QIBA Profile:

Magnetic Resonance Elastography of the Liver

Stage: A. Initial Draft

July 6, 2017

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Change Log:

This table is a best-effort of the authors to summarize significant changes to the Profile.

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Date	Sections Affected	Summary of Change
12/2/2016	All	Added References
12/7/2016	4	Added details on proposed test-retest study for sites to demonstrate conformance with profile.
12/23/2016	All	Changed profile claim to a 19% change (revised from a 22% change)
12/23/2016	3.3	Added brief discussion on comparison of MRE and materials testing in phantoms and tissue to highlight complexity and explain the role of the volunteer test-retest conformance validation as opposed to a phantom study.
1/9/2017	2/3.3	Moved discussion of MRE phantom measurements and DMA testing to from the Periodic QA section to the end of the Claims discussion section.
1/9/2017	3.5.1	Changed fasting time from 3 to 4 hours.
1/9/2017	4.2	Clarified that the test-retest conformance study should also be performed in the case of significant hardware modifications.
5/5/2017	4.2	Revised wording regarding demonstration of conformance with the profile.

Open Issues:

The following issues are provided here to capture associated discussion, to focus the attention of reviewers on topics needing feedback, and to track them so they are ultimately resolved. In particular, comments on these issues are highly encouraged during the Public Comment stage.

Closed Issues:

The following issues have been considered closed by the biomarker committee. They are provided here to forestall discussion of issues that have already been raised and resolved, and to provide a record of the rationale behind the resolution.

Q. The longitudinal claim presented in this profile requires that the MRE stiffness measurements (magnitude of the complex shear modulus) have a linear relationship with true stiffness. Can this be confirmed with phantom testing? A. The working group noted that existing technology does not provide a way to fabricate elastography phantoms with stiffness values that are precisely defined in advance by the composition and process. Existing dynamic mechanical testing devices used in laboratories have significant limitations for estimating the complex shear modulus of semi-solid materials. Therefore, no currently-accepted test procedure can be recommended to confirm the assumption of linearity. However, based on the physical principles of the MRE measurement process and published comparisons with benchtop mechanical testing (refs), the working group concludes that linearity is a reasonable assumption at this time.
Q. Should the profile attempt to identify commercial suppliers of MRE phantoms in this first edition? A. At this time, commercial products are limited, have not been widely tested, and may only be available from some of the MRI OEM's. The draft profile describes the use of an MRE phantom to aid training and as an optional tool for generally confirming proper system operation (not to test accuracy). Accordingly, it may be appropriate to defer attempting identify commercial MRE phantoms to the second edition of the profile, when there may be more experience to confirm availability and usability.
Q. References/Citations A. References were added

1. Executive Summary

The goal of a QIBA Profile is to help achieve a useful level of performance for a given biomarker.

The **Claim** (Section 2) describes the biomarker performance.

The **Activities** (Section 3) contribute to generating the biomarker. Requirements are placed on the **Actors** that participate in those activities as necessary to achieve the Claim.

Assessment Procedures (Section 4) for evaluating specific requirements are defined as needed.

This QIBA Profile (**Magnetic Resonance Elastography of the Liver**) addresses the **application of Magnetic Resonance Elastography (MRE) for the quantification of liver stiffness, which is often used as a biomarker of liver fibrosis.** It places requirements **on Acquisition Devices, Technologists, Radiologists, Reconstruction Software and Image Analysis Tools** involved in **Subject Handling, Image Data Acquisition, Image Data Reconstruction, Image QA and Image Analysis.**

The requirements are focused on **achieving sufficient accuracy and avoiding unnecessary variability of the measurement of hepatic stiffness.**

The clinical performance target is **to achieve a 95% confidence interval for a true change in stiffness has occurred when there is a measured change in hepatic stiffness of 19% or larger.**

This document is intended to help clinicians basing decisions on this biomarker, imaging staff generating this biomarker, vendor staff developing related products, purchasers of such products and investigators designing trials with imaging endpoints.

Note that this document only states requirements to achieve the claim, not “requirements on standard of care.” Conformance to this Profile is secondary to properly caring for the patient.

QIBA Profiles addressing other imaging biomarkers using CT, MRI, PET and Ultrasound can be found at qibawiki.rsna.org.

2. Clinical Context and Claims

Clinical Context

Chronic liver disease (CLD) is a major health burden in the US. CLD regardless of etiology when untreated may lead to liver fibrosis and if progressive to cirrhosis and its complications. Effective treatment methods for some forms of CLD are available and can prevent progression or even result in regression of fibrosis (1, 2). A reliable non-invasive technique is needed for detection, staging and treatment response assessment of liver fibrosis. Measurement of *liver stiffness* (defined in this document as the magnitude of the complex shear modulus) with MR Elastography (MRE) has been shown to be useful for non-invasive detection and staging of liver fibrosis (3, 4). Published evidence has established that MRE is an accurate and reproducible technique and promising for use in clinical trials (5-7).

Conformance to this Profile by all relevant staff and equipment supports the following claim(s):

Claim: A measured change in hepatic stiffness of 19% or larger indicates that a true change in stiffness has occurred in that patient with 95% confidence.

This claim holds when:

- **A change in liver stiffness is measured at two time points with the same scanner, driver hardware, parameters, and software.**

Discussion

This claim is based on estimates of the normal liver stiffness within-subject coefficient of variation (wCV) which we have estimated as 7% (8). The Repeatability Coefficient is then 2.77 × wCV, or 19%. If Y1 and Y2 are the stiffness values (in kPa) at the two time points, then the 95% confidence interval for the true change is (Y2-Y1) ± 1.96 x sqrt{ [Y1x0.07]^2 + [Y2 x0.07]^2 } kPa.

Clinical interpretation with respect to the magnitude of true stiffness change:
The magnitude of the true change is defined by the measured change and the error bars. For example, if 3.5 kPa and 2.5 kPa are the stiffness values at time points 1 and 2, respectively, then (3.5-2.5)/3.5 represents a 40% change. Since 40%>19%, we are 95% confident that a true change in hepatic stiffness has occurred. The 95% confidence interval for the true change is 1.0 ± 0.49 kPa.

Multiple studies have demonstrated good agreement in mechanical stiffness of phantom materials assessed using MRE, and of the same phantom materials assessed using dynamic mechanical analyzer (DMA) instruments (9-11). These studies provide confidence in the validity of MRE-based stiffness measurements. However, routine comparisons of MRE and DMA measurements for tissue and tissue-like materials are of limited use for MRE QA due to the technical limitations of DMA testing, including the difficulty of defining the geometry of semi-solid test specimens.

3. Profile Activities

The Profile is documented in terms of "Actors" performing "Activities". Equipment, software, staff or sites may claim conformance to this Profile as one or more of the "Actors" in the following table.

Conformant Actors shall support the listed Activities by conforming to all requirements in the referenced Section.

