interpretation with respect to progression or response:

For measurements at multiple points in time, a patient may be reclassified clinically if the newer measurement falls into a different clinical category AND if the difference between the new measurement and prior measurement are statistically different from one another.

2.2 Discussion

Groundwork studies conducted by the QIBA SWS Biomarker Committee have indicated that the key measures of biomarker performance, Bias and Precision, depend on the level of fibrosis present and upon other variables such as whether or not the measurements are taken by a single technologist with a single machine at a single site (hospital or clinic). Accordingly, several claims for bias and precision are made dependent on the use of the same or different technologist and scanner, and on the measured shear wave speed.

In shear wave elastography (SWE), the biomarker is, as noted above, shear wave speed (SWS) which is the speed of a shear wave generated in a patient's liver by an acoustic radiation force impulse (ARFI) push. Another device measuring propagation of shear waves using ultrasound is the non-imaging FibroScan® device which applies force by means of a mechanical piston pressing against the skin. Measurement using the FibroScan® device is not covered by this profile. A table for comparing FibroScan® and magnetic resonance elastography (MRE) values with ARFI SWS values obtained according to this profile will be listed at the end of this section when validated comparisons become available. The SWS biomarker is used for measurement at a single point in time intended to classify liver tissue according to fibrosis grade and also for monitoring shear wave speed (and corresponding fibrosis) changes over time.

Claim 1 describes the expected variability in terms of the coefficient of variation (%wCV) of measurements made at approximately the same time in the same patient and acquisition depth for several depths and for several ranges of SWS. These two variables (depth and SWS range) have been determined by the committee to have significant effects on technical performance but which can be

Commented [OK10]: GUIDANCE:

It is important to explain the assumptions underlying the Claims and the basis for relevant estimations.

² Ferraioli, Giovanna & Wong, Vincent & Castera, Laurent & Berzigotti, Annalisa & Sporea, Ioan & Dietrich, Christoph & Choi, Byung Ihn & Wilson, Stephanie & Kudo, Masatoshi & Barr, Richard. (2018). Liver Ultrasound Elastography: An Update to the World Federation for Ultrasound in Medicine and Biology Guidelines and Recommendations. Ultrasound in Medicine & Biology. 10.1016/j.ultrasmedbio.2018.07.008.

controlled for by acquisition technique and data analysis. The claim is based on results from a phantom study, where 10 repeat measurements were performed at each focus, within a phantom at each site.

Claim 2 is a cross-sectional claim describing the 95% confidence interval of the true SWS measurement for several depths and for several ranges of SWS. These two variables (depth and SWS range) have been determined by the committee to have significant effects on technical performance but which can be controlled for by acquisition technique and data analysis. The claim is based on two results from the phantom study: first, that the within-subject CV is as described in Claim 1; second, that the bias is negligible for most systems.

Claims 3a and 3b describe the confidence interval for differences between two measurements of SWS made on the same patient at different points in time when the same operator makes the measurement on the same scanner using the technique described in this profile. These claims make the following assumptions:

a. SWS measurements have the property of linearity

280

285

290

295

300

b. The slope of a line between the SWS measurements and the true value is 1.0.

Claims 4a and 4b describe the confidence interval for differences between two measurements of SWS made on the same patient at different points in time when a different operator and/or a different scanner <u>at the same imaging site</u> is used to make the measurements using the technique described in this profile. These claims make the following assumptions:

- a. SWS measurements have the property of linearity
- b. The slope of a line between the SWS measurements and the true value is 1.0.

Claims 5a and 5b describe the confidence interval for differences between two measurements of SWS made on the same patient at different points in time when a different operator and/or a different scanner <u>at a different imaging site</u> is used to make the measurements using the technique described in this profile. These claims make the following assumptions:

- a. SWS measurements have the property of linearity
- b. The slope of a line between the SWS measurements and the true value is 1.0.

Commented [OK11]: Minor point:

It feels like these two bullets could be stated a little more precisely. If linearity is a property of a relationship, then it's the relationship of an SWS measurement to the corresponding true SWS value that is linear and is assumed to have a slope of 1.0.

3. Profile Activities

305

The Profile is documented in terms of "Actors" performing "Activities". Equipment, software, staff or sites may claim conformance to this Profile as one or more of the "Actors" in the following table.

Conformant Actors shall support the listed Activities by conforming to all requirements in the referenced Section.

Table 1: Actors and Required Activities

Table 1: Actors and Required Activities		
Actor	Activity	Section
Ultrasound Scanner		
		3.
		3.
	Periodic QA	3.5.
Technologist/Sonographer	Subject/Patient Selection & Handling	3.8.
	Image Data Acquisition	3.9.
	Image QA	3.11.
	Staff Qualification	3.1.
Radiologist	Subject Selection	3.7.
	Subject Handling	3.8.
	Image QA	3.11.
	Image Analysis	3.10
QA Manager	Periodic QA	3.5.
	Site Conformance	3.0.
	Installation	3.4.
Image Analysis Tool	Image Analysis	3.10.
Manufacturer	Pre-delivery	3.3
	Installation	3.4

Commented [OK12]: GUIDANCE:

Inside each Activity section is a subsection for Specification which contains the requirements table. If it is necessary to explain the rationale or meaning of any of the parameters or requirements, that goes in the subsection for Discussion.

This keeps the requirements concise and allows implementers to jump straight to the meat, but still allows for relevant background. Keep the discussion $\underline{\text{brief}}$ though.

To help readers, at the beginning of a discussion paragraph (if possible as the first words) name the associated parameter and bold it, and sequence the discussion paragraphs in the same order as the specification table.

Commented [OK13]: KOD Editorial

In a variety of places below, the term "Operator" is used, presumably to refer to the person operating the scanner during the acquisition/measurement process and not caring whether that is a Technologist or Radiologist.

Suggest using that term instead of Technologist/Sonographer. It would make the requirements in 3.9 clearer to just be Operator. Radiologist would still be an actor with their non-operator requirements.

The requirements in this Profile do not codify a Standard of Care; they only provide guidance intended to achieve the stated Claim. Failing to conform to a "shall" in this Profile is a protocol deviation. Although deviations invalidate the Profile Claim, such deviations may be reasonable and unavoidable and the radiologist or supervising physician is expected to do so when required by the best interest of the patient or research subject. How study sponsors and others decide to handle deviations for their own purposes is entirely up to them.

A detailed sequencing of all of the Activities specified in this Profile is given in the excel spreadsheet in Appendix E in a format that can be reproduced for use on site during the generation of the biomarker.

3.0. Site Conformance Check

This activity involves establishing the overall conformance of an imaging site to this Profile. It includes criteria to confirm the conformance of each of the participating Actors at the site.

3.0.1 DISCUSSION

A site conforms to the Profile if each relevant actor conforms to each requirement assigned in the Activities of the Profile.

The requirements in section 3.0.2 are basically that a site-designated QA Manager confirm all the relevant Actors at the site have conformed to the Profile.

For a discussion of Conformance, see Section 5.

315

320

325

330

3.0.2 SPECIFICATION

Parameter	Actor	Specification
Ultrasound Scanner	I()Δ Manager	Shall confirm all participating ultrasound scanners conform to this Profile.
Technologist/Sonographer		Shall confirm that each participating technologist/sonographer conforms to this Profile with respect to training, documented acquisition performance and proper conduct of SWS acquisitions.
Radiologists		Shall confirm all participating radiologists conform to this Profile in terms of patient interaction, acquisition performance (if performing acquisitions), and reporting.
Image Analysis Tool	_	Shall confirm all participating image analysis tools conform to this Profile.

Commented [OK14]: GUIDANCE:

Various activity sections have been included to give a sense of where certain details might go and what the activities might be called. Over time QIBA may include more example text in each.

It is hoped this will facilitate some convergence in style, content and naming between profiles which will reduce learning curves of adopters and allow biomarker committees to steal benefit from each other's Profile work.

Feel free to delete sections that are not relevant for your biomarker or to populate them with null text such as "This activity is not a source of significant variance for this biomarker" or "No specific pre-delivery activities are required by this Profile".

The null text approach may be useful during early phases of Profile development because it keeps people thinking about it and you may change your mind later.

You can also merge multiple activities into a single activity if it is unreasonable that they would be performed on different equipment or by different people for a given subject.

Keeping the activities in roughly chronological order is probably

Commented [OK15]: MOVED

Much of the following material has been woven into the text in section 5. Duplicate text was not re-duplicated below. The "part way to conformance" material was left out for now.

Commented [OK16]: As we discussed on the phone, since this could/would invalidate the claims we'll hold off on it for now.

Commented [OK17]: GUIDANCE:

Inside each Activity section is a subsection for Specification which contains the checklist table of requirements. If it is necessary to explain the rationale or meaning of any of the parameters or requirements or how a requirement impacts the claim, that goes in the subsection for Discussion.

This keeps the requirements concise and allows implementers to jump straight to the meat, but still allows for relevant background. Keep the discussion brief though.

To help readers, at the beginning of a discussion paragraph (if possible as the first words) name the associated parameter and bold it, and sequence the discussion paragraphs in the same order as the specification table.

Remember: Normative material ("shall") goes in the Specification. Informative material goes in the Discussion.

Discussion might include the rationale for the value chosen in the specification section, or describe how going beyond the specified value might further improve performance, or elaborating on

tradeoffs/interactions between parameters

3.1. Staff Qualification

335

340

345

355

This activity involves evaluating the human Actors (Radiologist, Physicist, and Technologist) prior to their participation in the Profile. It includes training, qualification or performance assessments that are necessary to reliably meet the Profile Claim.

3.1.1 DISCUSSION

These requirements, as with any QIBA Profile requirements, are focused on achieving the Profile Claim. Evaluating the medical or professional qualifications of participating actors is beyond the scope of this profile.

3.1.2 SPECIFICATION

Parameter	Actor	Specification
Operator Training	Technologist/Radiologist	Shall be trained and approved for SWS acquisition
Operator Qualification	Technologist/Radiologist	Shall meet performance requirements on phantoms & subjects: phantom testing— wCV ≤ .05 and/or case review IQR/median ≤ 0.30 for measurements of stiffness in KPa (0.15 for measurements in m/s).

Operator qualification testing. After performing approximately 20 supervised SWS acquisitions on patients and 10 on phantoms, the operator's results in terms of wCV or IQR/median are reviewed. If 90% are within the specification above then the operator is qualified to perform the SWS measurements from a technique standpoint. Additional evaluation parameters such as patient-operator interactions, labeling etc. will be assessed in the usual manner for clinical personnel.

3.2. Product Validation

This activity involves evaluating the product Actors (Acquisition Device and Image Analysis Tool) prior to their use in the Profile (e.g. at the factory). It includes validations and performance assessments that are necessary to reliably meet the Profile Claim.

For ultrasound scanners, each system has unique software and means of display plus validation methods internal to the Manufacturer. For this reason, no requirements regarding product validation are provided here. Manufacturer performance testing is covered in the pre-delivery section.

Commented [BG18]: This section copied from the post public comment version section 3.3

Commented [BG19]: Added radiologist in case the rad performs the acquisitions at a site

Commented [BG20]: Correction per David Fetzer added. Also noted in change log

Commented [KA21]: David Fetzer, MD: "How was 20 chosen? What if a site has either a large number of sonographers or a small number of elastography requests that would make this requirement impractical. Also, what if a site is unable to obtain an elastic phantom?"

Commented [BG22R21]: NANCY OBUCHOWSKI: I THINK THIS NUMBER WAS CHOSEN IN A SOMEWHAT ARBITRARY FASHION BUT PARTLY BECAUSE OF CENTRAL LIMIT THEOREM CONSIDERATIONS. DO YOU WISH TO COMMENT ON THIS? COMMITTEE: I PLAN TO STATE THAT MANUFACTURERS PHANTOMS ARE WIDEL AVAILABLE AND ARE PURELY ELASTIC UNLESS OTHERWISE SPECIFIED AND THAT AVAILABILITY OF PHANTOMS WAS ONE REASON FOR LIMITING THIS VERSION OF THE PROFILE TO ELASTIC MATERIALS.

Commented [BG23R21]: Email sent to Nancy to discuss.

Commented [BG24R21]: Reply to questions to place in spreadsheet

How was 20 chosen? THIS NUMBER WAS CHOSEN IN A SOMEWHAT ARBITRARY FASHION BUT PARTLY BECAUSE OF CENTRAL LIMIT THEOREM CONSIDERATIONS. It is not based on a statistical argument but rather expert consensus. In section 4 when dealing with conformance, the N chosen has a statistical justification. "With 6 subjects and 10 replicates per subject per depth, and with claims stating wCV of 4% and 5% for depths of 4.5 and 7.0 for moderate SWS values, the maximum allowed wCVs are 3.3 and 4.1 for depths of 4.5 and 7.0, respectively."

What if a site has either a large number of sonographers or a small number of elastography requests? In those cases a subset of sonographers can be qualified rather than all of them. In fact not all sonographers will be qualified even after training. These criteria are meant to establish who should be doing the measurements. Gradually over time more sonographers will accumulate enough cases to establish whether they are qualified or not.

What if a site is unable to obtain an elastic phantom? Appropriate phantoms will be available from CIRS initially at reasonable cost so this should not be an issue. Alternatively a small clinic may borrow a phantom from a clinic who has one already.

3.3. Pre-delivery

This activity involves calibrations, phantom imaging, performance assessments or validations prior to delivery of equipment to a site (e.g. performed at the factory by the scanner manufacturer) that are necessary to reliably meet the Profile Claim.

3.3.1 DISCUSSION

3.3.2 SPECIFICATION

Parameter	Actor	Requirement
Acoustic Output (SWS Mode)	Manufacturer	Shall confirm the Ultrasound Scanner, when operating in SWS mode, is within FDA recommended maximum acoustic output levels for diagnostic ultrasound devices. MANUFACTURER specification and certification.
Acoustic Transmit Focusing	Manufacturer	MANUFACTURER specification and certification for SWS measurement and Imaging.
SWS Measurement Consistency	Manufacturer	Shall confirm that the SWS Measurement Consistency of the Ultrasound Scanner is within ± 5%. See 4.2 Assessment Procedure: SWS Measurement Consistency.
US Imaging Performance	Manufacturer	Shall confirm the scanner passes grayscale imaging tests and meets MANUFACTURER Specifications as published in scanner documentation. See 4.1 Assessment Procedure: Imaging Performance
SWS Imaging Performance	Manufacturer	Identification and display meets MANUFACTURER specifications as specified in Manufacturer section (Appendix D)
Software verification	Manufacturer	Shall confirm the software version equals version specified in QIBA profile (Manufacturer specific section – Appendix D).
Hardware and transducer Manufacturer specified parameters	Manufacturer	Shall ensure the equipment intended for use is listed in Appendix D as a compliant combination of System, Software Revision and Transducer.

Commented [KA25]: Milkowski (Siemens) "Clarify that Manufacturer needs to perform this testing and document"

Commented [BG26R25]: Clarifying sentence added

Commented [OK27R25]: Moved clarifying phrase into the corresponding spot in the preceding sentence for brevity. Added requirement to document in the assessment procedure.

Commented [OK28]: MOVED This assessment procedure material was moved to 4.1.1

Commented [KA29]: Aapm:
"Are the MANUFACTURER specifications and certification available to the user? Only available upon request?"

Commented [BG30R29]: MANUFACTURERS: IS THIS INFORMATION AVAILABLE IN THE FDA REQUIRED LABELING? OR ONLY ON REQUEST?

Commented [BG31R29]: Committee: variable based on Manufacturer. Will appear in the manual. Use may consult the manual.

Commented [BG32R29]: Added a footnote containing this information

Commented [OK33]: Since the procedure is for determining the SWS Measurement Consistency, we should make the procedure name match.

3.4. Installation

360

This activity describes calibrations, phantom imaging, performance assessments or validations following installation of equipment at the site that are necessary to reliably meet the Profile Claim.

3.4.1 DISCUSSION

The QA Manager is responsible for several of these requirements being met. The QA Manager may delegate actual performance of certain steps, e.g. to a scanner vendor engineer, and confirm the results.

375

380

370

The testing procedure in section 4.3 compares the SWS measured by the scanner in a phantom to the calibration values obtained by using the Verasonics system. These results **do not yet represent a formal claim for the profile** but could become one in a future edition. If the scanner does not meet the specifications in the table below (table 3.4.2), then the scanner may still be used, but the Manufacturer should be contacted about the discrepancy to determine possible causes. For example, the acquisition procedure provided by the Manufacturer in Appendix D may be incomplete or the site may not be following the procedure as intended by the Manufacturer. The site should record and report a discrepancy found here with their results reporting until the issue is resolved (in conjunction with the Manufacturer).

385

390

3.4.2 SPECIFICATION

Parameter	Actor	Requirement
Laraware	Manufacturer	No physical damage.
	Clinical Staff	No physical damage.
Software verification		Shall confirm the software version equals the version specified in the products QIBA Conformance Statement or one listed in Appendix D.
SWS Measurement Concordance		Shall confirm that SWS Measurement Concordance is within ± 5%. See 4.3 Assessment Procedure: SWS Measurement Concordance

****************************** stop here final acceptance of KOD final edits 1-20-21 23:49 ******

3.5. Periodic QA

This activity describes calibrations, phantom maging, performance assessments or validations performed periodically at the site, but not directly associated with a specific subject, that are necessary to reliably meet the Profile Claim.