Table 1: Actors and Required Activities

Actor	Activity	Section
Acquisition Device	Pre-delivery	3.1.
	Subject Handling	3.5.
	Image Data Acquisition	3.6.
Technologist	Subject Handling	3.5.
	Image Data Acquisition	3.6.
	Image Data Reconstruction	3.7.
Radiologist	Subject Handling	3.5.
	Image QA	3.8.
	Image Analysis	3.10.
Reconstruction Software	Image Data Reconstruction	3.7.
Image Analysis Tool	Image Analysis	3.10.

The requirements in this Profile do not codify a Standard of Care; they only provide guidance intended to achieve the stated Claim. Failing to conform to a "shall" in this Profile is a protocol deviation. Although deviations invalidate the Profile Claim, such deviations may be reasonable and unavoidable and the radiologist or supervising physician is expected to do so when required by the best interest of the patient or research subject. How study sponsors and others decide to handle deviations for their own purposes is entirely up to them.

3.1. Pre-delivery

There are no onsite pre-delivery testing requirements.

3.2. Installation

Installation and initial functional validation shall be performed according to manufacturer-defined procedures and specifications, including MRE driver system and pulse sequences.

3.3. Periodic QA

Required QA. Measurements of liver stiffness (magnitude of the complex shear modulus) obtained with MRE depend on the spatial fidelity of the acquired phase images. Therefore, the validity of the field of view and image linearity should be assessed and confirmed on an ongoing basis, as is already routine for all clinical scanners, using manufacturer-recommended procedures.

While other instrumental causes of drift in stiffness measurements have not been documented in the literature, technical failures such as faulty synchronization of the driver system or incorrect driver frequency settings can cause incorrect measurement.

Optional QA. Correct user set-up and proper functioning of the MRE system can be confirmed using a phantom with a known stiffness properties. These usually consist of a uniform, tissue-simulating material with known stiffness and known stability over time and storage conditions. An MRE phantom can be used to confirm proper functioning of the MRE system after initial installation and as a periodic test of correct functioning. There is as yet no consensus on recommendations for the frequency of phantom testing. Optional QA testing with a phantom should employ a protocol recommended by the phantom manufacturer. Appendix 2 describes a sample protocol for a currently available phantom.

3.4. Subject Selection

Local policies for patient eligibility for MRI should be followed. Definition of the relative and/or absolute contraindications to MRI is not within the scope of this document.

3.5. Subject Handling

3.5.1 Subject preparation

The subject should be fasting for at least 4 hours before the scheduled time of the imaging (14, 15).

3.5.2 Subject positioning

The subject will be scanned in supine position.

The passive driver is placed over the right lower chest wall at the level of xiphisternum in midclavicular line. (Can be placed in the right mid-axillary line if colon is present between the anterior body wall and the liver) (16, 17).

The passive driver is held in firm contact with the body wall using an elastic band. The passive driver is connected to the active driver, which is located outside the scan room, via a plastic tube.

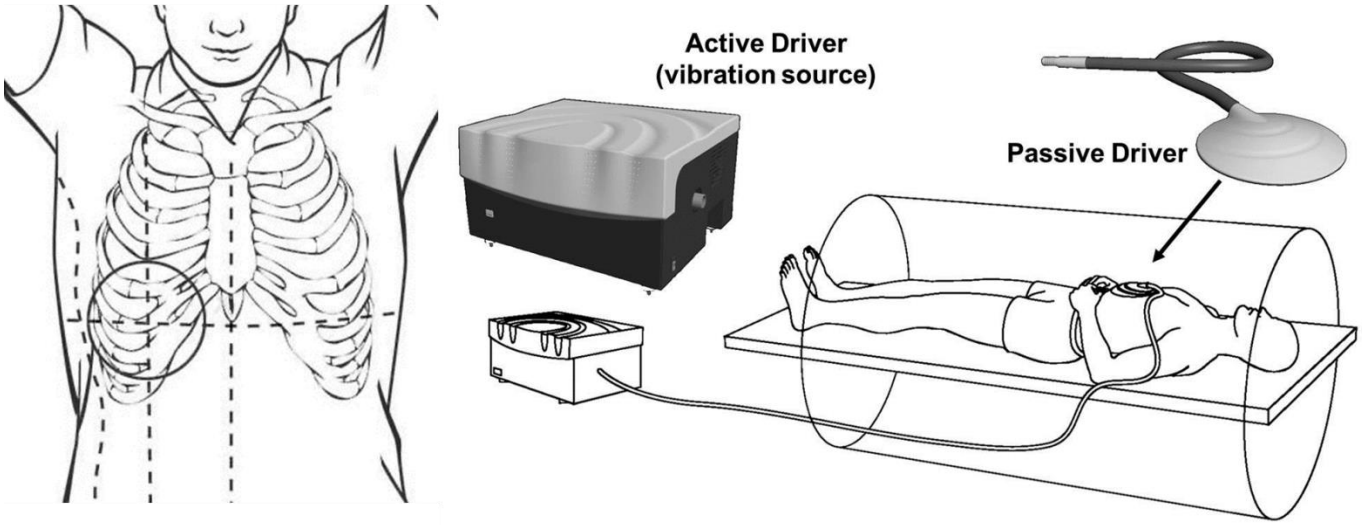


Figure 1: The passive driver should be placed over the right lower anterior chest wall at the level of the xiphisternum, centered on the mid-clavicular line. Once positioned, the passive driver should be held firmly against the chest wall by a wide elastic band, placed around the torso. Check to ensure that the band is stretched sufficiently so that the driver is not loose during full expiration. (video links on MR tech training – to be added) Note that the passive driver is connected via a plastic tube to the active driver (vibration source), which is located outside the scan room.

3.6. Image Data Acquisition

3.6.1 GRE-MRE Sequence

Sequences discussed are commercially available 2D MRE acquisition techniques. Image data are acquired during suspended expiration in a natural end-expiratory position.

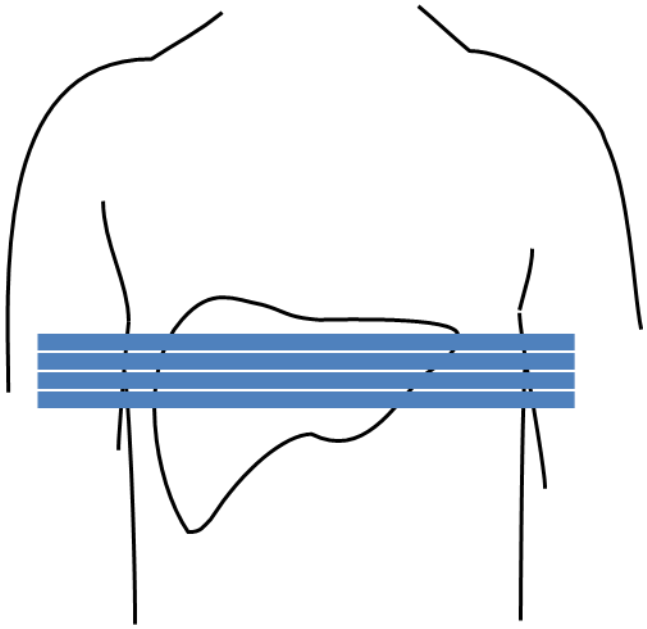


Figure 2: Acquired sections for MRE are positioned at the level of the widest transverse extent of the liver, avoiding the dome and inferior tip of the right lobe. Sections should be prescribed in a coronal image in relaxed end-expiration.