3.5.1 DISCUSSION

Test Phantoms for Ultrasonic Imaging and SWS should meet the phantom requirements given in section 3.1 above.

Commented [OK34]: MOVED

Moved procedure details to section 4.3

Commented [OK35]: Seems like it would be cleaner to assign this to the QA Manager rather than add a new Clinical Staff actor to the profile.

Commented [OK36]: MOVED the details into the procedure

Commented [BG37]: Stop here 1-20-21 23:49 final acceptance of KOD edits

Commented [OK38]: GUIDANCE:

Some assessment procedures use a database of control patient data instead of a phantom. Others might scan a "normal control" person rather than a phantom (e.g. there is no phantom for fMRI BOLD). Reconstruction or processing algorithms might be assessed with a virtual phantom to have known ground truth.

The QA Manager is shown as being responsible for much of the phantom-based testing. The QA Manager may delegate actual performance of certain steps to a selected Technologist and confirm the results.

3.5.2 SPECIFICATION

400

Parameter	Actor	Requirement
US Imaging QA	QA Manager	Shall perform standard ultrasound system QA on the Ultrasound Scanner as specified by AIUM guidelines.
SWS Measurement Consistency & System QA Testing Using SWS Phantom	QA Manager	Shall confirm that measurements of SWS on a QIBA elastic phantom using standard instrument settings and acquisition procedures annually, and after any software change are within ± 5% of the values of the Elastic SWS phantom specifications as determined by testing with a Verasonics system. If the system is already known to give results more than 5% different from the phantom values, the system should give values within ± 5% of the previously obtained results. See Measurement Concordance Test Procedure in section 3.4.1 above.
	Ultrasound Scanner	Shall be capable of performing SWS measurements at reproducible instrument settings using manufacture specific standard procedures [appendix D].
Operator training and qualification testing	QA Manager	The operator is trained on patient workflow and SWS acquisition then evaluated to confirm that qualification criteria are met (the requirements are in 3.1 Staff Qualification)
US Imaging and SWS Phantom Characterization and Stability Testing	Operator/QA Manager and/or Independent Phantom QA Site	Confirmation of SWS Phantom Acoustic and Mechanical Properties at Independent Test Site Using QIBA procedures after construction and if a weight change of >0.5% has occurred.

3.6. Protocol Design

405

410

This activity involves designing acquisition protocols for use in the Profile. It includes constraints on protocol acquisition parameters that are necessary to reliably meet the Profile Claim.

Modern Ultrasound scanners use fully automated internal protocols for SWS acquisition with little or no user modification capability. The parameters that may be adjusted are those used during the acquisition process. Those are described in the acquisition sections along with the general principles underlying the acquisition procedure. Because each scanner has its own internal acquisition design, custom acquisition procedures are often needed. These are placed in Appendix D and are to be used in place of the more general procedures in the profile whenever possible.

3.7. Subject Selection

Commented [OK39]: Not sure who, or how many, actors are here. Per guideline #6, it should be one.

http://gibawiki.rsna.org/index.php/How_to_Write_a_Profile#Follow

http://qibawiki.rsna.org/index.php/How to Write a Profile#Follo w Profile Writing Guidance

This activity describes criteria and procedures related to the selection of appropriate imaging subjects that are necessary to reliably meet the Profile Claim.

415 <u>3.7.1 DISCUSSION</u>

The profile is intended to be used in patients who require clinical assessment of liver fibrosis. The following factors affect patient selection.

Body Wall Thickness (and Measurement Depth)

Incorrect placement of the measurement region of Interest (ROI) can prevent effective measurement of SWS. Placement of the ROI too close to the liver capsule may result in artificially elevated SWS values as the liver is naturally somewhat stiffer near the capsule. Placement of the ROI too deep will result in noisy estimates due to attenuation of the acoustic radiation force push pulse and resulting weak, hard to measure shear waves. This can cause increased measurement error and increased numbers of technical failures. Therefore, the region being measured should be a minimum of 2cm deep to the liver capsule and a maximum of 6.5 cm deep to the skin. This means placing the upper edge of the ROI boundary at 2cm depth or greater and placing the lower (deeper) edge of the ROI at or less than 6.5cm depth.

Because of measurement depth requirements, such as those discussed in 3.9.1, if the body wall thickness is greater than 4cm correct depth placement of the acquisition region of interest will not be possible and the measurement may not meet the claims of the profile.

430 Intercostal Space (and COPD)

A narrow intercostal space and/or COPD may make SWS data acquisition more difficult.

If an intercostal approach is not feasible, consider a subcostal approach. However, a note to document this should be made in the patient/subject note or study report. The claims in this profile have not been validated for a subcostal approach but maybe validated in a later version of the profile. Consider MRE as an alternative.

Prior Surgery

435

can interfere with SWS data acquisition. If subjects have had a surgical resection of the all or portions of right lobe of the liver that prevents an intercostal measurement in the right liver lobe, then the patient should be considered for exclusion. Consider MRE as an alternative. The claims in this profile have not been validated for measurements other than the right lobe of the liver, but may be validated in later versions of the profile.

Informed Consent:

Obtain informed consent as needed per institutional policy. HIPAA authorization shall be obtained for research or other purposes as outlined in institutional policies.

445 3.7.2 SPECIFICATION

Parameter	Actor	Requirement	
Clinical Indication	Ordering	Shall assess liver stiffness for liver pathology that may lead to	
	Physician or	increased organ stiffness and increased shear wave speed (for	
	Radiologist	example liver fibrosis). A valid research protocol or a clinical concern	

Commented [OK40]: Modified titles to match parameters they discuss in the table below.

Commented [KA41]: AAPM:

Canon (page 48).'

">=2cm distance from the liver capsule seems to be different compared to most existing literatures which state ~1.5-2cm. Are there any data to support this decision? In addition, how to handle the inconsistency with the vendor recommendations? For example, >=1cm from

Commented [BG42R41]: The SWS committee believes that 2cm is safer from a reproducibility standpoint than 1.5cm and still falls within the literature specifications. This section is a discussion to explain how body wall thickness may affect patient selection. For actual acquisition, the profile specifies that the Manufacturer recommendations should be followed.

Commented [KA43]: AAPM:

"Is the maximum 6.5cm recommendation corresponding to the lower edge of the acquisition ROI? What about patients with ascites? Because of the lower attenuation, many of these cases appear to have sufficient signal at 6.5cm or slightly deeper, even though they are more susceptible to motion artifacts."

Commented [BG44R43]: We should clarify whether the upper margin center or lower margin of the ROI is used to determine ROI depth

Should we address exceptions to the 6.5cm maxiumum?

 $\begin{tabular}{ll} \textbf{Commented [BG45R43]:} Committee agrees: upper edge for 2cm and lower edge for 6.5 cm \end{tabular}$

 $\mbox{Add:}\\mbox{and}\ \mbox{measurement}$ not valid (place after the phrase "not be possible"

Explain that >6.5cm has not been tested and will not meet claim requirements.

Commented [BG46R43]: ANSWER TO PLACE IN THE SPREADSHEET

The 6.5cm maximum refers to placement of the lower (deeper) edge of the ROI. The 2cm minimum depth refers to placement of the upper edge of the ROI. This has been clarified in the profile. Depths greater than 6.5cm have not been tested by the committee, so we cannot guarantee that the claims will be met. This issue will be re-examined for the next version of the profile. We have also added a phrase pointing out the consequences of not placing the ROI deeper than 2cm from the liver capsule in a patient with a body wall thickness of >4cm.

Commented [OK47]: KOD Editorial

This mostly duplicates the material in 3.9.1 on ROI Placement. Consider deleting this text here and just referencing 3.9.1 as shown.

Formatted: Indent: Left: 0", Space After: 8 pt, Add space between paragraphs of the same style

Commented [KA48]: David Fetzer, MD: "For an FDA-approved clinical technique, why would informed consent be needed?"

Commented [BG49R48]: ANSWER TO PLACE IN THE SPREADSHEET: The FDA by law does not regulate clinical techniques as these are considered to be the practice of medicine. The assumption is that medical boards and medical societies will regulate the practice of medicine. For research protocols IRB approval will likely require a consent. Most institutions have requirements for consent that must be followed if a procedure is

Commented [OK50]: Consider removing unless you want to add another actor to the profile.

Parameter	Actor	Requirement
		supported by the literature is needed.
Approach	Radiologist or Operator	Shall confirm an intercostal approach is feasible.
Body Wall Thickness	Radiologist or Operator	Shall confirm the patient body wall thickness is 4cm or less.
Intercostal space	Radiologist or Operator	Shall confirm a sufficiently wide intercostal space for probe placement.
Breathing	Radiologist or Operator	Shall confirm the ability of the patient to follow the breath hold instructions.
Prior Surgery	Radiologist or Operator	Shall confirm the presence of the right lobe of the liver and the absence of surgical/other scars that could cause shadowing.
Informed Consent	Technologist or Radiologist	Informed consent obtained.

3.8. Subject Handling

This activity describes details of handling imaging subjects that are necessary to reliably meet the Profile Claim.

3.8.1 DISCUSSION

Subject handling for quantitative SWS measurement with ultrasound focuses on proper preparation of the patient for the acquisition of high reliability data.

An information/instruction sheet supplied to the patient prior to acquisition may be very helpful. The sheet could describe the technology, explain why it is useful, and give instructions to the patient on how to fast prior to the procedure (see Fasting State in 3.8.2). It may also provide information on maneuvers such as breath holding that will occur during the procedure. An example patient information sheet is given in Appendix G.

In some cases (for example elastography research), an informed consent may be needed.

3.8.2 SPECIFICATION

Parameter Actor Specification		Specification
Patient Instructions	Technologist	Shall instruct the patient ahead of the procedure to fast (avoid food or beverage other than occasional small sips of water) for a minimum of 4 hours prior to the procedure. The instruction may be in the form of a patient information sheet describing how to accomplish the fasting and how it is important for obtaining good SWS results as well as exceptions (e.g. oral medications, insulin).

Commented [OK51]: KOD Editorial Issue "Consent" is scattered in a few different places.

Per Profile Writing Guideline #8, it should actually be removed since

it doesn't impact the SWS variability. http://qibawiki.rsna.org/index.php/How to Write a Profile

Commented [OK52]: GUIDANCE:

This may include

- Timing Relative To Index Intervention Activity
- Timing Relative To Confounding Activities
- Contrast Preparation And Administration
- Subject Positioning
- Instructions to Subject During Acquisition
- Timing/Triggers

Alternatively, some of these topics may be elevated to activities in their own right. $% \label{eq:controller}$

This can include relative timings between scans or details related to the interaction of contrast media or tracers from a prior scan with the following scan.

On the other hand, issues related to running two sequences/series would generally be handled inside the acquisition activity rather than here.

Commented [KA53]: David Fetzer, MD: "Would it be prudent for an actor to verify other potential confounders such as presence of markedly elevated AST/ALT, evidence of biliary obstruction, and evidence of right heart failure/passive hepatic congestion?"

Commented [BG54R53]: I propose the following response. The goal of the profile is to provide a means by which accurate SWS measurements may be made. The confounders mentioned affect SWS and must be considered when using SWS clinically as a surrogate for liver fibrosis. The clinical use and interpretation of the SWS measurements is constantly changing and is beyond the scope of this profile.

Commented [BG55R53]: INCLUDE THE ABOVE EXPLANATION IN THE SPREADSHEET

Commented [OK56R53]: For what it's worth, the above makes sense and is in alignment with QIBA Profiling practices. Good answer.

450

455

Parameter	Actor	Specification	
Fasting State ⁱ	Technologist	Shall query the patient prior to acquisition on whether they actually fasted or not. Offer to acquire the data on a later date or later in the day if the patient is not in a fasting state.	
	Radiologist	Shall query the patient prior to acquisition on whether they actually fasted. Offer to acquire the data on a later date or later in the day if the patient did not fast.	
Informed Consent	Technologist or Radiologist Shall confirm presence of informed consent if needed institutional policy. Shall obtain HIPAA authorization for research or othe purposes, as outlined in institutional policies. (Sample consent form language in Appendix G)		
Patient Information	Technologist or Radiologist	acquisitions, transducer application between ribs, amou	

3.9. SWS Image Acquisition (SWEI) and Point SWS Measurement

This section describes details of the data acquisition process that are necessary to reliably meet the Profile Claim. It includes calibrations, performance assessments or validations during acquisition that are necessary to reliably meet the Profile Claim.

3.9.1 DISCUSSION

465

480

SWS Acquisition System. Even though efforts have been made to reduce variation in SWS measurements by different ultrasound systems, such variation still exists and it may be significantly higher when acquisitions are performed in patients vs. phantoms. For this reason, every effort should be made to acquire successive SWS measurements with the same system or with a system from the same Manufacturer. This guideline cannot be followed in many clinics with systems from multiple Manufacturers because it results in scheduling difficulties. In cases where more than one system is used on a given patient on different exam dates, then the system should be identified and the median values the system gave using the calibration phantom should be given to aid the reader in determining if a difference in median/mean value between two systems should be taken into account during interpretation of the results.

Patient position. For SWS acquisition this varies somewhat between institutions. Supine or slight (<30°) left decubitus positions are thought to be similar enough³ so as not to induce variation in liver stiffness

Commented [OK57]: Matching discussion headings to corresponding parameter below.

Commented [KA58]: AAPM:

"The efficacy of phantom calibration may depend on whether the phantom is viscoelastic or elastic. Elastic phantom may not be able to provide a good calibration among different persons for initial liver."

different scanners for in vivo liver measurements. Some comments about phantom properties may be

Commented [BG59R58]: COMMITTEE: I HAVE NOTED THAT WHILE WE MAKE FREQUENT REFERENCE TO ELASTIC PHANTOMS WE NEVER STATE THAT THE CURRENT PROFILE IS BASED ON ELASTIC PHANTOM RESULTS AND DOES NOT CURRENTLY ADDRESS THE ISSUE OF FREQUENCY DEPENDENCE OF SHEAR WAVE SPEED IN VISCO-ELASTIC MATERIALS. SHOULD WE STATE THAT IN THE INTRODUCTION—EXECUTIVE SUMMARY? IN BOLD LETTERS?

Commented [BG60R58]: Committee suggestion: add elastic vs visco statement line 184 above

Commented [BG61R58]: Statement was added at line 191 and reads as follows: "Strictly speaking, the claims in this version of the profile only apply to purely elastic materials and phantoms. This is because visco-elastic phantoms are generally not available for sites to verify the profile claims and the committee must further verify the profile claims for a clinically relevant range of visco-elastic materials. Claims for visco-elastic phantoms and tissues will appear in the next version of the profile."

Commented [BG62R58]: Answer for spreadsheet: The current profile is based on our experiments with elastic phantoms only, but our data from viscoelastic phantoms seem to indicate that the claims will be similar for visco-elastic phantoms and tissues. A statement clarifying why this version of the profile is based on elastic phantoms only has been added to the end of the executive summary at the beginning of the profile. The statement reads: "Strictly speaking, the claims in this version of the profile only apply to purely elastic materials and phantoms. This is because viscoelastic phantoms are generally not available for sites to verify the profile claims and the committee must further verify the profile claims for a clinically relevant range of visco-elastic materials. Claims for visco-elastic phantoms and tissues will appear in the next version of the profile."

³ Barr et.al. Elastography assessment of Liver Fibrosis: SRU Consensus Conference Statement. Radiology 2015; 276(3): 845-

even though there is evidence that full left lateral decubitus positioning significantly affects measured SWS.

Respiration. Suspended tidal respiration is recommended to avoid additional pressure on the liver that might increase liver stiffness. In addition, this form of suspended respiration may result in less movement of the liver during acquisition since the diaphragm may move less than during a deep inspiration.

Instruction on how the patient should suspend respiration should be given immediately prior to data acquisition. Practice runs should be performed to allow the patient to learn how to suspend respiration. This will provide the patient or subject with useful information on what the ultrasound probe feels like and how long they will be asked to hold their breath.

Transducer Position. Intercostal transducer positioning has been shown to reduce variability in measurements. However, there are situations where intercostal acquisition is not feasible. For example, smaller patients may not have wide enough intercostal spaces to allow intercostal positioning of the transducer without partial blockage of transducer elements resulting either in obvious shadowing or loss of transmit power on the shear wave push pulse. Either will likely result in poor quality shear wave speed estimates. Another problem arises when the subject has COPD and the hyper-expanded lung pushes the liver below the costal margin. Consider subcostal only if intercostal is not feasible. The claims in this profile have not been validated for a subcostal approach. Where necessary, consider excluding the subject, and using MRE and/or liver biopsy for evaluation.

To avoid additional power loss of acoustic push for SWE acquisitions, keep the liver capsule parallel to the transducer face in both planes (transverse and elevational planes). For the same reason, the acquisition ROI placement should be in the center of the image.

Please refer to Manufacturers' instructions on acquisition techniques, procedures and machine specific pitfalls for additional information. Appendix D contains this material for a number of Manufacturers.

Liver Movement. Absence of motion during SWS acquisition is critical to obtain accurate and precise SWS measurements. Even though challenging in some patients, it is critical to ensure that no appreciable motion occurs during acquisition. Otherwise, the acquisition should not be included in the analysis. Having the patient practice breath holds (suspended tidal respiration) may be helpful but avoid practicing so much that patient becomes fatigued.

Transducer Pressure. Too much transducer pressure can increase the stiffness of underlying tissue. Only light transducer pressure should be applied during shear wave imaging and point quantification. Slightly increased pressure may be applied if it is needed to compress the abdominal wall sufficiently to enable SWS acquisition at an appropriate depth in the liver.

515 <u>Point Shear Wave Speed Measurement</u>

The above considerations in image acquisition also apply to the measurement of shear wave speed from a single location with or without SWS imaging, often referred to as point SWS measurement. The following are some additional specifics to point SWS measurement.

Measurement Region of Interest (ROI) Placement. ROI placement with respect to depth and lateral positioning is critical. A **depth** greater than 2cm deep to the liver capsule will avoid the slightly stiffer

Commented [OK63]: No related information in Appendix G.

Commented [KA64]: AAPM:

"Newer data seem to suggest that stronger pressure is fine for intercostal acquisition, which actually decreases the acquisition failure rate without changing the quantification results (Byenfeldt, et al. 2019 Ultrasound in Med & Biol). One Manufacturer suggests using this approach. Obviously, it would be different for subcostal acquisition."

Commented [BG65R64]: FOR COMMITTEE DISCUSSION: IS THERE ENOUGH EVIDENCE TO REMOVE OUR RECOMMENDATION OR QUALIFYING IT TO SAY IT DOES NOT APPLY TO INTERCOSTAL ACQUISITION?

Commented [BG66R64]: Reply not enough data yet to recommend higher pressure. Will eval again for next version

Commented [BG67R64]: Add the following to the spreadsheet as a response: The committee feels that there are not yet enough data to recommend higher pressure and how much higher that might be. This willi be re-evaluated for the next version of the profile.

861.

485

490

495

500

505

510

subcapsular liver tissue. A depth <6.5 cm will help to ensure that the shear wave amplitude is sufficient for reliable estimates of shear wave speed. Positioning away from discrete structures (e.g., vessels) is important as the algorithms used to estimate SWS assume homogeneous isotropic tissue, not heterogeneous tissue containing specific structures or lesions. An image should be acquired to document the ROI location relative to vessels so as to allow future acquisition at the same location for additional measurements, either at the same time or on follow-up examinations.

Positioning the ROI away from the **centerline** of the image may introduce variation in SWS estimates as may changing the ROI size. The effects of changing ROI size have not yet been systematically examined.

Please refer to Manufacturer specific instructions and specifications for guidance on additional steps to take during point shear wave speed acquisition (see Appendix D).

Positioning the ROI at a **constant depth** as close as practicable from measurement to measurement and from one patient visit to another is important because SWS estimates are known to decline as a function of depth with many current SWS software implementations. Measuring at a constant depth will help to minimize variations.

535 Shear Wave Speed Imaging

525

530

540

545

550

555

560

This section deals with imaging settings that may be operator controlled which may affect diagnosis and ROI placement for point measurements

SWS Imaging Color Map. If control of the color map used for imaging is possible, the operator (technologist or radiologist) should ensure that a map is used that is consistent from patient to patient and exam to exam. An agreed upon standard (i.e. blue is stiff or soft) has not yet been devised but the operator is encouraged to use the standard once it is agreed upon.

SWS Imaging Color Transparency. When color is overlaid upon the grayscale b-mode image, the amount of b-mode image that shows through the color image should be adjusted so that grayscale landmarks may be seen but changes in color are still clearly identifiable. Follow the Manufacturer's recommendation as a starting point (see appendix D).

SWS Imaging Frame Averaging. The color display may be averaged over several frames to reduce flicker and rapidly changing colors. This should be set to manufacturers specifications unless the Manufacturer provides guidance for the use of other settings.

SWS Imaging Frame Rate and Color Box Size. If the size of the box within which color is displayed is controllable the operator should select the largest box that provides an acceptable frame rate. Until a standard emerges the Manufacturer's specification and guidance may be used (see appendix D).

Point Shear Wave Speed Measurements from Shear Wave Images

This section describes criteria and procedures related to producing quantitative measurements from the SWS images that are necessary to reliably meet the Profile Claim.

SWS Image Point Measurement ROI Location. The location in the shear wave speed image for point measurements may depend on the type of pathology of concern. For example, for diffuse organ disease a global assessment may require positioning some ROI's in the largest homogeneous areas showing the predominant SWS in the images. Some ROI's may also be placed in the areas of high SWS for estimates of SWS in areas of greatest pathological change. Values from these ROI's should be identified as maximum SWS values to distinguish them from predominate SWS values so that the reader may provide

Commented [OK68]: So either do what the manufacturer says or do what the manufacturer says?

an interpretation based on complete information.

For some focal lesions (such as breast cancers), the literature supports positioning ROI's in only areas of maximum SWS identified in the images. This is because most values in a cancer may be artificially decreased due (probably) to artifacts from shear wave reflection at lesion boundaries. Please also refer to Manufacturers guidance regarding ROI positioning based on SWS image appearance. Some Manufacturers have begun to supply additional images related to SWS quality and variability estimates. These images can be used to help position the ROI in the manner specified by the Manufacturer.

SWS Imaging Point Measurement ROI size. The ROI size may be pre-selected by the Manufacturer. If adjustable use the default setting for suspected diffuse disease and consider decreasing ROI size if small areas of increased SWS speed on the SWE image are being evaluated. Check Manufacturer guidance regarding reduction of ROI size and potential problems that may result.

SWS Imaging Point Measurement Data Transfer. Follow Manufacturer's instructions and/or institutional quidelines for this. Transfer may include capture of the measurement screens into PACS and/or recording of values on a worksheet. Transfer to PACS or a report via DICOM SR (structured reporting) is another option.

3.9.2 SPECIFICATION

565

570

575

Parameter	Actor	Requirement	DICOM Tag
SWS Acquisition System	Operator	Shall perform acquisition on the same ultrasound system or same brand of ultrasound system whenever possible and especially when performing successive measurements on the same patient. If this is not possible calibration values obtained for each system used on the same patient should be forwarded with the test results for use during interpretation.	
Patient Position	Technologist or Radiologist	Shall position the patient supine or approximately 30° left lateral decubitus.	
Respiration ⁱⁱ	Technologist	Shall perform several practice acquisitions with patient in suspended tidal respiration so that the patient can learn the technique and get used to the sensation of the ultrasound transducer while in suspended tidal respiration, and the duration of the required breath hold. Shall ensure that patient is in suspended tidal respiration during acquisition of shear wave data and postacquisition image and that no other liver movement is observed during this process.	
Transducer Position	Technologist or Radiologist	Shall position the transducer at an intercostal space wide enough to accommodate the transducer and at the correct level to image/acquire from the mid to upper	

Formatted: Body Text, Space After: 0 pt

SWS Profile FINAL REVISION FOR CONSENSUS STATUS VOTE-KOD20201221 bsg final review in process.docxSWS Profile FINAL REVISION FOR CONSENSUS STATUS VOTE-KOD20201221

Parameter	Actor	Requirement	DICOM Tag
		right liver lobe. Shall position the transducer face long axis parallel to the intercostal space and check for correct positioning by inspection of the image for shadowing at the image edges. Shall position the transducer face in contact with the skin and parallel to the liver capsule so that the acoustic waves travel perpendicular to the capsule.	
Transducer Pressure	Technologist or Radiologist	Shall use only light pressure during SWS acquisition –just enough to maintain skin contact. May use slightly more pressure to compress body wall when needed to enable ROI to be positioned in proper position in Liver.	
Ultrasound image – location confirmation	Technologist or Radiologist	Shall confirm the absence of focal structures near image center and confirm no acoustic shadowing from the ribs.	

Parameter	Actor	Specification
Measurement Region of Interest (ROI) Placement	Technologist or Radiologist	Shall position the ROI at least 2cm deep into the liver capsule and less than 6.5 cm from the transducer face.
		Shall position the ROI away from discrete structures such as liver margin, nodules, portal triads or hepatic veins.
		Shall position the ROI near the center of the image in the lateral direction and away from the right or left image margins.
		Shall use the standard ROI size specified by the ultrasound vendor as the default for their system. The standard for each MANUFACTURER should conform to a minimum size of 6mm X 10mm or diameter of 10mm.
Follow-up Consistency	Technologist	Shall make follow-up acquisitions and ROI placements consistent with the baseline measurement in terms of the Transducer Position and Measurement Region of Interest (ROI) Placement.
Number of Measurements	Technologist or Radiologist	Shall take the number of measurements specified by the Manufacturer (see Appendix D) or if not specified, 10 measurements.
Liver Movement	Technologist or Radiologist	Shall acquire only when there is no visible liver motion.
SWS Imaging Color Map	Technologist or Radiologist	Shall ensure consistency of selection between examinations and patients. Shall adhere to institutional and/or national standards. See Manufacturer specific guidelines.

Parameter	Actor	Specification
SWS Imaging Color Transparency	Technologist or Radiologist	Shall set to adequately visualize color changes and grayscale anatomy. See Manufacturer guidelines.
SWS Imaging Frame Averaging	Technologist or Radiologist	Shall set according to preference after initially setting according to Manufacturer recommendations.
SWS Imaging Frame Rate/ Color Box Size	Technologist or Radiologist	Shall set to provide as large a box as possible consistent with adequate frame rate for visualization of color. See Manufacturer guidelines.
SWS Imaging Point Measurement ROI location	Technologist/ Radiologist/	Shall place the measurement ROI location in most homogenous region of SWS color map or other images related to SWS variability as specified by MANUFACTURER (Appendix D).
SWS Imaging Point Measurement ROI size	Technologist/ Radiologist	As per MANUFACTURER specifications (Appendix D). Each Manufacturer should specify an optimal measurement ROI size and make that a default for their system. A minimum size of 6mm X 10mm or diameter of 10mm.
SWS Imaging Point Measurement Data Transfer	Technologist/ Radiologist	Shall transfer SWS measurement objects to PACS or other storage and confirm successful storage.

3.10. Image Data Reconstruction

This activity describes criteria and procedures related to producing images from the acquired data that are necessary to reliably meet the Profile Claim.

Reconstruction protocols are preset by the Manufacturers and not user modifiable or selectable. Image display parameters are user selectable but do not affect quantification of SWS or the profile claims. Therefore this section is not applicable to this profile on SWS.

3.11. Image QA

This activity describes criteria and evaluations of the images that are necessary to reliably meet the Profile Claim.

590 <u>3.11.1 DISCUSSION</u>

As SWS estimates may be variable with current implementations, care must be taken to avoid introducing additional variation. Assessment of the quality of each acquisition should be made and values obtained during suboptimal acquisitions should be deleted and not included in mean or median estimates. Situations where suboptimal acquisitions may be made include:

- liver movement during acquisition,
- patient talking during acquisition,
- transducer slippage during acquisition,

Commented [OK70]: KOD Editorial

It appears that there are Manufacturer specifications, guidelines, and recommendations. The specifications are provided in Appendix D and presumably guidelines and recommendations are elsewhere? Or if it's all the same thing, lets use the same word.

Commented [OK69]: KOD Technical

This seems to be a duplicate of the Measurement ROI Placement higher up in this table. If so, can remove this row.

Commented [OK71]: KOD Editorial

This is what 3.12 was intended to cover (images and data). In any case, this probably does not affect the wCV. Can probably just drop.

580

585

- inadvertent shift of ROI to a deeper or shallower depth, and
- placement of the ROI near to a vessel or other discrete structure.

Images acquired immediately prior to and immediately after SWS acquisition may be used to confirm lack of liver movement during the acquisition. Different ultrasound systems vary greatly in their ability to save pre-acquisition and post-acquisition images in close temporal proximity to the SWS acquisition. Experimentation to determine the best procedure for this may be necessary and often, practice to make the images quickly is needed.

Subjective assessment of motion is sufficient at this stage since the amount of motion that can be tolerated is not known. If upon further study, acquisition is extremely motion sensitive, measures to quantify motion and automatically discard suboptimal acquisitions may be required in future profile versions.

The operator should discard the acquisition if movement is detected by any method.

3.11.2 SPECIFICATION

Parameter	Actor	Requirement
Suboptimal SWS Acquisition	Technologist or Radiologist	Shall exclude any SWS measurement deemed to have been acquired sub-optimally, either based on observations made during the acquisition or based on inspection of the saved images. See section 3.9.2 for acquisition-related exclusion criteria.
User training on image display	Manufacturer	Shall provide radiologist training on image interpretation and Operator training on optimal placement of measurement ROI.

3.12. Image Distribution

This activity describes criteria and procedures related to distributing images that are necessary to reliably meet the Profile Claim.

There are no relevant requirements for image distribution.

3.13. Image Analysis

This activity describes criteria and procedures related to producing quantitative measurements from the images that are necessary to reliably meet the Profile Claim.

No actual image analysis is needed to meet the Profile claim. See section 3.9. SWS Image Acquisition (SWEI) and Point SWS Measurement for requirements on producing the SWS measurements.

3.14. Image Interpretation

This activity describes criteria and procedures related to clinically interpreting the measurements and

Commented [OK72]: Since this training likely occurs around the time of the installation activity, rather than every day during the OA step of each study, consider moving this requirement up to 3.4.2 or perhaps 3.1.2.

Commented [BG73R72]: This typically occurs on an on-going basis as new personnel arrive and need training. So leave it here

Commented [OK74]: GUIDANCE:

Since the output of the Image Analysis is often the biomarker value which is in one or more of the Profile Claims, requirements on the Image Analysis Software will likely include a quantitative performance requirement that relates very closely to the Claim performance.

The profile author will likely need to draft an assessment procedure for Section 4 that describes clearly how to assess whether the software conforms to that requirement. Since the Claim is based on all actors conforming to the Profile, this assessment procedure should use data that is conformant to the rest of the profile. It would be unfair to expect Analysis Software to achieve the requirement when working on "sub-standard" data.

600

605

610 T

615

625 images that are necessary to reliably meet the Profile Claim.

No clinical interpretation is required to meet the profile claim

4. Assessment Procedures

Most of the requirements described in Section 3 can be assessed for conformance by direct observation, however some of the performance-oriented requirements are assessed using a procedure. When a specific assessment procedure is required or to provide clarity, those procedures are defined in subsections here in Section 4 and the subsection is referenced from the corresponding requirement in Section 3.

4.1. Assessment Procedure: Imaging Performance

This procedure can be used by a scanner vendor or an imaging site to assess the imaging performance of an ultrasound system. Imaging performance is assessed in terms of change compared to specifications and/or initial testing of most recent prior QA testing when imaging a phantom.

4.1.1 OBTAINING AND MAINTAINING THE IMAGING PHANTOMS

Ultrasonic Imaging and SWS Phantoms Used for Testing:

A commercially available standard ultrasound imaging phantom may be used to confirm imaging performance of the ultrasound systems used for SWS acquisition.

For testing of instrument (scanner) SWS performance, an elastic phantom will be used since it is both affordable and practical. A viscoelastic phantom may be used for testing in later versions of the profile to better address possible bias (bias is not part of the claims in this version).

A Simple phantom rather than a complex structured phantom will be used since the liver is a relatively homogenous organ.

The phantoms selected for instrument pre-delivery testing by Manufacturer should meet the following specifications:

Ultrasonic Imaging Phantom Specifications:

- a. Attenuation: 0.5 ± 0.1 dB/cm/MHz
- b. Back Scatter: Approximately $10^{-4}-10^{-3}~\rm cm^{-1}Str^{-1}$ at 3 MHz or sufficient to create mean speckle brightness comparable to a human liver-mimicking phantom (\pm 3 dB)
- c. Speed of Sound: $1540 \pm 30 \text{ m/sec}$
- d. Volume and Shape:
 - i. Cylindrical or rectangular
 - ii. Height: 15 ± 3 cm
 - iii. Diameter: 12.5 ± 3cm in inner diameter (ID)

Shear Wave Speed Phantom Specifications:

- a. Attenuation: 0.5 dB/cm/MHz (± 0.1 dB/cm/MHz)
- b. Back Scatter: Approximately $10^{-4} 10^{-3}$ cm⁻¹Str⁻¹ at 3 MHz or sufficient to create mean speckle

Commented [OK75]: KOD Editorial

This statement doesn't quite match the actual assessment requirement stated in 4.1.2.

Commented [OK76]: I would be inclined to make some normative requirements in this section. Currently it is all "shoulds", "mays", and "wills" but no "shalls". But that could be addressed later if people are tired now. And it makes it easier to conform if you're allowed to deviate from these specs.

Commented [KA77]: AAPM:

"The specifications of the phantom are not consistent. Attenuation is given as 0.6 or 0.5 dB/cm/MHz with a

standard deviation of 0.1 or 0.2. In addition, speed of sound value and tolerance range are also not consistent."

Commented [BG78R77]: The correct values is: $.5 \, dB/cm/MHz \pm 0.1$. Will make all listings consistent.

Commented [BG79R77]: All listings are verified as being correct.

Commented [KA80]: AAPM:

"Do the phantom specifications make sense for a pediatric patient as well (attenuation & backscatter)?"

Commented [BG81R80]: Answer to AAPM: The phantom specifications are for "healthy" liver. Patients may have wide variation in the parameters but producing phantoms with a wide range of various acoustic parameters would be costly and testing on all those phantoms would be unnecessarily burdensome for clinical sites given our current knowledge. If problems with SWS estimates appear during the clinical confirmation phase of profile testing then additional phantoms may be required. Clinical confirmation is currently beyond the scope of QIBA due to the need for a costly multicenter trial.