See Appendix D for detailed vendor specific and scanner specific protocol parameters.

3.6.2 Technical success

The raw magnitude and phase images obtained from the MRE acquisition should be reviewed on the scanner console at the time of the exam. As shown in Figure 3, the magnitude images should show signal loss in the subcutaneous fat just below the passive driver placement, confirming that mechanical waves are being applied. The phase images (also known as wave images) should demonstrate shear waves in the liver. If no waves are imaged in the liver, then the driver system should be checked.

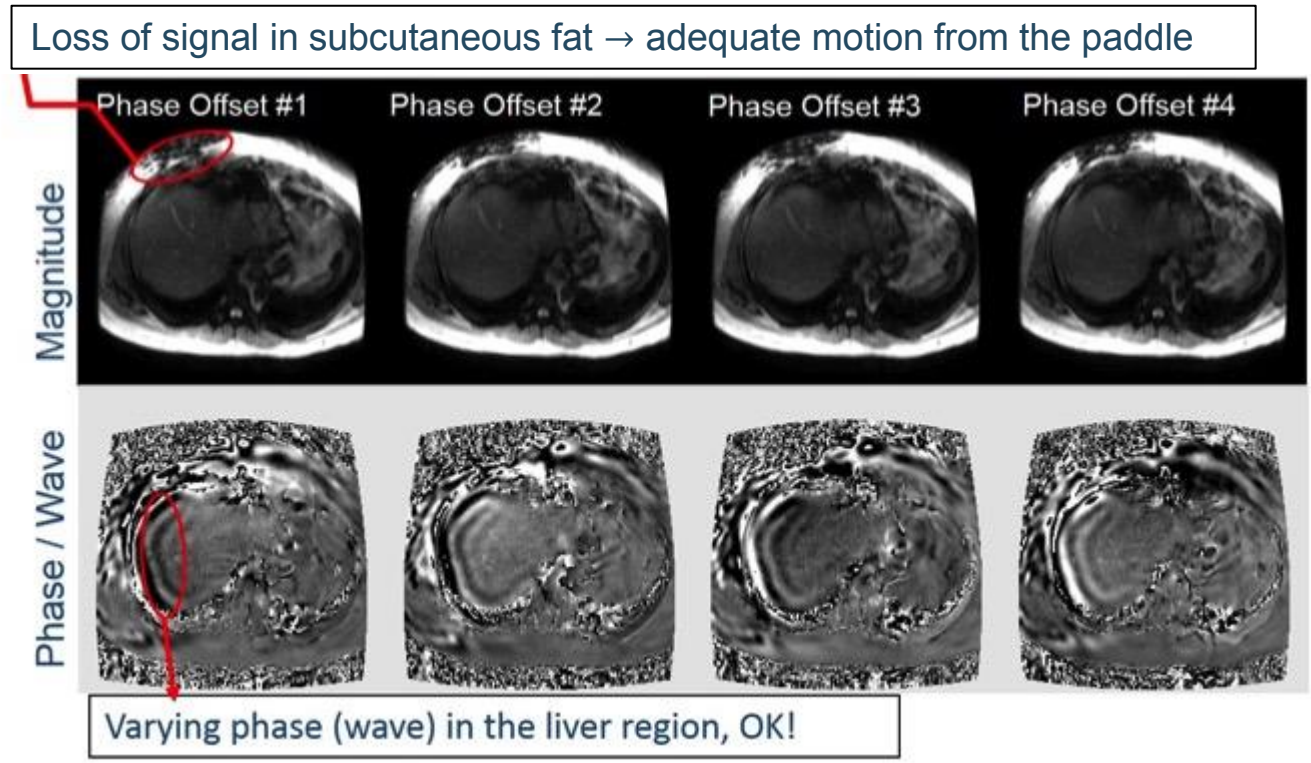


Figure 3: Valid MRE. Top row shows the magnitude images of four offsets and bottom row shows the phase (wave) images. The four offsets belong to a single slice location.

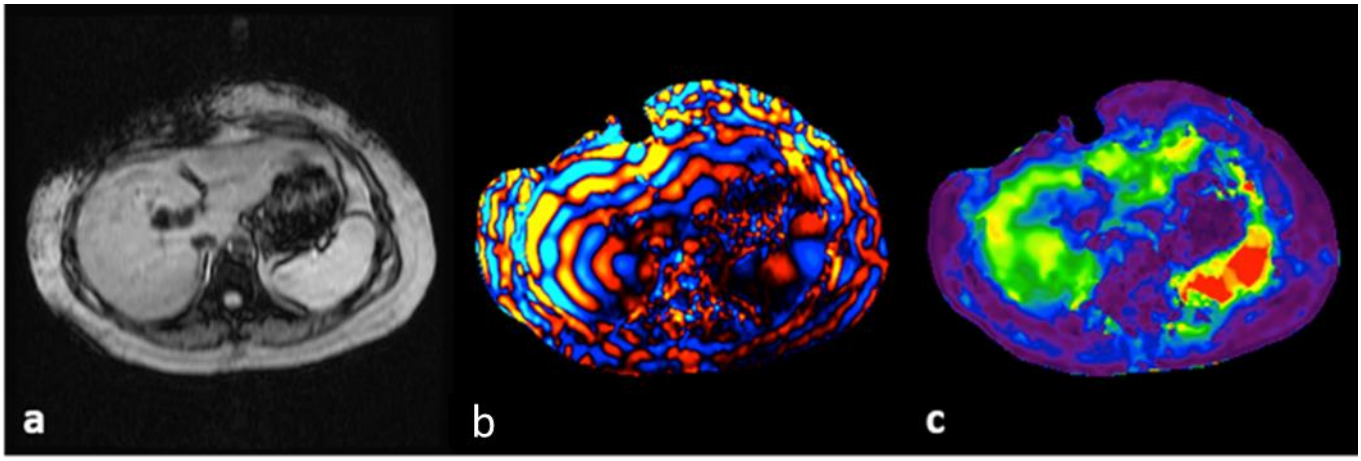


Figure 4: Magnitude (a) and color-coded wave (b) images of a successful MRE showing excellent illumination of waves through the liver. Stiffness map (c) shows elevated liver stiffness consistent with significant fibrosis.