660

655

640

645

brightness comparable to a human liver-mimicking phantom (± 3 dB)⁴

- c. Speed of Sound: 1520-1540 m/sec
- d. Stiffness: Two phantoms can be used or a single phantom with two different components: Normal Liver Equivalent & Fibrotic F3 Liver equivalent. ± 5% of the specified values. Stiffness verified using Verasonics system and software from Duke University and Mayo Clinic. See https://github.com/RSNA-QIBA-US-SWS/QIBA-DigitalPhantoms.
- e. Volume and Shape Cylindrical, 20 cm tall, 12.5 cm in diameter. (Cylindrical preferred, rectangular is acceptable if width and depth are 12.5 cm and 20cm tall)

Ultrasonic Imaging Phantom Characterization:

Phantom is weighed upon construction. It is then tested following procedures in the AIUM Guidance document.⁵

<u>Pass Fail Tolerances for Site-Phantom Characterization and/or Retesting</u> (these are the same specifications as the phantoms used for pre-delivery instrument testing)

Testing to be performed at 21±1 °C.

 Method to verify temperature of phantoms prior to testing. Temperature measurement method: TBD [open issue]

Attenuation: ± 20%

• 0.5 dB/cm/MHz± 0.1 dB/cm/MHz

685 Back Scatter: ± 3dB

665

670

675

680

690

695

700

 Approximately 10⁻⁴ – 10⁻³ cm⁻¹Str⁻¹ at 3 MHz or sufficient to create mean speckle brightness comparable to a human liver-mimicking phantom (± 3 dB)]

Speed of Sound: ± 2%

1540 ± 30 m/sec [1510-1570 m/sec]

*Phantoms failing these tolerance tests shall be refused or replaced if already acquired.

Ultrasonic Imaging Phantom Temporal Stability testing:

The phantoms should be re-weighed every six months and if the phantom weight changes by more than 0.5%, the phantom should be retested to confirm that acoustic properties are within the specifications above prior to next use.

If the phantom Manufacturer has other criteria for stability testing prior to acoustic property testing, those should be used instead.

Testing of phantom acoustic properties shall be as specified by the AIUM guidelines noted previously and the phantom supplier's recommendations.

⁴ Reference - IEC 61391-2: Ultrasonics – Pulse-echo scanners – Part 2: Measurement of maximum depth of penetration and local dynamic range. 2010, Int Electrotechnical Comm: Geneva.

Commented [BG82]: FINAL REVIEW / REVISION STOP HERE 9-15-20 0:28am

Commented [BG83R82]: START FURTHER REVISIONS HERE 9-21-20

Commented [OK84]: This seems to duplicate material in the Ultrasonic Imaging Phantom Specifications above

Commented [BG85R84]: This is to emphasize the point that both types of phantoms are weighed for initial stability evaluation.

Commented [KA86]: AAPM:

"The specifications of the phantom are not consistent. Attenuation is given as 0.6 or 0.5 dB/cm/MHz with a standard deviation of 0.1 or 0.2. In addition, speed of sound value

and tolerance range are also not consistent."

 $\label{local_comment} \mbox{\bf Commented [BG87R86]: } \mbox{ Change to .5 dB/cm/MHz ± 0.1 dB/cm/MHz for consistency has been made.}$

Commented [BG88R86]: SWS COMMITTEE AGREES?

Commented [BG89R86]: All phantom attenuation values are confirmed as corrected to the above value

Commented [OK90]: Note: with the current wording, none of this is normative.

Commented [KA91]: AAPM:

"Are there any calibration specifications for a scale that would weigh the phantom?"

Commented [BG92R91]: NO...that would be getting too far afield.

⁵ Methods for Specifying Acoustic Properties of Tissue-Mimicking Phantoms and Objects 2nd Edition. AIUM Technical Standards Committee. American Institute of Ultrasound in Medicine. 2015.

*If the values are changing faster than the rates above, sites should consider replacement or testing more frequently than every 6 months.

SWS Phantom (pre-delivery and on-site phantoms)

The initial characterization of the phantoms will be performed and verified by the QIBA committee, the phantom Manufacturer, Verasonics or another party using measurements obtained from Verasonics research ultrasound systems. Independent verification of phantom properties to ensure that the phantom meets the SWS Phantom specifications above is strongly recommended. If a newly procured phantom has already been independently tested within six months of the date of manufacture and
 those results are available then additional independent testing prior to use is not necessary. The phantom Manufacturer may be contacted for assistance in finding a site that will perform independent testing.

715 SWS Phantom Temporal Stability Testing (pre-delivery and site-phantoms)

Weigh the SWS phantom monthly and if the weight changes more than 0.5% over a six-month period the following parameters will be checked by sending the phantom to a testing facility capable of performing the tests using a Verasonics system. The phantom Manufacturer may be contacted for assistance with obtaining the tests. Alternatively, a calibrated replacement phantom may be procured.

720 SWS Phantom Stability Tolerances:

725

730

735

- (1) SWS: <5% change in both hard and soft components over 6 months.
- (2) Speed of Sound: <1% change over 6 months.

If SWS Phantom stability is demonstrated at six months, then the timeline can be changed to annual testing.

SWS Phantom Temperature Sensitivity and Shipping Considerations

SWS Phantom stiffness may change as a function of temperature. For this reason, the temperature of the phantom should be recorded at the time of use. The phantom should be used at the temperature specified by the Manufacturer. Very cold or hot temperatures may damage the phantom and permanently change its acoustic and mechanical properties. Please ship according the Manufacturer's recommendations and contact the Manufacturer if shipping in extreme heat or cold is not discussed in the instructions.

Ultrasound System Phantom Testing

- a. Grayscale imaging tests as normally conducted by the ultrasound system Manufacturer or as described in the AIUM document "AIUM Quality Assurance Manual for Gray Scale Ultrasound Scanners"⁶.
 - b. Shear Wave Speed Estimations are obtained from the SWS phantom using the Manufacturer specified

Commented [OK93]: Why no normative? Is it because this will not affect performance or because these are unrealistic requirements?

If the requirements are impactful and realistic, make them shalls.

Commented [KA94]: Aapm:

"It may be helpful to add discussions of the impact of extreme temperature during shipping of calibration" $\,$

Commented [BG95R94]: COMMITTEE, SHOULD WE INCLUDE A STATEMENT ON SHIPPING? IF SO HOW SHOULD THAT READ AND WHERE SHOULD WE PUT IT?

Commented [BG96R94]: Committee: temp of acquisition should be recorded in case of phantom temp dependence. Acquisition temp already specified. Shipping should be according manufuacturers recommendations.

Commented [BG97R94]: Added as new section titled SWS Phantom Temp Sensitivity and shipping Considerations has been added at the end of 3.1.1.

⁶ AIUM Quality Assurance Manual for Gray Scale Ultrasound Scanners, AIUM Technical Standards Committee, American Institute of Ultrasound in Medicine, www.aium.org, 2014 (ISBN 1-932962-31-X)

procedures as defined in Appendix D of the QIBA SWS Profile.

Shear Wave Speed (SWS) Tolerance: ± 5% of the Verasonics system calibration value for the phantom as determined by the QIBA calibration site.

4.1.2 ASSESSING IMAGING PERFORMANCE

740

750

760

765

745 The assessor shall perform grayscale imaging tests as normally conducted by the ultrasound system manufacturer or as described in the AIUM document "AIUM Quality Assurance Manual for Gray Scale Ultrasound Scanners".

A link to the QA Tests and expected results recommended by AIUM is given here (login required): http://aium.s3.amazonaws.com/resourceLibrary/14qa.pdf

4.2. Assessment Procedures: SWS Measurement Consistency

This section describes a group of procedures for assessing the performance of a site or of individual actors to determine if pre-established quantification performance specifications are met. For a site, those pre-established quantification performance specifications are the claims made in the claims section of the profile. For the individual actors, the performance specifications are those that have been shown, or are likely to be necessary for the site to meet the performance claims of the profile. The performance specifications for actors are based on the results of the technical and claims confirmation studies performed during the QIBA profile development process (see the QIBA wiki: https://qibawiki.rsna.org/index.php/Process) and/or on typical acceptable performance achieved in clinical practice worldwide.

The overall performance of a site (and its ability to meet the profile claims) depends upon multiple actors meeting or exceeding their performance specifications, even if they already meet the procedural performance expectations of the profile (checklist compliance – see section 5). Clearly if an actor's performance does not meet specification, the profile claim may be invalidated for that site but inadequate performance on the part of one actor may be compensated for by better than expected performance of another actor. The described assessment procedures are designed to test the hypothesis that an Actor's wCV meets the Profile requirement at a specified type I error rate (usually 5%). It is not sufficient to show that the observed wCV is <10% for only a sample of cases.

Therefore, two types of assessment procedures and performance specifications are described: A) those for assessment of composite performance of a site and B) those for testing individual actors. The assessment procedures for types a and b may be the same or very similar to one another but different performance specifications will be given.

⁷ AIUM Quality Assurance Manual for Gray Scale Ultrasound Scanners, AIUM Technical Standards Committee, American Institute of Ultrasound in Medicine, www.aium.org, 2014 (ISBN 1-932962-31-X)

Commented [KA98]: AAPM::

"The link is broken."

Commented [BG99R98]: COMMITTEE: SAME ISSUE AS THE OTHER LINK...IT DOESN'T WORK EVEN WHEN YOU ARE LOGGED IN AND GETTING THE DOCUMENT REQUIRES THAT YOU VISIT THE RESOURCE LIBRARY NOT THE STORE. GIVEN THAT THE LINK MAY CHANGE AGAIN EVEN IF WE UPDATE IT, SHOULD WE JUST DIRECT INDIVIDUALS TO THE AIUM RESOURCE LIBRARY?

I HAVE UPDATED THE LINK

Commented [BG100R98]: Committee: direct to AIUM resource library

Commented [BG101R98]: The footnote listing has been retained but the broken link has been removed. A link to the reference library has been tentatively inserted pending an answer from AIUM regarding a stable link and note has been made that one must login to the AIUM site to obtain the document.

Formatted: Body Text

Cross-sectional claims (for a given patient at a single time point) require testing of within subject precision, often termed "repeatability" as well as bias. Longitudinal claims (for a given patient at different time points or for different imaging methods at one or more time points require testing of repeatability, bias, linearity and regression slope. As this profile makes multiple longitudinal claims and one cross-sectional claim, numerous testing procedures are described below along with the claim that each applies to.

4.2.1 SITE ASSESSMENT TOOLS AND TESTS.

4.2.1.0 Site assessment dataset.

The dataset (or "parts being measured" in six sigma measurement system analysis) are livers of patients and two test phantoms, a b-mode imaging test phantom and a calibrated elastography phantom.

4.2.1.1. Site assessment data acquisition

4.2.1.1.A. ——B-mode imaging:

For Ultrasound b-mode imaging assessment a standard ultrasound test phantom shall be used to acquire test images and measurement values that will be evaluated according to the methods described in the AIUM quality assurance manual. The specification for the phantom is given in section 34.1.2-1 above.

4.2.1.1.B. Phantom SWS:

For assessment of SWS performance and conformance in phantoms, calibrated SWS phantoms shall be used. These phantoms can be obtained from phantom manufacturers and consist of either two phantoms, one with stiffness approximating normal liver and the other with a stiffness approximating a liver with F3 fibrosis, or a single two-part phantom containing regions with each of the two stiffnesses. The specifications of the phantoms are given in section 3.3.1 above along with instructions for periodic phantom stability checks.

The site assessment phantom data will consist of SWS acquisitions obtained by each operator who has been qualified by training and testing to acquire SWS data according to the following criteria:

Twenty (20) distinct SWS measurements will be collected from each of the two phantoms at both 4.5cm and 7 cm depths, by each operator. For these tests a measurement is defined as completed when the scanner outputs a SWS to the screen or to the data collection table within the machine. A system may acquire multiple SWS values and then report an overall SWS value (i.e. mean and median). The individual SWS values are the measurements, not this summary result. So, for each operator a total of 80 measurements, 20 for each of the two phantoms and for each of two different depths.

* If a site has ultrasound systems from more than one manufacturer, the test measurements must be performed for each manufacturer's system (only one set of test measurements per manufacturer unless the manufacturer notes that different models of their systems give different SWS results). So, for multiple different ultrasound systems being used to acquire SWS, the total number of measurements taken per operator will be 80 x n where n = the number of ultrasound

Formatted: Space After: 0 pt

Formatted: Heading 4

Commented [KA102]: AAPM:

"Are there any pediatric-specific phantoms that are required during this evaluation? It states only that two phantoms will be used."

Commented [BG103R102]: ANSWER FOR SPREADHEET: Pediatric specific phantoms should not be required since existing phantoms test system performance for probes typically used for pediatric imaging as well as those for adults. A phrase briefly clarifying what the two phantoms are has been added.

Commented [BG104R102]: Committee agrees

Formatted: Heading 4, Space After: 0 pt

Formatted: Heading 5, Space After: 0 pt

Formatted: Indent: Left: 0.2", Hanging: 0.2"

805

ደበበ

780

610

systems. It is expected that acquisition of these phantom measurements will take approximately 20 minutes per machine.

•

*Depth is defined as the distance from the transducer surface to the center of the region of interest from which the point SWS is acquired.

•

*Between each measurement, the transducer will be removed from contact with the phantom and the phantom will be shifted so that each measurement is performed with the transducer oriented differently relative to the phantom in a random manner. NO effort to reposition the transducer in the same exact spot as the previous measurement should be made.

825

320

*The temperature at which the testing was performed at should be recorded. It is strongly recommended that the measurements be performed at the temperature at which the phantom was calibrated by the QIBA test site or manufacturer using approved QIBA instrumentation and methodology.

830

840

*Each ultrasound scanner will have different specific instructions that should be followed as noted above, but one important requirement is that the transducer should remain motionless during each measurement. If transducer movement is detected by any method during measurement, that value should be discarded and another measurement taken.

835

*The operators will be blinded with respect to the actual SWS values represented in the phantom(s). The operator will however see a large number of SWS measurements from each phantom since the phantom(s) will be used repeatedly. Therefore, the operator must NOT discard a SWS measurement solely because it appears different from the others or from the assumed "true" value for the phantom

4.2.1.1.C. In-vivo SWS data:

Six volunteers having no history of liver disease and with normal AST, ALT, Alkaline Phosphatase and Total Bilirubin values will be recruited. The volunteers should cover a range of BMI values from 20 to 35-and ildeally-volunteers who will be available for at least several rounds of testing (months to years)-can be recruited. The site assessment in-vivo data set will consist of ten (10) measurements by each operator on each of the six volunteers and at two different depths made according to the following criteria:

850 e

855

- * Ten (10) distinct SWS measurements at each of two depths (4.5cm and 7cm) will be made from each volunteer by each operator. Depth is defined as the distance from the transducer face to the center of the region of interest used for acquisition of the SWS value (not the region defined for shear wave imaging display).
 - * The measurements will be performed with the volunteer having fasted for at least six hours
- * The measurements will be made according to the instructions provided by the scanner manufacturer and according to the guidelines in section 3.9 of this profile.
 - * The measurements should be performed for each brand of ultrasound scanner if scanners from multiple manufacturers are used to acquire SWS data. All scanners from a given manufacturer are

Formatted: List Paragraph, Indent: Left: 0.2", Hanging: 0.2", Bulleted + Level: 1 + Aligned at: 1.13" + Indent at: 1.38"

Formatted: List Paragraph, Indent: Left: 0.2", Hanging: 0.2", Bulleted + Level: 1 + Aligned at: 1.13" + Indent at:

Formatted: List Paragraph, Indent: Left: 0.2", Hanging: 0.2", Bulleted + Level: 1 + Aligned at: 1.13" + Indent at: 1.38"

Formatted: List Paragraph, Indent: Left: 0.2", Hanging: 0.2", Bulleted + Level: 1 + Aligned at: 1.13" + Indent at: 1.38"

Formatted: List Paragraph, Indent: Left: 0.2", Hanging: 0.2", Bulleted + Level: 1 + Aligned at: 1.13" + Indent at: 1.38"

Formatted: Heading 5, Space After: 0 pt

assumed to give identical results unless otherwise specified by the manufacturer.

- * Between each measurement, the transducer should be removed from contact with the volunteer, and the volunteer should get up from the scan table between each measurement. If this is not feasible due to time limitations or physical condition of the volunteer, the measurements should be divided into groups of five (5) measurements and the volunteer should get up from the scan table before lying down for the next measurement group.
- * As for the phantom data collection, a SWS measurement is defined as whenever a SWS value appears on the scanner screen, NOT the mean value or median value reported by the scanner after several measurements.
- * As for phantom SWS measurement, values obtained during visible patient or transducer movement should be discarded and repeated.
- * SWS values that appear different from the others by a sizeable amount should never be discarded unless there was movement during the measurement, or another error occurred. Errors in measurement are defined as measurements where the manufacturer instructions were not followed. If a SWS is discarded, a repeat SWS measurement should be collected.

4.2.1.2. Site Conformance - Quality Metrics and Computation

As a number of distinct claims are made that depend on the depth that SWS is estimated and the stiffness of the tissue being examined, separate performance analysis will be performed for each combination of the two parameters, depth and material stiffness. The test data will contain data from the exact same two depths as specified in the claims but only two test phantoms will be used to assess performance at the three different stiffness ranges specified in the claims. The two phantoms are high and low stiffness and are expected to have stiffness values the will result in SWS values in the low (0.9-1.2 m/s) and at the lower bound of the high stiffness range. Performance will therefore be judged using the claims for these two stiffness ranges.