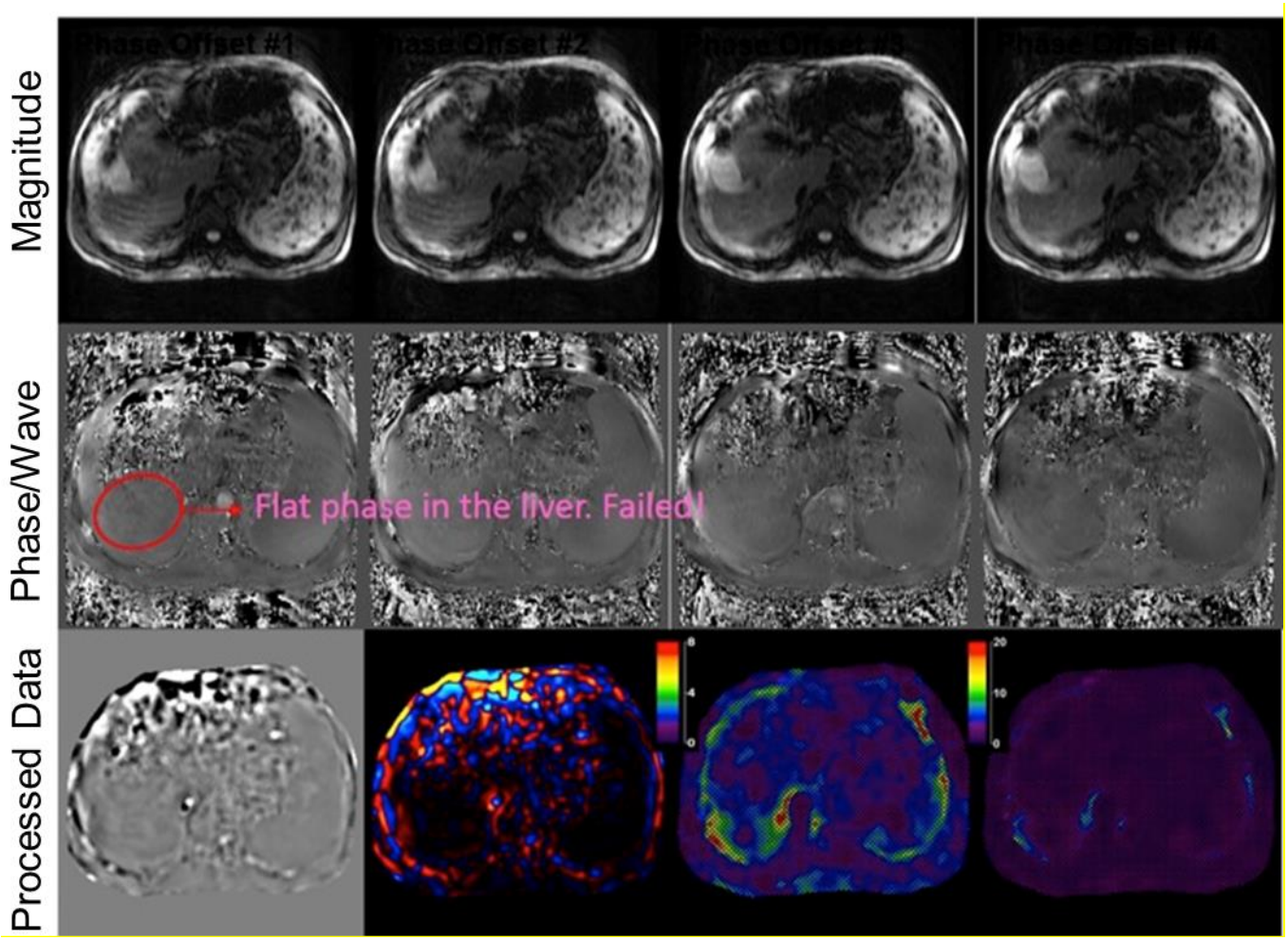


Figure 5: Failed MRE – Representative images of failed MRE due to colonic interposition between paddle and liver.

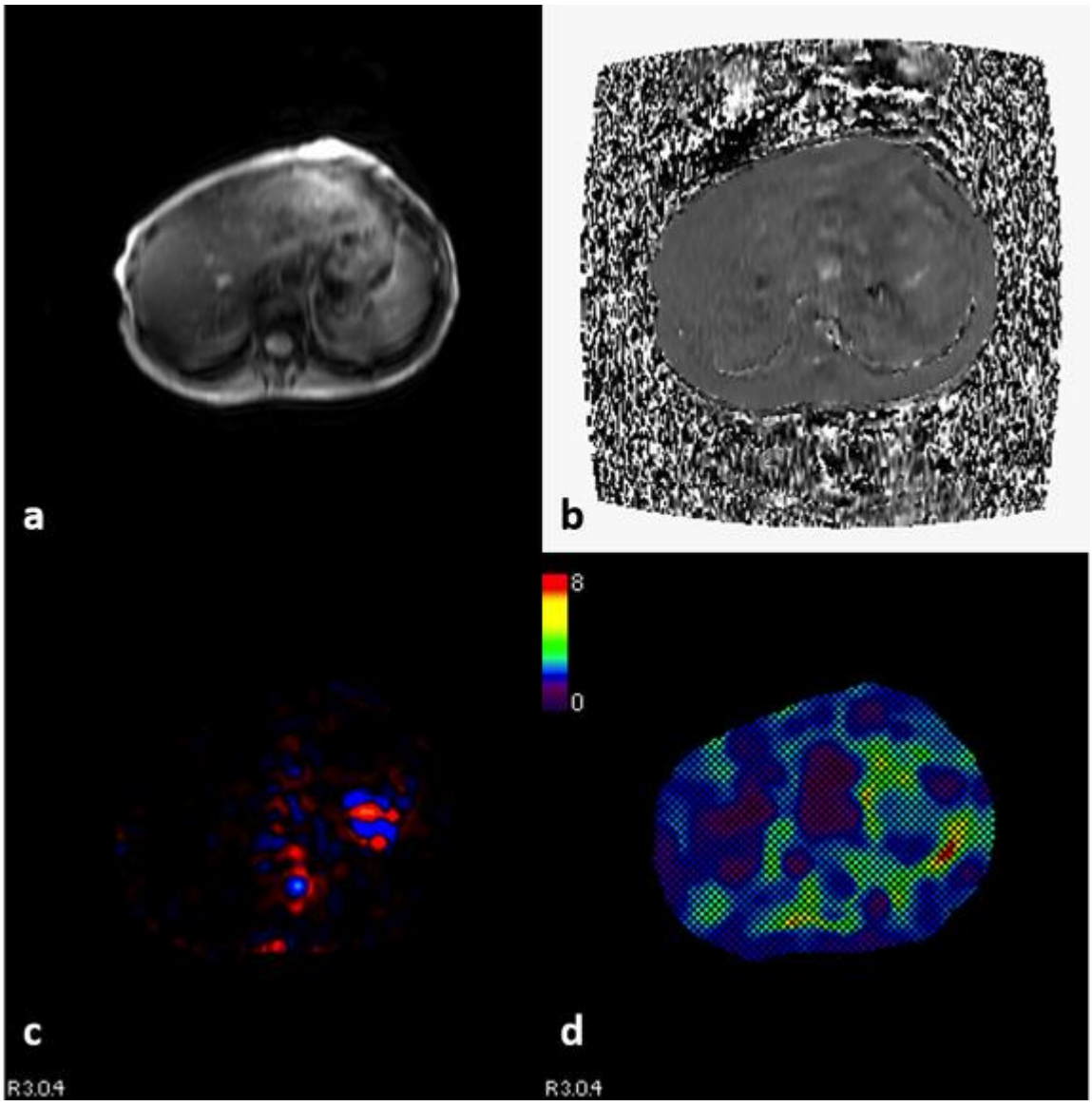


Figure 6: Failed MRE – Representative images of failed MRE due to disconnection of plastic tube between passive and active drivers. Magnitude (a), phase (b), and color-coded wave (c) images show no waves traversing the liver. Stiffness map (d) has no valid data.

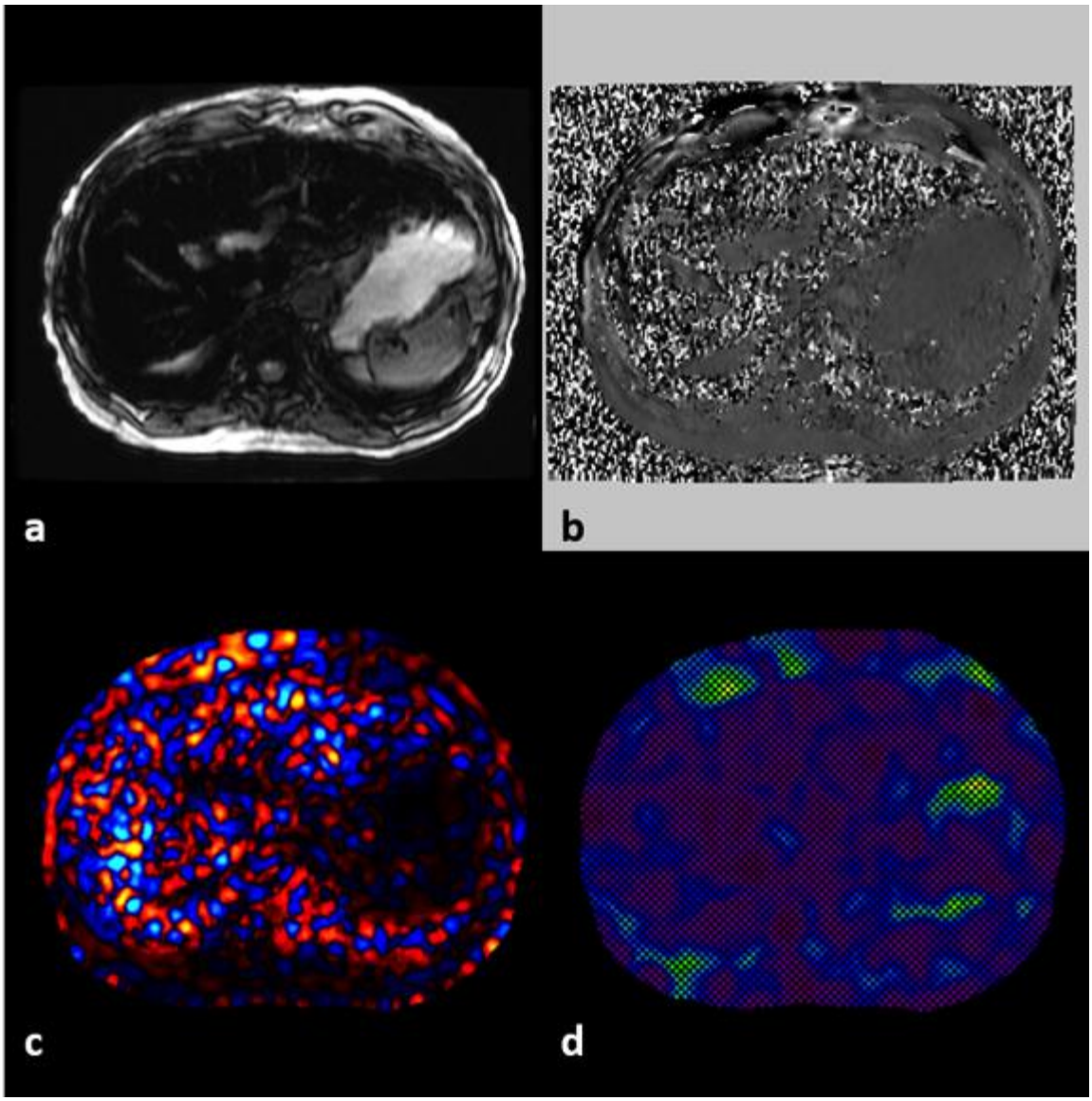


Figure 7: Failed MRE – Representative images of failed MRE failed due to hepatic iron overload. Magnitude (a), phase (b), and color-coded wave (c) images show no waves traversing the liver. Stiffness map (d) has no valid data.

3.7. Image Data Reconstruction

3.7.1 DISCUSSION

Post-processing of the acquired magnitude and phase (wave) images is performed to create quantitative maps of liver stiffness, or elastograms. This post-processing technique is standardized across vendors.

3.7.2 QUANTITATIVE ELASTOGRAMS

After the magnitude and phase images are acquired, the scanner computer automatically processes

the information to generate the following images on the scanner console as illustrated in Figure 4.

1. **Quantitative stiffness maps (elastograms), depicting the magnitude of the complex shear modulus in a gray or color scale. The most appropriate default scale is 0-8 kPa.**
2. **Confidence maps: quantitative elastograms in which areas where the estimated stiffness values have reduced reliability due to low wave amplitude are indicated with cross-hatching or other means.**
3. **Unwrapped wave images, providing a clear depiction of the observed waves. Phase wrapping occurs when the shear wave motion is large. Since MRE is a phase-based technique, the displacement data typically must be unwrapped before subsequent processing is performed.**