4.2.1.2.A. Within Subject Measurement Variation.

860

865

870

875

885

890

895

SWS claims use within subject coefficient of variation (wCV) as an important quality metric, wCV computation from the test dataset (dataset as described under 4.2.1.1.B above) is as follows (next paragraph):

For each case (corresponding to the liver of a single patient where the variable i denotes the case number), the first measured SWS as described in 4.2.1.1 represents the first replicate measurement (denoted Y_{11}) and the second measured SWS represents the second replicate measurement (Y_{12}) for that case. For phantoms, there is only a single phantom for each of the two stiffness being analyzed separately so i takes on the single value i =1. For patient data, there are six volunteer subjects so the variable i ranges from 1 to 6. For each case and for each combination of depth and stiffness range, the assessor shall first calculate the mean and variance of the measurements (five per operator per machine for phantoms and three per operator per machine for human volunteers). From these values, the variance divided by the square of the mean (mean²) will be calculated for each case and the results for each case will be summed and the total divided by the number of cases (one for the phantom and 6 for the human data). The square root of this value is the wCV. The equations for these computations are:

Formatted: Heading 4, Space After: 0 pt

Formatted: Heading 5, Space After: 0 pt

$$\widehat{wCV} = \sqrt{\sum_{i=1}^{N} \left\{ \frac{Variance_i}{Mean_i^2} \right\} / N}$$

Where N=6 for the patient data and N=1 for phantom data.

As noted in the preceding paragraph, if data were acquired from more than one brand of machine and more than one operator, the measurements from all machines and all operators should also be pooled for the computation to accurately reflect these sources of variability.

4.2.1.2.A-1 Maximum Allowable Variance.

900

905

910

915

925

To assure site conformance to the profile claims, the upper 95% confidence bound of the wCV computed above must be less than the wCV reported in the claim to ensure that the calculated wCV for a site meets the claim with 95% confidence.

[Data available for maximum allowable wCV and RC:

Phantoms: 20 per operator, per phantom stiffness value (2 values), per depth (two different depths)

Patients: 10 per operator, per depth (two depths), per patient (6 patients).]

With 6 subjects and 10 replicates per subject per depth, and with claims stating wCV of 4% and 5% for depths of 4.5 and 7.0 for moderate SWS values, the maximum allowed wCVs are 3.3 and 4.1 for depths of 4.5 and 7.0, respectively.

4.2.1.2.B Site Percentage Bias Estimation:

Although bias claims are not made in the current version of the profile, this calculation is provided for use in later versions of the profile where bias claims will be made. At the present time, bias claims for phantoms only are expected as no verified clinical methods for estimation of true SWS in patients are available. MRE may eventually be a qualified method for provision of "gold standard" SWS values for computation of bias. Currently the values obtained using a standard acquisition procedure in phantoms (using a Verasonics research system) are considered the "gold standard" for bias and linearity estimation.

As the claims are stratified by acquisition depth and SWS range, bias estimates will also be estimated by the same categories.

For each of the four measurement situations (3.5cm depth, soft phantom; 7cm depth soft phantom; 3.5cm depth stiff phantom, 7cm depth stiff phantom), the data available are 20 x N where N is the number of operators.

For each measurement, the assessor shall calculate the value of the SWS (denoted Y_i), where i denotes

Formatted: Heading 6, Space After: 0 pt

Formatted: Heading 5, Space After: 0 pt

Commented [KA105]: AAPM:

"There needs to be a closing parenthesis to end the sentence."

Commented [BG106R105]: PARENTHESIS HAS BEEN ADDED

Formatted: Body Text

the i-th acquisition. The assessor shall calculate the % bias: $b_i = [(Y_i - X_i)/X_i] \times 100$, where X_i is the true value of the measurand. Over N acquisitions estimate the population bias: $\hat{b} = \sum_{i=1}^N b_i / N$. The estimate of variance of the bias is $\widehat{Var}_b = \sum_{i=1}^N (b_i - \hat{b})^2 / N(N-1)$. The assessor shall calculate the 95% CI for the bias as $\hat{b} \pm t_{\alpha=0.025,(N-1)df} \times \sqrt{\widehat{Var}_b}$, where $t_{\alpha=0.025,(N-1)df}$ is from the Student's t-distribution with α =0.025 and (N-1) degrees of freedom. The lower bound of the 95% CI must be > -5% and the upper bound of the 95% CI must be < +5%.

Formatted: Body Text, Space After: 0 pt

4.2.1.2.C Site Linearity Estimation and Slope Estimation.

940

945

950

960

965

970

The phantom data set will be used. Since the longitudinal claims specify using the same operator and ultrasound system at each point in time the measurements from each operator and US system will be analyzed separately. The test data for each operator and machine consist of 20 measurements for each of two different measurement depths and for two different stiffness values.

For each operator and ultrasound system combination calculate linearity as follows:

For each measurement, the assessor shall calculate the SWS (denoted Y_i), where *i* denotes the *i*-th measurement. Let X_i denote the true value for the i-th measurement. The assessor shall fit an ordinary least squares (OLS) regression of the Y_i's on X_i's. A quadratic term is first included in the model to rule out non-linear relationships: $Y = \beta_o + \beta_1 X + \beta_2 X^2$. If $|\beta_2| < 0.5$, then the assessor shall fit a linear model: $Y = \beta_o + \beta_1 X$, and estimate R².

The absolute value of the estimate of β_2 should be <0.50 and R-squared (R²) should be >0.90. For the linear model fit, let $\widehat{\beta_1}$ denote the estimated slope. The assessor shall calculate its variance as $\widehat{Var}_{\beta_1} = \{\sum_{i=1}^N (Y_i - \widehat{Y}_i)^2 / (N-2)\} / \sum_{i=1}^N (X_i - \overline{X})^2$, where \widehat{Y}_i is the fitted value of Y_i from the regression line and \overline{X} is the mean of the true values. The assessor shall calculate the 95% CI for the slope as $\widehat{\beta_1} \, \pm \, t_{\alpha=0.025,(N-2)df} \sqrt{\widehat{Var}_{\beta_1}}$.

Allowable Slope Range: For most Profiles it is assumed that the regression slope equals one. Then the 95% CI for the slope should be completely contained in the interval 0.95 to 1.05. These thresholds should be specified in Section 3 of the Profile.

4.2.2 ASSESSING SWS CONSISTENCY COMPARED WITH PHANTOM SPECIFICATIONS--- SEE THIS TOPIC IN SECTION 3.4.1

4.2.3- INDIVIDUAL ACTOR TOOLS AND TESTS

As this profile was created based on considerable preliminary phantom data testing designed to assess the contribution of various actors to overall imprecision and bias, a "top down threshold selection" approach is used to assess the bias and imprecision attributable to each actor. Phantom studies have shown that the site and observer are small contributors to variability in phantoms. This finding may not generalize to patients however since the potential for operator errors and operator-patient interaction

variation is much greater. Analysis of the test data using six sigma measurement systems analysis methods such as crossed gauge r and r with anova are expected to provide sufficient information on relative contribution of the various actors to overall variance so that appropriate corrective measures may be taken to reduce overall imprecision to levels consistent with the profile claims. (further discussion in next version).

4.2.3.1. Technologist/Operator Qualification Testing-

975

980

985

990

995

1000

1005

The test data set for phantoms and for in-vivo [patients] are described in sections 4.2.1.1.B and 4.2.1.1.C. The test data are acquired by each Technologist/Operator so are suitable for qualification testing. A similar data set acquired only in-vivo would also suffice. See section 3.1.2 Staff Qualification for the test and test criteria for qualification.

4.3. Assessment Procedure: SWS Measurement Concordance

This procedure can be used by a manufacturer or an imaging site to assess the concordance of SWS measurements an ultrasound system. Measurement concordance is assessed in terms of the difference between the measurement made on a phantom by the ultrasound system and a reference value for that phantom.

The assessor shall obtain an elastic SWS phantom as described in section 4.1.1.

The assessor shall <u>have someone else</u> measure the shear wave speed on the phantom using the instrument settings and acquisition procedures specified by the Scanner Vendor in Appendix D <u>and</u> according to the phantom acquisition protocol defined in section 4.2.1.1.B. Phantom SWS data acquisition.

The <u>assessorse results wishall be compared to obtain for the same phantom</u> the shear wave speed obtained using the Verasonics system for the same phantom as determined by the QIBA calibration site (which may be the phantom <u>m</u>Manufacturer). If the phantom specifications and independent test values are slightly different, the average of the two values will be used.

The assessor shall compute the SWS Measurement Consistency as the percentage difference between the ultrasound and MRE SWS measurements. This computation may be made according to the instructions given in section 4.2.1.2.B, Site Percentage Bias Estimation.

To keep the <u>assessorindividual acquiring the data</u> blinded to the true phantom values, the computation of Site Bias should be conducted by **someone different** than the individual acquiring the data.

5. Conformance

To conform to this Profile, participating staff and equipment ("Actors") shall support each activity assigned to them in Table 1 in Section 3. Activities represent steps in the chain of preparing for and generating biomarker values (e.g. product validation, system calibration, patient preparation, image acquisition, image analysis, etc.).

Formatted: Heading 4, Space After: 0 pt

Commented [OK107]: MOVED

Details moved here from 3.4.1

Formatted: Body Text, Space After: 0 pt

Commented [OK108]: Added to match the sentence below about blinding

Formatted: Body Text

Commented [OK109]: KOD Editorial Issue

I wasn't quite clear on what this referred to. If I've broken the flow, you may need to add a few words. It sounds like there are two sources of reference values, neither of which takes priority over the other?

On the other hand if it's OK to drop, that is OK too.

Commented [OK110]: KOD editorial

I expected we would take the percentage difference between the SWS measured on the phantom and the Verasonics measurement.

Formatted: Body Text

Commented [OK111]: KOD Editorial

Is this the same as the SWS Measurement Consistency? If so, let's not introduce multiple terms.

Commented [OK112]: MOVED

Some of the new text here is moved from 3.0.1 or is a rephrasing to weave into existing text.

1010

1015

1020

1025

1030

To support an activity, the actor shall conform to the requirements (indicated by "shall language") listed in the Specifications table of the activity. Each activity has a dedicated subsection in Section 3.

For convenience, <u>all</u> the Specification table requirements have been duplicated and regrouped by actor in the form of a-checklists in a <u>MS Excel spreadsheet</u>, <u>with a tab labeled "Conformance" for each actor</u>. Appendix E <u>describes how to obtain the spreadsheet</u>.

Some requirements reference a specific assessment procedure in section 4 that shall be used to assess conformance to that requirement.

<u>Formal claims of conformance by the organization responsible for an Actor shall be in the form of a published QIBA Conformance Statement.</u>

If a QIBA Conformance Statement is already available for an actor (e.g. your analysis software), you may choose to provide a copy of that statement rather than confirming each of the requirements in that Actors checklist yourself.

Formal claims of conformance by the organization responsible for an Actor shall be in the form of a published QIBA Conformance Statement.

Vendors publishing a QIBA Conformance Statement shall provide a set of "Model-specific Parameters" (as shown in Appendix D) describing how their product was configured to achieve conformance. Vendors shall also provide access or describe the characteristics of the test set used for conformance testing.

In addition to the Conformance Checklists, the spreadsheet also contains tabs for Execution Checklists which are organized in chronological order with a tab for each Activity in Section 3. This is intended to work best for actual acquisition of quantitative image data and be easy to follow in a clinical or research environment.

Note: Execution Checklists may contain additional items that are included as reminders about best practices but are not requirements to conform to the profile. Profile requirements are limited to things necessary to achieve the performance in the Claims. Requirements can be easily identified by the use of the word "shall".

Formatted: Indent: Left: 0.5"

Appendices

1040

1045

1050

1055

1060

1065

1070

1080

Appendix A: Acknowledgements and Attributions

This document is proffered by the Radiological Society of North America (RSNA) Quantitative Imaging Biomarker Alliance (QIBA), The QIBA Ultrasound Coordinating Committee and the QIBA Ultrasound Shear Wave Speed Biomarker Committee* (US SWS BC) under the leadership of Brian Garra, Tim Hall and Andy Milkowski. Paul Carson served as QIBA Ultrasound Coordinator.

Profile Editor and leading coauthor was Brian Garra. Manish Dhyani, M.D. was a major coauthor and initial editor. Special contributions in conduct of groundwork studies and their publication were made by Mark Palmeri and his colleagues at Duke University. Other leaders of groundwork studies included Anthony Samir and colleagues at Massachusetts General Hospital, Tim Hall and colleagues at the Univ. of Wisconsin, Matthew Urban and colleagues at the Mayo Clinic, Stephen McAleavey and colleagues at The University of Rochester, and Jingfeng Jiang and colleagues at Michigan Technical University. Andy Milkowski performed an initial analysis. Discussions and contributions from Nancy Obuchowski greatly improved the statistical methods used in the analysis. Proofreading and guidance on structure of the profile were provided by Kevin O'Donnell. Cooperation of the MR Elastography Biomarker Committee, through Richard Ehman's team at the Mayo Clinic, was much appreciated for their testing in phantoms for comparison with ultrasound. The 15 ultrasound system companies mentioned below were helpful in their contributions. In particular, those included in Appendix D. provided systems and/or performed studies for the groundwork. Also participating were companies producing phantoms, test equipment, contrast agents and drug studies and volunteers from government and many academic and clinical institutions.

*Biomarker Committee members at the time of this publication:

Brian Garra, MD (co-chair) Center for Devices and Radiological Health, FDA
Tim J. Hall, PhD (co-chair) University of Wisconsin, School of Medicine & Public Health
Andy Milkowski, MS (co-chair) Siemens Healthineers USA, Inc.

S. Kaisar Alam, PhD Institute of Electrical and Electronics Engineers (IEEE)

Karen Alton, BS, RDMS, RVT Karen Alton Consulting, LLC

Michael André, PhD San Diego VA Healthcare/University of California, San Diego (UCSD)

Brian Anthony, PhD MIT John J. Antol BK Ultrasound

Michalakis (Mike) A. Averkiou, PhD University of Washington, Seattle

Paul Barbone, PhD Boston University

Felipe Barjud Pereira do Nascimento, MD Albert Einstein Hospital (São Paulo, Brazil)

Richard G. Barr, MD, PhD Northeastern Ohio Medical University

1075 Tharakeswara K. Bathala, MBBS, MD University of Texas, MD Anderson Cancer Center

Parviz Behfarin, MD Plainview Hospital

John Benson Siemens

Matt Berger, BS Samsung Electronics Co., Ltd. (South Korea)

Laura Brattain, PhD Massachusetts General Hospital

Paul L. Carson, PhD University of Michigan Medical Center

Huan Wee Chan, MB ChB The National Hospital for Neurology and Neurosurgery

Formatted: Heading 1, None, Space Before: 0 pt, After: 0 pt

	Anil Chauhan, MD University of Pennsylvania
	Jun Chen, PhD Mayo Clinic
	Shigao Chen, PhD Mayo Clinic
1085	Yuling Chen, PhD Mindray (Zonare)
	Hyo-Min Cho, PhD Korea Research Institute of Standards and Science
	Wui K. Chong, MD University of Texas, MD Anderson Cancer Center
	Yi Hong Chou, MD Taipei Veterans General Hospital
	A Jung Chu, MD Seoul National University Hospital (South Korea)
1090	Claude Cohen-Bacrie, MS e-Scopics
	Elaine Collins, RDMS PAREXEL International
	Ron Daigle, PhD Verasonics
	Jonathan R. Dillman, MD, MSc Cincinnati Children's Hospital
	Marina Doliner, MD Ann and Robert H. Lurie Children's Hospital of Chicago
1095	John Donlon Philips
	Marvin M. Doyley, PhD University of Rochester (NY)
	Shuyan Du, PhD Bristol-Myers Squibb
	Richard L. Ehman, MDMayo Clinic
	Todd Erpelding, PhD, MSE Canon Medical Systems USA
1100	Alex Exposito SuperSonic Imagine
	Steven E. Fick, PhD National Institute of Standards and Technology (NIST)
	Caterina M. Gallippi, PhD University of North Carolina at Chapel Hill
	Joel Gay, MSc Supersonic Imagine (SSI) - (Aix-en-Provence, France)
	Albert Gee Zonare Medical Systems
1105	Gilles Guenette, RDMS, RDCS, RVT Siemens
	Alexander Guimaraes, MD, PhD Oregon Health & Science University
	Zaegyoo (Jay) Hah, PhD, MBASamsung Electronics Co., Ltd. (South Korea)
	Alpana Harisinghani, MD PAREXEL International
	Peggy Harrigan, PhD PAREXEL International
1110	Christopher Hazard, PhD GE Corporate R&D (NY)
	Anis Hadj Henni, PhD Rheolution, Inc. (Montréal, Canada)
	Yasunori Honjo, PhD Canon Medical Systems
	Kenneth (Ken) Hoyt, PhD University of Texas at Dallas
	Yu Igarashi, PhD Canon Medical Systems
1115	Edward F. Jackson, PhD University of Wisconsin, School of Medicine & Public Health
	Jingfeng Jiang, PhD Michigan Technical University
	Thiago Julio, MD Hospital Israelita Albert Einstein (São Paulo, Brazil)
	Muneki Kataguchi, PhD Canon Medical Systems
	Tetsuya, Kawagishi, PhD Canon Medical Systems
1120	So Yeon Kim, MD Adan Medical Center, Korea
	Riwa Kishimoto, MD, PhD National Institute of Radiological Sciences
	Sonal Krishan, MD Medanta (India)
	Viksit Kumar, PhD Massachusetts General Hospital
	Koichiro Kurita, PhD Canon Medical Systems
1125	Hyoung Ki Lee, PhD Samsung Electronics Co., Ltd. (South Korea)
	Julian Lee Alpinion Medical Systems
	NAL Lung Loo MID LIND Coverance Children's Hespital Vencei University College of Medicine