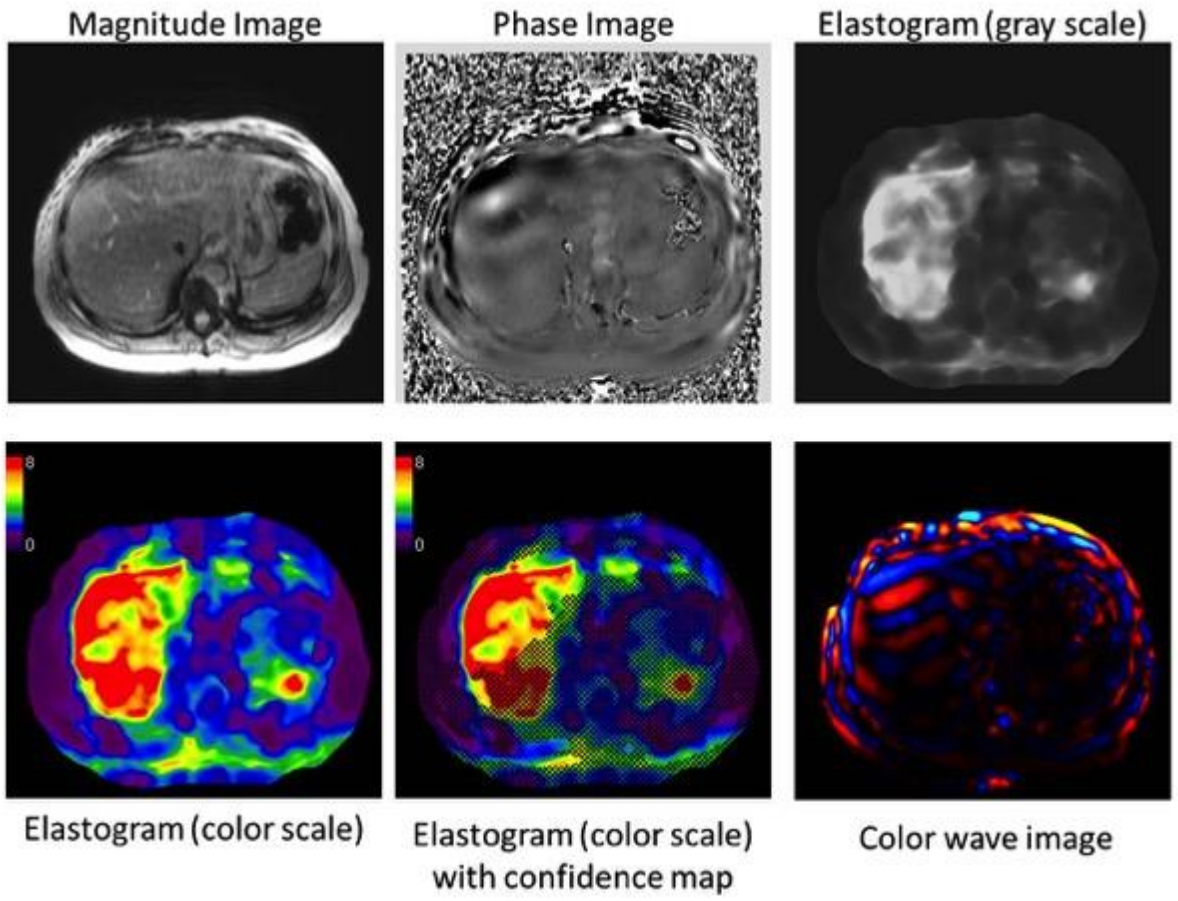


Figure 8: Representation of images generated in a MRE study. Additional post-processed images may be available depending on the software version installed on the scanner.

3.8. Image QA

At the time of image review, the suitability of the data should be checked again by confirming the presence of signal loss in subcutaneous fat under the driver in the magnitude images, and presence of visible of waves in the liver in the phase and wave images (Figure 3).

The quantitative elastograms of successful exams should demonstrate areas of valid stiffness data within the liver in the confidence maps (see figures 3 to 8 as representative examples of a successful

and failed MRE studies).

3.9. Image Distribution

There are no specific requirements on image distribution for MRE.

3.10. Image Analysis

Mean shear stiffness of the liver is calculated using manually specified regions of interest (ROIs). The ROIs are drawn manually in the largest possible area of liver parenchyma in which coherent shear waves are visible, while excluding major blood vessels seen on the MRE magnitude images. To avoid areas of incoherent waves, avoid regions immediately under the paddle and stay ~1 cm inside the liver boundary and contain a minimum of 500 pixels per slice (3, 18). ROIs should be placed in individual slices and in the right lobe whenever possible. The mean value is calculated from all slices and reported as stiffness in kilopascals (kPa).

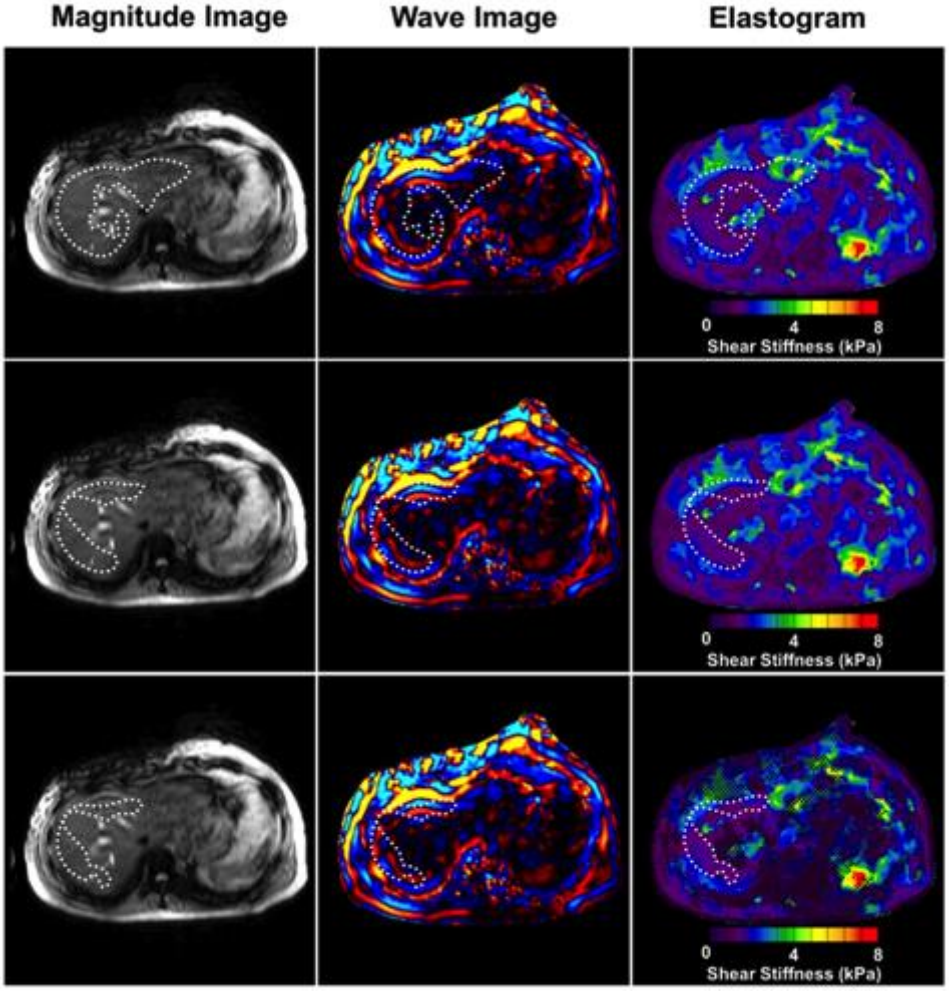


Figure 9: Regions of interest (ROIs) should be drawn with reference to the magnitude, wave, and elastogram images. The ROI should be within the contour of the liver, excluding areas near the margins and major vessels (top row). The ROI should be modified to exclude areas with low wave amplitude as well as incoherent waves, as observed in the wave images (middle row). The ROI should also exclude areas of low confidence, as seen by the checkerboard pattern in the masked elastogram images (lower row). In practice, the ROIs may be drawn in a single step, keeping these principles in

mind. Generally the ROI should be confined to the right lobe of the liver. (video links on training – will be added)

3.11. Image Interpretation

Overall mean stiffness of liver is reported by recording the mean stiffness value of each ROI and then calculating the mean value, weighted by ROI size.

Example: Slice 1: mean liver stiffness = 2.32 kPa and ROI size = 2500 mm^2; Slice 2: mean liver stiffness = 2.25 kPa and ROI size = 1500 mm^2; Slice 3: mean liver stiffness = 2.52 kPa and ROI size = 500 mm^2; and Slice 4: mean liver stiffness = 2.22 kPa and ROI size = 1000 mm^2; then the weighted mean = ((2.32 X 2500)+(2.25 X 1500)+(2.52 X 500) + (2.22 X 1000))/(2500+1500+500+1000) = 2.30 kPa.

4. Assessment Procedures

To conform to this Profile, participating staff and equipment ("Actors") shall support each activity assigned to them in Table 1.

To support an activity, the actor shall conform to the requirements (indicated by "shall language") listed in the specifications table of the activity subsection in Section 3.

Although most of the requirements described in Section 3 can be assessed for conformance by direct observation, some of the performance-oriented requirements cannot, in which case the requirement will reference an assessment procedure in a subsection here in Section 4.

Formal claims of conformance by the organization responsible for an Actor shall be in the form of a published QIBA Conformance Statement. Vendors publishing a QIBA Conformance Statement shall provide a set of "Model-specific Parameters" (as shown in Appendix D) describing how their product was configured to achieve conformance. Vendors shall also provide access or describe the characteristics of the test set used for conformance testing.

4.1. Assessment Procedure: Stiffness Measurement in the liver

This procedure can be used by a vendor, physicist, or an imaging site to assess the stiffness measurement with MRE. For MRE use as a quantitative imaging biomarker of liver stiffness, it is essential to ensure quality assurance of the acquisition and image processing methodology.

For MRE image acquisition, it is important to consider the availability of:

- **Appropriate imaging equipment**
- **Experienced MR technologists for the imaging procedure**
- **Procedures to ensure standardized image analysis techniques**

4.1.1 IMAGING EQUIPMENT

As outlined in Section 3.2, installation and initial functional validation shall be performed according to manufacturer-defined procedures and specifications. This includes specific guidelines on the MRI scanner and MRE driver system. The scanner must be under quality assurance and quality control processes as outlined by local institution and vendor requirements. The scanner software version should be identified and tracked across time.

4.1.2 IMAGING PROCEDURE

MR technologists or other site personnel performing liver MRE should be MR-certified according to site-specific local or institutional requirements. These individuals should be trained or have prior experience in conducting liver MRE as outlined in Section 3.6. Currently, there is not a standard imaging phantom for standardized image acquisition and processing procedures.

4.1.3 IMAGE ANALYSIS

Image analysis software for liver MRE is standardized across vendors. Therefore, the quantitative elastograms or stiffness maps are highly reproducible across sites and vendors. For the determination of ROIs, training and procedures should be followed as outlined in Section 3.10.

4.2. Test-Retest Conformance Study

Actors should demonstrate conformance to the profile through a test-retest repeatability study which may be performed in a group of healthy volunteers. An important assumption underlying the claim is that the image analysis software has a within-subject test-retest coefficient of variation (wCV) of <0.07 (7%) (or RC of <19%).In order to test this assumption, N=40 normal subjects will be imaged twice on the same day (and additionally, some of these subjects may return for a third scan within one week). Subject selection should be performed as outlined in Section 3.4. Subjects should be scanned at three time points: twice in one day and a third time less than one week later. The same scanner, driver hardware, parameters, and software should be used following the guidelines outlined in Section 3.5 for subject preparation and positioning. Following the liver MRE acquisition on day 1, subjects will be asked to stand and are repositioned for a second MRE exam. A third MRE exam should be performed within 7 days. The data is reconstructed and analyzed using the techniques outlined in Section 3.7 and 3.10 respectively.

Let Y_{i1} denote the liver stiffness measurement from the first scan 1, Y_{i2} denote the liver stiffness measurement from the second scan, and, as available, Y_{i3} denote the liver stiffness measurement from the third scan on the i-th subject. For each subject, calculate the mean of the J measurements (where J=2 or 3) and the wSD:

$$\overline{Y}_i = \sum(Y_{ij})/J \text{ and } wSD_i^2 = \sum(Y_{ij} - \overline{Y}_i)^2/(J-1).$$

Then estimate the wCV:

$$wCV = \sqrt{\sum_{i=1}^{N=40}(wSD_i^2/\overline{Y}_i^2)/N}.$$

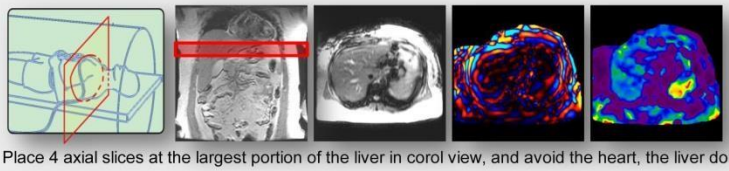
The percent repeatability coefficient is then calculated as follows: $\%RC = 1.96 \times \sqrt{2 \times \%wCV^2}$.

To demonstrate conformance with the profile claim, this estimated %RC from the test-retest study must be ≤19%.

Appendix D: Detailed MRE Protocols

For acquisition modalities, reconstruction software and software analysis tools, profile conformance requires meeting the activity specifications above in Sections 2, 3, and 4.

This Appendix provides, as an informative tool, some specific acquisition parameters, reconstruction parameters and analysis software parameters that are expected to be compatible with meeting the profile requirements.