Mi-Jung Lee MD, PhD Severance Children's Hospital, Yonsei University College of Medicine

Eleni Liapi, MD, MSc Johns Hopkins University Ken Linkhart Verasonics Jianwen Luo, PhD 1130 Tsinghua University (China) Ted Lynch, PhD Computerized Imaging Reference Systems, Incorporated (CIRS, Inc.) Andrei Lyshchik, MD, PhD Thomas Jefferson University Hospital Jerry Mabary Echosens (US operations) Michael MacDonald, PhD GE Healthcare (Ultrasound) Ravi A. Managuli, PhD, RDMS Hitachi Medical Corporation; University of Washington 1135 Stephen McAleavey, PhD University of Rochester (NY) Glen McLaughlin, PhDZonare Medical Systems Martha G. Menchaca, MD University of Illinois (UIC) Chicago Wayne L. Monsky, MD, PhD University of Washington 1140 Jaime Morales, MD Instituto Nacional de Perinatología (INPER) (Mexico) Thomas (Tom) R. Nelson, PhD Retired Kathryn Nightingale, PhD **Duke University** Svetoslav Nikolov, PhD **BK Ultrasound** Marcello H. Nogueira-Barbosa, MD, PhD University of São Paulo - Ribeirão Preto School of Medicine (Brazil) 1145 Adrian D. Nunn, PhD Bracco Research USA Nancy Obuchowski, PhD Cleveland Clinic Foundation Arinc Ozturk, MD Harvard-Massachusetts General Hospital Hugo José Paladini, MD Hospital Universitario Fundación Favaloro 1150 Mark Palmeri, MD, PhD **Duke University** Seong-Hoon Park, MDWonkwang University School of Medicine (South Korea) Kevin Parker, PhD University of Rochester (NY) Patrick Ploc Gammex, Inc. Nicolas Rognin, MSc, PhD Moffitt Cancer Center Stephen Rosenzweig, PhD 1155 Siemens Jonathan Rubin, MD, PhD University of Michigan Anthony Samir, MD, MPH Massachusetts General Hospital Leah E. Schafer, MD Partners Healthcare Mark Schafer II, PhD Sonic Tech, Inc. Cedric Schmitt, PhD Rheolution, Inc. (Montréal, Canada) 1160 Vijay Shamdasani, PhD **Philips** James Shin, MD Stony Brook University Medical Center Claude Sirlin, MD University of California, San Diego (UCSD) Gale Sisney, MD University of Wisconsin Bob Spaulding ATS Laboratories, Inc. 1165 Daniel C. Sullivan, MD Duke University Joon Sunwoo, MD, MBA Samsung Electronics Co., Ltd. (South Korea) Mihra S. Taljanovic, MD, PhD University of Arizona Kai E. Thomenius, PhD Consultant 1170 Ronald Tosh, PhD National Institute of Standards and Technology (NIST) Gregg Trahey, PhD **Duke University**

> Yao-Sheng Tung, PhD Verasonics Theresa Tuthill, PhD Pfizer

Matthew Urban, PhD Mayo Clinic College of Medicine

Tomy Varghese, PhD University of Wisconsin, Dept of Medical Physics

Sudhakar Venkatesh, MD Mayo Clinic

Michael Wang, PhD, MASc GE Healthcare (Ultrasound)
Masaki Watanabe, PhD Canon Medical Systems

Keith A. Wear, PhD U.S. Food and Drug Administration (FDA)

Thaddeus (Thad) Wilson, PhD, MS* The University of Tennessee Health Science Center

Russ Witte, PhD University of Arizona

Hua Xie, PhD Philips

Tadashi Yamaguchi, PhD Chiba University, Graduate School of Engineering Dept. of Medical

Engineering

1175

1180

1185

1190

1195

1200

1205

1210

Shuji Yamamoto, PhD National Cancer Center (Japan)

Zhi Yang Binzhou Medical University Hospital

Terry S. Yoo, PhD Center for Drug Evaluation and Research (CDER)

Kwon-Ha Yoon, MD, PhD

James A. Zagzebski, PhD

Wonkwang University School of Medicine (South Korea)

University of Wisconsin, School of Medicine & Public Health

Heng Zhao, MS, PhD GE Healthcare (Ultrasound)
Haoyan Zhou, MS Case Western University

Many of the published papers, proceedings articles and abstracts produced in this effort are referenced in http://gibawiki.rsna.org/index.php/QIBA in the Literature Citations

under the link "QIBA Literature References". Major contributors to the primary manuscript reporting much of the SWS US Biomarker Committee's work were, Mark L. Palmeri and, in alphabetical order, Richard Barr, Paul Carson, Mathieu Couade, Jun Chen, Shigao Chen, Manish Dhyani, Richard Ehman, Brian Garra, Albert Gee, Gilles Guenette, Zaegyoo Hah, Ted Lynch, Michael Macdonald, Ravi Managuli, Veronique Miette, Kathryn R. Nightingale, Nancy Obuchowski, Ned C. Rouze, Anthony E. Samir, Vijay Shamdasani, Matthew Urban, Keith Wear, Hua Xie, Timothy J. Hall. Not in order, they are from: Duke University, Durham, NC, USA, CIRS, Norfolk, VA, USA, Mayo Clinic, Rochester, MN, USA,

Philips Research, Cambridge, MA, USA, Food and Drug Administration, Silver Spring, MD, USA, Siemens Ultrasound, Issaquah, WA, USA, University of Michigan, Ann Arbor, MI, USA, The Surgical Hospital at Southwoods, Boardman, OH, USA, Philips Ultrasound, Bothell, WA, USA, General Electric, Milwaukee, WI, USA, Toshiba Medical Research Institute, Redmond, WA, USA, Massachusetts General Hospital, Boston, MA, USA, Samsung Medison, Seoul, South Korea, Zonare Medical Systems, Mountain View, CA, USA, The Cleveland Clinic, Cleveland, OH, USA, University of Wisconsin, Madison, WI, USA SuperSonic Imagine, Aix-En-Provence, France

Echosens, Paris, France Hitachi Healthcare, Seattle, WA, USA

Appendix B: Background Information

Appendix C: Conventions and Definitions

Appendix D: Model-specific Instructions and Parameters

Formatted: Heading 1, None, Space Before: 0 pt, After: 0 pt

Formatted: Body Text

D.1 Canon

Canon Medical Systems (formerly Toshiba)

Manufacturer Name:

- Canon Medical Systems Corporation (formerly Toshiba Medical Systems Corporation)

Equipment Models:

1220

1225

1230

1240

1245

1250

- Aplio i-series (i600/i700/i800/i900)
- Aplio a-series (a450/a550/a)
- Aplio Platinum Series (300/400/500)
- Xario 200 Platinum Series

Software Versions:

- Aplio i700/800/900 V1.1 or later
- Aplio i600 V2.0 or later
- Aplio a450/a550/a V1.0 or later
- Aplio 400/500 V6.0 or later
- Aplio 300 V6.7 or later
- Xario 200 V6.0 or later

1235 Transducer(s):

Transducer	Aplio i700/i800/i900	Aplio i600	Aplio a450/a550/a	Aplio 300/400/500	Xario 200
PVI-475BX	х				
PVI-475BT	Х	Х			
PVI-574BX	Х				
PVT-375BT	Х	Х	х	Х	
PVT-375SC	Х	Х	х	х	
PVT-475BT			х	Х	
PVT-574BT	Х	Х	х		
PVU-375BT					Х

Acquisition Procedures:

[See specifications in Profile Section 3.6, 3.8, & 3.10]

- Patient fasted minimum 4- 6 hours (including alcohol)
- Patient lying supine or slight left lateral decubitus position with the right arm behind the head.
- Normal gentle breathing or mid-expiration breath hold, as needed.
- Intercostal acoustic window with minimal rib shadowing and keeping the liver capsule parallel to the transducer surface; optimizing visualization of liver tissue.
- Select an area of the right lobe of the liver parenchyma free of the following structures:
 - Portal Trunk; Vessels; Visible Fibrous Bands
- Shear wave acquisition ROI:
 - o ROI size: approximately 3 cm in lateral direction and 3 cm in axial direction.
 - $\circ\quad$ Position acquisition ROI at least 1 cm below the liver surface.
 - Shear wave measurement ROI:
 - o A circular measurement ROI with a diameter of 1 cm is recommended.
 - Place measurement ROI in region of the shear wave speed /elasticity display that is homogenous and without defect.

Formatted: Heading 2, None, Space Before: 0 pt, Don't keep with next, Don't keep lines together

1255

1260

1265

SWS Profile FINAL REVISION FOR CONSENSUS STATUS VOTE-KOD20201221 bsg final review in process.docxSWS Profile FINAL REVISION FOR CONSENSUS STATUS VOTE-KOD20201221

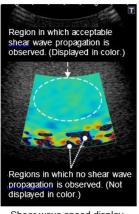
- o The Propagation map displays can be used for additional guidance on the placement of the measurement ROI (see below). The measurement ROI should be placed in a region where smooth, parallel contour lines are observed in the Propagation display.
- Repeat at least 5 measurements from the same window in the right lobe of the liver.

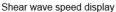
Outlier Identification specifications and instructions for use:

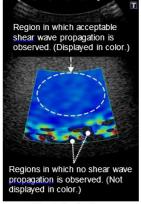
The following shear wave display maps are available:

N4 T	Diaglass	Description
Map Type	Display	Description
Speed	Shear wave speed display (m/s)*1	The stiffness distribution for the scanned
Elasticity	Elasticity display (kPa)*1	plane can be observed.
Propagation	Propagation display*2	The shear wave arrival time is presented as contour lines. (The wavefront of the shear wave is displayed at regular time intervals.)
Dispersion	Frequency dispersion display*1	The change in shear wave speed between frequencies is represented (dispersion slope) in color.
Variance	Variance display*1	Minor distortions in shear wave arrival times are represented in color.

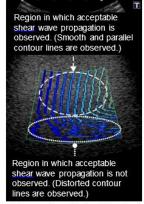
- *1: Regions in which no shear wave propagation is observed or acceptable shear wave propagation is not observed are not displayed in color.
- *2: Distorted contour lines are displayed for regions where no shear wave propagation is observed or where acceptable shear wave propagation is not observed.
- The region in which the desired shear wave propagation is observed can be confirmed by using the propagation display together with the shear wave speed display or elasticity display.







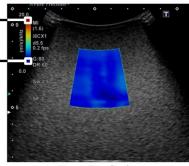
Elasticity display



Propagation display (Contour)

Colors near the top of the color bar indicate greater change in shear wave speed with changes in frequency.

Colors near the bottom of the color bar indicate less change in shear wave speed with changes in frequency.



Dispersion display

The mean, median, standard deviation, and IQR from multiple shear wave measurements can be displayed on a worksheet report page (up to 14 measurements). Individual measurements (i.e. outliers) can be excluded from the calculation of these statistical values as selected by the user.

Formatted: Body Text, Left

D.2 ESAOTE

1270

Esaote

Manufacturer Name:

Esaote S.p.A

Equipment Model

- MyLab Nine
- -•_MyLab X8
- MyLab Eight
- MyLab Twice

Formatted: Heading 2

Formatted: Font: Bold

Formatted: None, Space Before: 0 pt, Line spacing: single, No widow/orphan control, Don't keep with next, Don't keep lines together, Hyphenate, Don't adjust space between Latin and Asian text, Font Alignment: Auto

Formatted: Strong, English (United States)

Formatted: None, Space Before: 0 pt, Line spacing: single, No widow/orphan control, Don't keep with next, Don't keep lines together, Hyphenate, Don't adjust space between Latin and Asian text, Font Alignment: Auto

Software Versiones:

- -• MyLab 9 F070101 or later
- MyLab X8 version F080101 or later
- MyLab Twice release 10 or later
- - MyLab Eight release 11 or later

Formatted: Font: Bold

Formatted: None, Space Before: 0 pt, Line spacing: single, No widow/orphan control, Don't keep with next, Don't keep lines together, Hyphenate, Don't adjust space between Latin and Asian text, Font Alignment: Auto

Transducer(s) to be used

- C 1-8 with MyLab 9, MyLab X8 and MyLab 8
- L 4-15 with MyLab 9, MyLab X8
- L 3-11 with MyLab 9, MyLab X8
- CA541 with MyLab Twice

Formatted: Font: Bold

Formatted: None, Space Before: 0 pt, Line spacing: single, No widow/orphan control, Don't keep with next, Don't keep lines together, Hyphenate, Don't adjust space between Latin and Asian text, Font Alignment: Auto

1295

1285

Acquisition Procedure:

1. Instructions

1300

1305

1310

1315

1320

1325

1330

a. Scanning Instructions

- Recommended fasting of 4 -6 hours

- Right intercostal access has to be used, with the patient in the dorsal decubitus position, examining the right lobe of the liver (VI/VII segments) .by using the Convex array
- Put the right arm of the patient behind his/her head in order to maximize the intercostal space.
- The coupling between probe and liver has to be complete (the whole echo image has to be properly visible) - a correct amount of gel has to be used. Dark areas of the echo image have to be avoided.
- A correct pressure has to be applied, in order to be stable and to be properly coupled with the skin over the liver - the pressure shouldn't be not excessive in order to not compress the liver.
- No respiration during the acquisition, the patient should be asked to stop breathing just for few seconds in neutral respiratory phase.

b. ROI Positioning

- The ROI has to be positioned in an area free of vessels, bile ducts or nodules. It is recommended to check also the adjacent planes, not only the one of the ROI.
- The ROI should be positioned about 1 cm below the Glisson capsule to avoid reverberation artefacts. The optimized depths are between 3 cm and 5 cm.

c. ROI Size

- Point Shear Wave ~ 1.0cm x 1.0 cm
- 2D Shear Wave ~ 2 x 2.5 cm
- d. Number of measurements
 - Point Shear Wave 10 measurements or more
 - 2D Shear Wave 5 measurements or more

2. Pitfalls

- Low echogenicity and thick abdominal wall could make weak shear waves
- Modification of the acquisition liver window
- ROI axis not perpendicular to the liver capsule
- Reverberations could generate artefacts
- Some liver diseases may affect the stiffness assessment with SWE technique

Outlier Identification specifications and instruction for use:

Outliers are excluded based on a statistical signal analysis

The users have the possibility to discard some unreliable measurements and proceed to a new acquisition.

Formatted: Font: Bold

Formatted: None, Space Before: 0 pt, Line spacing: single, No widow/orphan control, Don't keep with next, Don't keep lines together, Hyphenate, Don't adjust space between Latin and Asian text, Font Alignment: Auto

Formatted: Font: Bold

Formatted: None, Space Before: 0 pt, After: 0 pt, Line spacing: single, No bullets or numbering, No widow/orphan control, Don't keep with next, Don't keep lines together, Hyphenate, Don't adjust space between Latin and Asian text, Font Alignment: Auto

Formatted: No bullets or numbering

Formatted: Font: Bold

Formatted: Normal, None, Space Before: 0 pt, Line spacing: single, No bullets or numbering, Don't keep with next, Don't keep lines together, Hyphenate, Font Alignment: Auto

In pSWE stiffness assessment, a quality index is indicated side the measurement with a capital letter H for High, M for Medium and L for Low giving some indication to the user about the reliability of the measurement.

In 2D SWE stiffness assessment, a reliability color map is available, indicating to the user, the areas were the measurement values are more stable and affordable.

Ultrasound System	No fibrosis (F0 – F1)	Moderate fibrosis (F 2- F3)	Severe Fibrosis (> F4)
MyLab 9 / X8			
MyLab Twice / Eight			

D.3 General Electric

<u>GE</u>

Manufacturer Name: GE Healthcare

Equipment Model: LOGIQ E9, LOGIQ S8

Software Version: R5 and higher on LOGIQ E9, R3 and higher on LOGIQ S8

Transducer(s) to be used: C1-6-D, 9L-D

Acquisition Procedures:

1. Instructions

 a. ROI positioning: Place Top of Shear Wave box 1-2cm below liver capsule with middle of the Shear wave box between 3-6cm

b. Measurement ROI size: Default measurement caliper size is recommended (Size = 1.25 cm diameter)

c. Number of measurements: 10 measurements

2. Pitfalls: Avoid rib shadows and vessels within the SWE ROI

Outlier Identification specifications and instructions for use:

Scanning Technique for best Shear Wave Results:

- Fasting 4-6 hours
- Patient in supine position
- Elevate Right arm above head
- Scan intercostally with enough pressure to maintain stable contact
- Take measurements in Segment 7 and/or 8 of the liver
- Place Top of Shear Wave box 1-2cm below liver capsule with
- middle of the Shear wave box between 3-6cm for best results
 - o Avoid rib shadows
 - o Avoid vessels in the Shear Wave region of interest
- Obtain measurement on suspended breath hold, not inspiration
- Acquire at least 10 measurements using caliper tool

Formatted: Heading 2, None, Space Before: 0 pt, Don't keep with next, Don't keep lines together

1350

1340

1355

1360

1365

1370

1380

Locations with inaccurate measurement are not displayed in the SWE color image, and do not contribute to the quantitative measurement.

1385

1390

Best Practice Tips for Acquisition:

 Ensure good probe contact with patient and optimize imaging window to get best possible B-mode image quality before starting SWE acquisition

✓ Place ROI in shadow-free region

- √ Place ROI near center of image (laterally) if possible
- ✓ Place ROI in region free of vessels and 1-2cm below liver capsule
- 1395 Best Practice Tips for Measurement:
 - √ Take measurement when >50% of ROI has color-fill with default gain
 - ✓ Take measurement on region with uniform color-fill and without obvious artifact like vertical stripes caused by probe movement during SWE acquisition

1400

GE Healthcare

LOGIQ E9 Shear Wave Elastography

Liver Fibrosis Staging

Liver Fibrosis Staging	Metavir Score	kPa	m/s
Normal – Mild	F1	5.48 kPa – 8.29 kPa	1.35 m/s - 1.66 m/s
Mild – Moderate	F2	8.29 kPa – 9.40 kPa	1.66 m/s - 1.77 m/s
Moderate – Severe	F3	9.40 kPa – 11.9 kPa	1.77 m/s - 1.99 m/s
Cirrhosis	F4	> 11.9 kPa	> 1.99 m/s

A GE study has demonstrated that LOGIQ" E9 Shear Wave Elastography is a robust technique and capable of evaluating stiffness changes in the liver associated with fibrosis. Although a limited number of subjects were evaluated at the hospital in this study, liver stiffness measurements were shown to be useful for discriminating different stages of fibrosis. It is important to note that of small criminating different stages of fibrosis are evaluated in this study, and that a mis of disease etiologies were present. Therefore, the values shown may not be directly applicable to other patient populations. Data was ocquired using LOGIQ E9 R5.1.0 equivalent software and the C1-6-0 probe. For detatled information, please see the LOGIQ E9 short Wave Eligitography white paper.



GE, the GE Monogram and LOGIQ are trademarks of the General Electric Company

Minimum ROI Size -

1105

D.4 Hitachi

Formatted: Heading 2, None, Space Before: 0 pt, Don't keep with next, Don't keep lines together

Hitachi

Manufacturer Name:

Hitachi, Ltd.

1410

1425

1430

1440

Equipment Model:

- ARIETTA 850
- ARIETTA 70
- HI VISION Ascendus

Software Version:

- ARIETTA 850 Ver.1 or later
- ARIETTA 70 Ver.3 or later
- HI VISION Ascendus Step 4 or later

1420 Transducer(s) to be used:

- C252 and C251 with ARIETTA 850
- C251 with ARIETTA 70
- C715 with HI VISION Ascendus

Acquisition Procedures:

1. Instructions

a. ROI positioning

Same as QIBA profile. See below.

- Position the ROI at least 2cm deep to the liver capsule and less than 6.5 cm from the transducer face.
- Position the ROI away from discrete structures such as liver margin, nodules, portal triads or hepatic veins for acquisition of SWS estimates.
- Position the ROI near the center of the image in the lateral direction and away from the right or left image margins.

1435 b. Measurement ROI size

Fixed ROI size with 10mm width and 15mm depth.

c. Number of measurements

10 measurements

2. Pitfalls

Under the following conditions, the generation and/or detection of shear wave will be insufficient.

- Low echogenicity
- Thick abdominal wall
- Liver capsule non parallel to the abdominal wall or not perpendicular to beams
- Place the ROI on rib shadows and/or near the liver capsule
- 1445 Large body motion by respiration

Outlier Identification specifications and instructions for use:

- Hitachi has a reliability index (VsN). Outliers are excluded using specific Vs range and/or shear wave signal quality. If VsN equals 0%, all data are outliers and error message is displayed.
- 1450 IQR/Median is displayed. Users can exclude individual measurements and the statistical values (i.e. IQR/Median) are automatically updated. (only for ARIETTA 850)

D.5 Philips

1460

1465

1475

1480

Philips

1455 Manufacturer Name: Philips

Equipment Model: EPIQ

Software Version: Evolution 3.0

Software version: Evolution 5.0

Transducer(s) to be used: C5-1 Curvilinear Transducer

Acquisition Procedures: Please refer to Philips "Quick Guide EPIQ Series ElastQ Imaging" for complete instruction

3.1. Instructions

ROI positioning

- i. Ensure good transducer contact
- Before starting shear wave elastography, always scan the region of interest in 2D mode to assess tissue consistency
 - Do not position the shear wave imaging region of interest (ROI) box over fetal tissue, tissue with gas pockets (lung, stomach, bowels), a bone tissue boundary, gallstones, metal, or the borders of the image.
 - Avoid rib shadow in the image, when possible.
 - Position the ElastQ Imaging ROI box in the center of the image.
 - Do not place the ElastQ Imaging ROI box on or near a rib shadow or liver capsule.
 - Place the top of the ROI box 1.0 to 1.5 cm below the liver capsule, to avoid reverberation artifacts
 - Do not place the circle caliper on a rib shadow, blood vessels
 - Position the circle caliper in the area of the ROI box that displays the majority of the uniform color
- ROI size
 - iii. ElastQ Imaging ROI: maximum size ~5cm (height) x 7 cm (width)
 - iv. Making stiffness measurement and calculations
 - 1. Default circle caliper size: dimeter 1cm
 - User has the option to calculate the average stiffness in the entire ElastQ Imaging ROI
 - 3. User has the option to make single point measurements in the ROI
 - 4. Stiffness measurement is also available for areas defined by the user in the form of ellipse and continuous trace
- b. Number of measurements
 - Take a minimum of 8 to 10 liver stiffness measurements

-2. Pitfalls

Formatted: Heading 2, None, Space Before: 0 pt, Don't keep with next, Don't keep lines together

Formatted: Numbered + Level: 1 + Numbering Style: 1, 2, 3, ... + Start at: 1 + Alignment: Left + Aligned at: 0.25" + Indent at: 0.5"

Formatted: Numbered + Level: 2 + Numbering Style: a, b, c, ... + Start at: 1 + Alignment: Left + Aligned at: 0.75" + Indent at: 1"

 $\begin{tabular}{ll} Formatted: Numbered + Level: 3 + Numbering Style: i, ii, iii, ... + Start at: 1 + Alignment: Right + Aligned at: 1.38" + Indent at: 1.5" \end{tabular}$

 $\begin{tabular}{ll} Formatted: Numbered + Level: $3 + Numbering Style: i, ii, iii, ... + Start at: $1 + Alignment: Right + Aligned at: $1.38" + Indent at: $1.5" \end{tabular}$

Formatted: Numbered + Level: 4 + Numbering Style: 1, 2, 3, ... + Start at: 1 + Alignment: Left + Aligned at: 1.75" + Indent at: 2"

Formatted: Numbered + Level: 2 + Numbering Style: a, b, c, ... + Start at: 1 + Alignment: Left + Aligned at: 0.75" + Indent at: 1"

Formatted: Numbered + Level: 1 + Numbering Style: 1, 2, 3, ... + Start at: 1 + Alignment: Left + Aligned at: 0.25" + Indent at: 0.5"

ı

Outlier Identification specifications and instructions for use:

To ensure high quality stiffness measurement, a concurrent real-time confidence map that combines multiple image quality metrics is also available along with the stiffness image. Outliers in stiffness measurement are automatically detected and excluded from subsequent quantification and statistical analysis. In addition, users are provided with the ratio of stiffness interquartile range (IQR) to median as a measure of variability for further measurement quality control.

D.6 Samsung

Samsung

1505 Manufacturer Name:

Samsung Medison Co., Ltd.

Equipment Model:

- RS80A

1510 - RS85

Software Version:

- RS80A v2.0 or later

- RS85 v1.0 or later

1515

1520

1530

1535

1500

Transducer(s) to be used:

- RS80A

CA1-7A

LA2-9A

- RS85

CA1-7A LA2-9A

1525 Acquisition Procedures:

- Patient position
 - Supine / oblique left decubitus position is recommended
 - The right arm would better be elevated to make the intercostal spaces wider
 - Scan while patients' holding a normal breath (If not possible, ask the patient to breath as shallowly as possible)
 - Prolonged breath holding should be avoided
 - Patients should not move during the measurements
- · Liver segment
 - Right hepatic lobe (between 5 and 8 segment from the right intercostal space) is recommended.
 - Avoid the left hepatic lobe because the measurement is affected by cardiac movements.
 - Segment 4 of the liver is sensitive to the motion artifact. There are more chances of the failure of measurement.

Formatted: Heading 2, None, Space Before: 0 pt, Don't keep with next, Don't keep lines together

ROI positioning

- Position the ROI Box neat the homogeneous region
- Position the ROI Box at the suspected lesion without obscuring vessels.
- The ROI must be positioned at least 1.5 cm below the liver capsule.
- To obtain a stable measurements, position the ROI on the same locations and repeat the measurements
- The depth of ROI is recommended 6cm or less (if the depth is more than 6cm, the result may not be reliable). The bottommost depth should be less than 7cm.
- ROI is recommended to be positioned near the center line.
- 1550 ROI size

1545

1555

1560

1565

1570

1575

1580

1585

Point shear wave: 1.0cm X 1.0cm S shear wave: 2.5cm X 3.0cm

Number of measurements:

10 times or more

Scanning instruction

- After checking the probe and the application, start a scan.
- When you get the desired image, tap the S-Shearwave Imaging on the touch screen.
- Use the track ball to move to a desired ROI measurement position.
- Press the **Freeze** button on the control panel, and then the **Elasticity Measure** button on the touch screen.
- Use the trackball to move to a desired ROI measurement position within the Elasticity Image ROI.
- Pressing the **Set** button will display elasticity statistics within the Measure ROI, and save the value.
- A maximum of four Sites can be specified, and a maximum of ten Measure ROIs can be specified per Site

2. Pitfalls

(1) Weak shear waves

Avoid the ROI in the region where B mode image is too dark. This can induce insufficient tissue displacement by the push pulse to measure shear wave speed. Severe attenuation in tissue/muscle layer, shadowing by the ribs, defocusing of push pulses, loose probe contact can be the reasons.

(2) Reverberation

Obese patients typically have a thick fat/muscle layer and produce reverberations deep in the liver. The reverberations distort scanning pulses to produce erroneous shear wave speed readings. To reduce reverberation artifact, depth of ROI should be at least twice the thickness of the muscle/fat layer, and the probe angle should be chosen to minimize reverberation between strong parallel reflectors. Measurements deemed contaminated by reverberation will display RMI (Reliability Measurement Index) value of 0.0.

(4) Reflections

Abrupt changes at the tissue/ tumor boundary produces reflections that may alter the observed propagation of shear waves. Typically this alteration may produce higher stiffness at the periphery of stiff tumors.

Outlier Identification specifications and instructions for use:

- Reliable Measurement Index (RMI) shows how reliable the measurement is and it is more reliable if the value gets closer to the maximum value of 1. (If RMI is 0.4 or higher, it is considered as very reliable.)
- It is recommended that this process is repeated more than 10 times.
- Auto profiling automatically removes outliers with RMI less than 0.4 or too far away from the
 calculated median value. The process automatically repeats itself until the number of remaining
 measurements is bigger than 5 and IQR/MED is less than 0.3.
- Following table is the chart provided by Samsung for liver fibrosis staging.

Liver Grading	Normal – Mild	Mild	Moderate – Severe	Severe
METAVIR Scoring	F0 - F1	F1 - F2	F3 - F4	F4
Кра	2 - 5.4kpa	5.4 - 7.4kpa	7.4 - 11.6kpa	11.6 – 21.4kpa
m/s	0.81 - 1.34 m/s	1.34 - 1.57 m/s	1.57 - 1.97 m/s	1.97 - 2.7 m/s

1600

1590

1595

D.7 Siemens

Siemens

Manufacturer Name:

Siemens Medical Solutions, USA, Inc.

1605

Equipment Model:

ACUSON Sequoia ACUSON S2000, S3000

1610 Software Version:

ACUSON Sequoia: VA10A or later ACUSON Redwood ACUSON Juniper VA10A or later ACUSON S2000, S3000: VC20A or later

1615

Transducer(s) to be used:

ACUSON Sequoia: 5C1, DAX, 4V1, 10L4 ACUSON S2000, S3000: 6C1HD, 4C1, 4V1

1620 Acquisition Procedures:

Follow cross-vendor recommendations in Profile

Best Practice Techniques

Formatted: None, Space Before: 0 pt, No widow/orphan control, Don't keep with next, Don't keep lines together, Don't adjust space between Latin and Asian text, Don't adjust space between Asian text and numbers

Formatted: Heading 2, None, Space Before: 0 pt, Don't keep with next, Don't keep lines together

- Patient has fasted for a minimum of 4-6 hours
- Position patient supine or slight (30°) left lateral decubitus position with right arm raised above head
- Scan with the transducer parallel to ribs and in an intercostal space in the right lobe of the liver (segments 5 or 8)
- Optimize B-mode image so liver parenchyma is bright and large vessels, bile ducts and rib shadows are avoided

Activate Virtual Touch from the Abdomen exam preset

- ACUSON Seguoia
 - Press VT button on control panel
 - Select pSWE for point Shear Wave Elastography or SWE for 2D Shear Wave Elastography
- ACUSON S2000 and S3000 systems
 - o Press E button on control panel
 - o Select VTQ (Virtual Touch Quantification) on the touch screen

Position the Region of Interest (ROI)

- Position the ROI between 3–6 cm deep and at least 1–2 cm below liver capsule
- To position the ROI, roll the trackball
- In SWE, if desired, press Set key and roll trackball to resize the ROI

Perform Acquisition

1625

1630

1635

1640

1645

1650

1655

1660

1665

- Perform acquisition during suspended respiration, neither deep inspiration nor expiration;
 patient may resume normal breathing after audible "beep" is heard
- To begin acquisition, press Update on the control panel; an audible tone indicates when the
 acquisition ends

Store Measurement Result

- ACUSON Sequoia pSWE
 - The Liver Site 1 label is automatically selected; change the measurement label if desired on the touch screen
 - Press Image to store an image, or Press right or left Set key to store the measurement without storing an image
- ACUSON Seguoia SWE
 - o Press Caliper to enter measurement workflow
 - o Select desired measurement label on the touch screen
 - o Roll the trackball to position measurement caliper
 - $\circ\quad \mbox{If needed, rotate \sc ROI Diameter}$ control to resize measurement caliper
 - Press Image to store an image, or Press right or left Set key to store the measurement without storing an image
- ACUSON S2000 and S3000 systems
 - o Select desired measurement label on the touch screen
 - Press Image to store an image, or Press right or left Set key to store the measurement without storing an image

1670 Study Conclusion

1675

1680

1685

1690

1695

1705

1710

- Acquire and store 10 total valid measurements at the same imaging location
- Select Report on left side of touch screen
- Ensure IQR/Median is less than 0.3

Outlier Identification specifications and instructions for use:

The ACUSON Sequoia pSWE and ACUSON S2000/S3000 VTQ measurements display X.XX m/s when the threshold for measurement quality was not reached. Users should discard those measurements and repeat the acquisition until the system displays a numerical value.

The ACUSON Sequoia SWE image provides a Quality map to confirm that shear wave generation was adequate and identify regions of the shear wave image where shear wave velocity or elasticity estimations may be incorrect due to poor shear wave signal quality. To view the quality map, rotate the **Shear Wave** control from **Velocity** to **Quality**. The measurement caliper should be placed in regions of the highest visible quality and near the center of the acquisition ROI.

Ensure overall IQR/Median ratio for acquired measurements is less than 0.3 as provided in the patient report.

D.8 Supersonic Imagine

Supersonic Imagine

Manufacturer Name:

SuperSonic Imagine

Equipment Model:

Aixplorer®

Software Version:

Most recent version released: V11.1.1

1700 Transducer(s) to be used:

SC6-1 from version V3.0 to V11.1 XC6-1 from version V9.3.1 to V11.1

1. Number of values averaged for each pixel in the color image:

The number of values averaged for each pixel depends on imaging parameters. Operator-adjustable parameters are:

- Map persistence: the operator can change the number of frames averaged from 1 to 3
- Map smoothing: this spatial filtering uses sizeable 2D areas to calculate and display one pixel value on the color image. The size of this 2D area ranges from 3x3 to 19x19, the default size being 11x11 values.

 $\begin{tabular}{ll} \textbf{Formatted:} & \textbf{Heading 2, None, Space Before: 0 pt, Don't keep} \\ \textbf{with next, Don't keep lines together} \\ \end{tabular}$

2. Average Variance per pixel:

1715

1720

1725

Acquisition Procedures:

5-3. Instructions – Pre-requisites

Optimal acoustic window should be found, assessed on grayscale imaging, prior to engaging SWE™ Mode by appropriate patient's positioning and proper probe holding.

a. Patient's positioning:

- Patient is placed in supine position to favor acquisitions and measurements on the right liver lobe
- ii. Right arm in maximum abduction
- iii. Change to left lateral decubitus only when necessary

b. Probe holding

- Acquisitions and measurements should be preferably performed on the right liver lobe via intercostal access
- ii. Probe should be placed parallel to the intercostal space to avoid shadowing from the ribs
- iii. Probe should be held orthogonal to the liver capsule to maximize ultrasound transmission, shear wave generation and shear wave propagation recording
- iv. When scanning intercostally, extra pressure should be applied on the probe to:
 - 1. Enlarge intercostal space
 - 2. Decrease subcutaneous fat thickness
 - 3. Ensure optimal contact between the probe and patient's thoracic wall

Image stabilization must be achieved before freezing the image

- Motion from the operator and the probe must be avoided
- Appropriate patient's normal breath hold for 3-4 seconds must be achieved

6.4. Instructions – SWE Acquisition

- a. ROI positioning
 - i. The colored SWE Box should be positioned:
 - 1. At a minimum depth of 2 cm from the liver capsule,
 - 2. Ideally enabling measurements between 3 to 7 cm in depth,
 - 3. Over morphologically homogeneous, vessel-free, liver parenchyma
 - ii. The Q-Box™ ROI should be placed:
 - In the central area of the SWE Box; borders of the SWE Box should be avoided.
 - 2. Over an area of relative homogeneous elasticity, avoiding recognizable artifacts
 - From V10.0, use the stability index to reject any location for which the SI would be < 90%

b. ROI size [See specifications in Profile Section 3.10.2]

The SWE default settings have been optimized for the assessment of liver fibrosis. Default settings should be used first, and adjusted only when necessary.

i. The default size of the SWE Box is 2 cm in height and 3 cm in width.

1730

1735

1745

1740

1750

- ii. The default size of the Q-Box ROI may be enlarged to encompass the largest quantification area possible, while ensuring no vessels, no parenchyma heterogeneity and no artifact are included.
- c. Number of measurements
 - Because of the large amount of SWS measurements included in 1 Q-Box ROI, a total number of 3 valid measurements* performed on 3 independent valid acquisitions are recommended.
 - ii. The average value of 3 valid measurements* can be considered as the estimation of SWS for a given patient.
- * Invalid measurements obtained with XC6-1 probe from V10.0 must be defined as measurements obtained with a Stability Index < 90%. Invalid measurements obtained with SC6-1, regardless of software version, or XC6-1 probe before V10.0 software release must be defined as measurements obtained from unstable SWE map evaluated as non-reliable acquisitions.
 - 7.5. Pitfalls
 - a. Usual limitations of conventional ultrasound apply to SWE™ mode
 - i. Narrow intercostal spaces,
 - ii. Thick layer of fat,
 - iii. Highly attenuating medium, low echogenicity
 - b. Several clinical factors influence liver stiffness measurements, and should be considered when assessing liver SWS:
 - i. Respiration, deep breath
 - ii. Central venous pressure
 - iii. Intrahepatic cholestasis
 - iv. Hepatic necro-inflammatory activity
 - v. Peliosis hepatitis
 - vi. Hepatic vein thrombosis
 - vii. Congestive hepatopathy

Outlier Identification specifications and instructions for use:

Acquisitions that are performed in sub-optimal acoustic conditions should be discarded and may present high risk for generating unreliable SWS measurements and outliers. Such sub-optimal conditions are:

- Lack of acoustic coupling and reduced acoustic transmission,
- Unstabilized grayscale and/or SWS image, particularly due to lack of breath control,
- Large highly attenuating or hypoechoic areas, especially from ribs shadowing.

Acquisitions that are unstable as illustrated by SWS maps being highly unstable over time, or with varying color patterns, should be considered as unreliable acquisitions and should be discarded. Such unreliable acquisitions may present high risk for generating unreliable SWS measurements and outliers.

Unreliable measurements and outliers should be expected in areas close to major hepatic vessels, focal liver nodules, and any visible structure on grayscale ultrasound that looks different from liver parenchyma.

Ultrasound	No Fibrosis or	Moderate Fibrosis (METAVIR F2 and	Severe

1765

1760

1770

1775

1780

1785

1790

1795

System	Minimal Fibrosis (METAVIR F0-F1)	F3)	Fibrosis/Cirrhosis (METAVIR F3 – F4)
System A			

Appendix E: Primary Checklists for Profile Execution and Conformance

See the Microsoft Excel file in this folder for the checklists. A link is given below: Appendix E - clean version for public.xlsx

Appendix F: Secondary Checklists for Profile Execution and Conformance

Appendix G: Patient information sheet and Data collection-

Standardized case report form for Elastography studies

Subject ID: _____

1805

1810

1825

1830

1835

1820 A. Patient Demographics

1. Gender M F

2. Age (years)
3. Patient Fasting Yes No Hours
4. Height (inches)
5. Weight (pounds)

B. Clinical Data

1. Confounders:

a. Right Heart Failure
b. Steatosis (on US)
c. Elevated markers for inflammation
Yes No
Yes No

2. Reason for Exam

☐ Elevated LFT's?

Formatted: Heading 1, None, Space Before: 0 pt, After: 0 pt

Commented [OK113]: KOD Editorial

The profile will be posted on the Wiki and then the pdf file will be in the hands of users so the instruction should allow one of those users to get to the Excel file.

Commented [OK114]: KOD Editorial

It's not clear what "Primary" and "Secondary" mean. If they are reexpressing "Conformance" and "Execution" then I'd suggest dropping the Primary/Secondary to reduce confusion.

Formatted: Font: Not Bold

Formatted: None, Space Before: 0 pt, After: 0 pt, No widow/orphan control, Don't adjust space between Latin and Asian text, Don't adjust space between Asian text and numbers

Formatted: Heading 1, None, Space Before: 0 pt, After: 0 pt

Formatted: Body Text, Left, Line spacing: single

☐ F/U Kno	wn Hx of Liver		Diagnos	stic for Fib	rosis	
□нс∨			☐ ?NA	\SH		
□ нв∨			☐ ?AII	Н		
☐ HIV +	HCV		☐ ?Dr	ug Toxicity	у	
☐ AIH _		_				
☐ Alcoh	olic Liver Disease					
☐ Healt	hy volunteer					
☐ Other						
i. i ii. , iii. , iv. , v.	kers (If evaluated) Platelets (x10 ⁹ /L) AST (IU/L) ALT (IU/L) Alkaline phosphata Total Bilirubin (µ m alculations from ab 1. AST/ALT ra 2. APRI 3. Fib-4	ol/L) ove values:			- - - -	
Optional FibroSURE						
SWS Examin Depth of liver	ation capsule from skin				_	
Measurement	Depth of	SWS	C	comments		

Measurement No.	Depth of measurement from capsule (cm)	SWS (m/sec)	Comments
1			
2			
3			
4			
5			
6			

7		
8		
9		
10		

IQR/Median Value:

1865

References (Steatosis has no effect):

- Yoneda M, Mawatari H, Fujita K, Endo H, Nozaki Y, Yonemitsu K, et al. Noninvasive assessment of liver fibrosis by measurement of stiffness in patients with nonalcoholic fatty liver disease (NAFLD). Dig Liver Dis [Internet]. 2008 May; 40(5):371–8. Available from:http://eutils.ncbi.nlm.nih.gov/entrez/eutils/elink.fcgi?dbfrom=pubmed&id=180830 83&retmode=ref&cmd=prlinks
- Friedrich-Rust M, Wunder K, Kriener S, Sotoudeh F, Richter S, Bojunga J, et al. Liver fibrosis in viral hepatitis: noninvasive assessment with acoustic radiation force impulse imaging versus transient elastography. Radiology. 2009 Aug;252(2):595–604.
- Lupsor M, Badea R, Stefanescu H, Sparchez Z, Branda H, Serban A, et al. Performance of a new elastographic method (ARFI technology) compared to unidimensional transient elastography in the noninvasive assessment of chronic hepatitis C. Preliminary results. J Gastrointestin Liver Dis. 2009 Sep;18(3):303–10.
- Fierbinteanu-Braticevici C, Andronescu D, Usvat R, Cretoiu D, Baicus C, Marinoschi G. Acoustic radiation force imaging sonoelastography for noninvasive staging of liver fibrosis. World J Gastroenterol [Internet]. 2009 ed. 2009 Nov 28;15(44):5525–32. Availablefrom:http://eutils.ncbi.nlm.nih.gov/entrez/eutils/elink.fcgi?dbfrom=pubmed&id=19938190&retmode=ref&cmd=prlinks
- Bota S, Sporea I, Sirli R, Popescu A, Danila M, Sendroiu M. Factors that influence the correlation of acoustic radiation force impulse (ARFI), elastography with liver fibrosis. Medical ultrasonography. 2011 Jun;13(2):135–40.
- Rifai K, Cornberg J, Mederacke I, Bahr MJ, Wedemeyer H, Malinski P, et al. Clinical feasibility of liver elastography by acoustic radiation force impulse imaging (ARFI). Dig Liver Dis [Internet]. 2011 Jun;43(6):491–7. Available from: http://linkinghub.elsevier.com/retrieve/pii/S1590865811000752
- Palmeri ML, Wang MH, Rouze NC, Abdelmalek MF, Guy CD, Moser B, et al. Noninvasive evaluation of hepatic fibrosis using acoustic radiation force-based shear stiffness in patients with nonalcoholic fatty liver disease. J Hepatol. 2011 Sep;55(3):666–72.
- 8. Motosugi U, Ichikawa T, Niitsuma Y, Araki T. Acoustic radiation force impulse elastography of the liver: can fat deposition in the liver affect the measurement of liver stiffness? Japanese journal of radiology. 2011 Sep 29;29(9):639–43.
- Ebinuma H, Saito H, Komuta M, Ojiro K, Wakabayashi K, Usui S, et al. Evaluation of liver fibrosis by transient elastography using acoustic radiation force impulse: comparison with Fibroscan((R)). J Gastroenterol. 2011 Oct;46(10):1238–48.
- 10. Rizzo L, Calvaruso V, Cacopardo B, Alessi N, Attanasio M, Petta S, et al. Comparison

Commented [OK115]: GUIDANCE:

Use standard manuscript format

Commented [OK116]: The use of EndNote seems to have blocked Word seeing anything after the References. Appendix A and the rest no longer show up in the Table of Contents. Not familiar enough with EndNote to know how to fix. The workaround would be to move all the Appendices to come before the References.

Formatted: Normal

- of transient elastography and acoustic radiation force impulse for non-invasive staging of liver fibrosis in patients with chronic hepatitis C. Am J Gastroenterol. 2011 Dec;106(12):2112–20.
- 11. Chen S-H, Li Y-F, Lai H-C, Kao J-T, Peng C-Y, Chuang P-H, et al. Effects of patient factors on noninvasive liver stiffness measurement using acoustic radiation force impulse elastography in patients with chronic hepatitis C. BMC Gastroenterology [Internet]. 2012;12(105):105. Available from: http://eutils.ncbi.nlm.nih.gov/entrez/eutils/elink.fcgi?dbfrom=pubmed&id=22877310&re tmode=ref&cmd=prlinks
- 12. Guzmán-Aroca F, Frutos-Bernal MD, Bas A, Luján-Mompeán JA, Reus M, Berná-Serna J de D, et al. Detection of non-alcoholic steatohepatitis in patients with morbid obesity before bariatric surgery: preliminary evaluation with acoustic radiation force impulse imaging. Eur Radiol. 2012 Nov;22(11):2525–32.
- 13. Ferraioli G, Tinelli C, Dal Bello B, Zicchetti M, Filice G, Filice C, et al. Accuracy of real-time shear wave elastography for assessing liver fibrosis in chronic hepatitis C: a pilot study. Hepatology. 2012 Dec;56(6):2125–33.
- 14. Bota S, Sporea I, Sirli R, Popescu A, Jurchis A. Factors which influence the accuracy of acoustic radiation force impulse (ARFI) elastography for the diagnosis of liver fibrosis in patients with chronic hepatitis C. Ultrasound Med Biol. 2013 Mar;39(3):407– 12.
- 15. Friedrich-Rust M, Buggisch P, de Knegt RJ, Dries V, Shi Y, Matschenz K, et al. Acoustic radiation force impulse imaging for non-invasive assessment of liver fibrosis in chronic hepatitis B. J Viral Hepat. 2013 Apr;20(4):240–7.
- 16. Poynard T, Munteanu M, Luckina E, Perazzo H, Ngo Y, Royer L, et al. Liver fibrosis evaluation using real-time shear wave elastography: applicability and diagnostic performance using methods without a gold standard. J Hepatol. 2013 May;58(5):928– 35.
- 17. Tomita H, Hoshino K, Fuchimoto Y, Ebinuma H, Ohkuma K, Tanami Y, et al. Acoustic radiation force impulse imaging for assessing graft fibrosis after pediatric living donor liver transplantation: A pilot study. Liver transplantation: official publication of the American Association for the Study of Liver Diseases and the International Liver Transplantation Society. 2013 Sep 21;19(11):1202–13.

References (Inflammation affects SWS):

- Friedrich-Rust M, Wunder K, Kriener S, Sotoudeh F, Richter S, Bojunga J, et al. Liver fibrosis in viral hepatitis: noninvasive assessment with acoustic radiation force impulse imaging versus transient elastography. Radiology. 2009 Aug;252(2):595–604.
- Lupsor M, Badea R, Stefanescu H, Sparchez Z, Branda H, Serban A, et al. Performance of a new elastographic method (ARFI technology) compared to unidimensional transient elastography in the noninvasive assessment of chronic hepatitis C. Preliminary results. J Gastrointestin Liver Dis. 2009 Sep;18(3):303–10.

- 3. Takahashi H, Ono N, Eguchi Y, Eguchi T, Kitajima Y, Kawaguchi Y, et al. Evaluation of acoustic radiation force impulse elastography for fibrosis staging of chronic liver disease: a pilot study. Liver Int. Blackwell Publishing Ltd; 2010 Apr;30(4):538–45.
- Rifai K, Cornberg J, Mederacke I, Bahr MJ, Wedemeyer H, Malinski P, et al. Clinical feasibility of liver elastography by acoustic radiation force impulse imaging (ARFI). Dig Liver Dis. 2011 Jun;43(6):491–7.
- Ebinuma H, Saito H, Komuta M, Ojiro K, Wakabayashi K, Usui S, et al. Evaluation of liver fibrosis by transient elastography using acoustic radiation force impulse: comparison with FibroScan(®). J Gastroenterol. 2011 Oct;46(10):1238–48.
- Chen S-H, Li Y-F, Lai H-C, Kao J-T, Peng C-Y, Chuang P-H, et al. Effects of patient factors on noninvasive liver stiffness measurement using acoustic radiation force impulse elastography in patients with chronic hepatitis C. BMC Gastroenterology. BioMed Central Ltd; 2012;12(1):105.
- 7. Yoon KT, Lim SM, Park JY, Kim DY, Ahn SH, Han K-H, et al. Liver stiffness measurement using acoustic radiation force impulse (ARFI) elastography and effect of necroinflammation. Dig Dis Sci. Springer US; 2012 Jun;57(6):1682–91.
- Guzmán-Aroca F, Frutos-Bernal MD, Bas A, Luján-Mompeán JA, Reus M, Berná-Serna J de D, et al. Detection of non-alcoholic steatohepatitis in patients with morbid obesity before bariatric surgery: preliminary evaluation with acoustic radiation force impulse imaging. Eur Radiol. Springer-Verlag; 2012 Nov;22(11):2525–32.
- Sporea I, Bota S, Peck-Radosavljevic M, Sirli R, Tanaka H, Iijima H, et al. Acoustic Radiation Force Impulse elastography for fibrosis evaluation in patients with chronic hepatitis C: an international multicenter study. Eur J Radiol. 2012 Dec;81(12):4112–8.
- 10. Potthoff A, Attia D, Pischke S, Kirschner J, Mederacke I, Wedemeyer H, et al. Influence of different frequencies and insertion depths on the diagnostic accuracy of liver elastography by acoustic radiation force impulse imaging (ARFI). Eur J Radiol. 2013 Aug;82(8):1207–12.
- 11. Bota S, Sporea I, Peck-Radosavljevic M, Sirli R, Tanaka H, Iijima H, et al. The influence of aminotransferase levels on liver stiffness assessed by Acoustic Radiation Force Impulse Elastography: a retrospective multicentre study. Dig Liver Dis. 2013 Sep;45(9):762–8.
- 12. Fierbinteanu-Braticevici C, Sporea I, Panaitescu E, Tribus L. Value of acoustic radiation force impulse imaging elastography for non-invasive evaluation of patients with nonalcoholic fatty liver disease. Ultrasound Med Biol. 2013 Nov;39(11):1942–50.
- 13. Takaki S, Kawakami Y, Miyaki D, Nakahara T, Naeshiro N, Murakami E, et al. Non-invasive liver fibrosis score calculated by combination of virtual touch tissue quantification and serum liver functional tests in chronic hepatitis C patients. Hepatol Res. 2014 Mar;44(3):280–7.
- 14. [Reference IEC 61391-2: Ultrasonics Pulse-echo scanners Part 2:

Measurement of maximum depth of penetration and local dynamic range. 2010, Int Electrotechnical Comm: Geneva.]

<Not sure how to do two TOC, so left this one out and made vendors Heading 2 so they appear in the overall TOC>

Formatted: Centered, Line spacing: Multiple 1.15 li