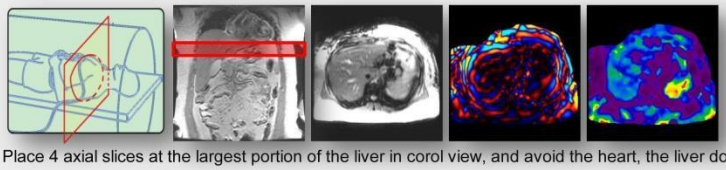
GE 1.5T - Hepatic MRE Protocols - April 2016 Draft 2				
Scanners and Sequences	Scanner	HDx	HDx	MR450w
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	fgremre (Resoundant-GE)	epimre (Resoundant-GE)	MR-Touch (GRE)
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	FC, ASSET, MultiPhase	Fast, ASSET, MultiPhase
Patient Cooperation	(1) Patients fast at least 4-6 hours prior to the exams			
	(2) Patients hold breath at the end of expireation during all MRE scans, as well as during scout scans and parallel imaging calibration scans.			
Slice Positing	 Place 4 axial slices at the largest portion of the liver in corol view, and avoid the heart, the liver dome and the liver bottom tip.			
Patient Inforamation Input	Position	feet-first, supine	feet-first, supine	feet-first, supine
	Weight	Actual Weight	Actual Weight	Actual Weight
	Height			
Coil (note 1)	Coil	Torso	Torso	Torso
Imaging Prameters	Imaging Plane	Axial	Axial	Axial
	No. of slices	4	4	4
	Slice thickness (mm)/gap	10 mm / 0 mm	8 mm / 2 mm	10 mm / 0 mm
	FOV (mm) / Phase FOV (100%)	420/1 (note 4)	420/1 (note 4)	420/1 (note 4)
	Matrix	256 × 64	80 × 80	256 × 64
	TE (msec)	in-phase TE (about 18.2)	min full(around 55.4) (note 1)	min TE (type a value colse to 18.2 if possible)
	TR (msec)	50	1000	50
	Flip Angle (degree)	25	default (90)	25
	NEX, EPI shots	1	1, 1shot	1
	Bandwidth (kHz)	31.25	250 (hard coded)	31.25
	Freq Encoding Dir	right - left	right - left	right - left
	Phases per Location	4	4	
	Phase Acq. Order	Interleaved	Interleaved	
	Delay After Acq.	Minimum	Minimum	
	Acceleration	ASSET (Note 1)	ASSET (Note 1)	ASSET (Note 1)
	Acceleration factor	2	2	2
	No. of breath holds	4 (note 2)	1	4 (note 2)
	Shimming Volume	Cover the whole body	Cover the whole body	Cover the whole body
	Spectrum Peaks	Water Peak	Water Peak	Water Peak
	Saturation Band	SI	SI	SI
	scan time	55 s (note 2)	16 sec	55 sec (note 2)

GE 1.5T - Hepatic MRE Protocols - April 2016 Draft 2				
Scanners and Sequences	Scanner	HDx	HDx	MR450w
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	fgremre (Resoundant-GE)	epimre (Resoundant-GE)	MR-Touch (GRE)
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	FC, ASSET, MultiPhase	Fast, ASSET, MultiPhase
Driver Parameters (Generic) (note 5)	Driver Power (%)	50	50	50
	Driver frequency (Hz)	60	60	60
	Driver cycles/ trigger (Duration)	3 (auto-caculated)	Auto-calculated	Auto-caculated
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz) (or Period Mismatch)	75 Hz (0.8)	155	75
	MEG Amplitude (G/cm)	About 3 G/cm with Zoom gradient (75%) (note 3)	Full Scale (note 3)	
	Axis of MEG	4 (Z)	4 (Z)	4 (Z)
User CV or Advanced Table (Specific: epimre -DV16 and DV24) (note 5)	CV0 -Ramp Sampling (1=on, 0=off)		1	
	CV1			
	CV2			
	CV3			
	CV4			
	CV5 -Scale for RF2 Crusher Area		1	
	CV6 -Split MEG (0=L,1/2/3 = L-R in/half/min		2	
	CV7 -Flow Comp. Type for MEG		0	
	CV8 -Driver Frequency Percent Increase		0.5	
	CV9 -Time from Start of MEG1 to MEG2 (-1 = opt, 0=min)		0	
	CV10 -Number of Gradient Pairs		1	
	CV11 -Soft-start Ramp-up Time (sec)		0	
	CV12 -Fraction of Max Gradient Amplitude		1	
	CV13 -Desired MEG Frequency (Hz)		155	
	CV14 -Driver Amp. % (-1 = not V3)		50	
	CV15 -Recon (Def-1912;3D ver =1914;Brain=1915;2D MMDI = 1916)		1916	
	CV16 -Trigger Loc # of Cycles Pre-MEG		4	
	CV17 -MEG Direction (F/P/S=1/2/4, Tetra=8)		4	
	CV18 -Vibration Mode (0=Burst, 1 or 2 = Contin.)		1	
	CV19 - MENC (um per radians)		Don't edit	
	CV20 -# of Motion Periods for Offsets		1	
	CV21 -Frequency of Applied Motion (Hz)		60	
	CV22			
	CV23 -Burst Mode Burst Count		1	

350 230

GE 1.5T - Hepatic MRE Protocols - April 2016 Draft 2				
Scanners and Sequences	Scanner	HDx	HDx	MR450w
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	**fgremre (Resoundant-GE)**	**epimre (Resoundant-GE)**	**MR-Touch (GRE)**
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	FC, ASSET, MultiPhase	Fast, ASSET, MultiPhase
	CV24 -Do High-Resolution Recon.?		1	
User CV (Specific: fgremre - DV16) (note 5)	CV 12 -use version3 driver	1		
	CV 13 -Motion Encoding Gradient (MEG) pairs	1		
	CV 14 Motion Frequency - Hz	60		
	CV 15 Scale Max Gradient Amplitude	0.75		
	CV 17 freq=1, phase=2, slice=4	4		
	CV 21 period mismatch	0.8		
	CV 24 driver amplitude	50		
MR-Touch Tab (Specific fgremre-DV22.1, DV24) (note 5)	Temporal Phases	4		
	MEG Frequency (Hz)	75		
	Driver Amplitude (%) (note 6)	50		
	Driver Cycle Per Trigger	3		
	MEG Direction	4 (Z)		
Advanced Tab (Specific fgremre-DV22.1, DV24) (note 5)	CV12 use resoundant	1.00		
MR-Touch Tab (Specific MR-Touch sequence - DV22.1, DV24) (note 5)	Temporal Phases			4
	MEG Frequency (Hz)			75
	Driver Amplitude (%) (note 6)			50
	Driver Cycle Per Trigger			3
	MEG Direction			4 (Z)

NOTE: (1) Use body coil instead of torso if paitents cannot fit into the bore with the torso coil; if body coil is used then the ASSET is turned off automatically, scan time is longer (gre) or TE is longer (epi). (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time and breath-hold time. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (420 mm), even for small patients for consistency. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners.(6) Driver Frequencey is 60Hz (default).

GE 3T - Hepatic MRE Protocols - April 2016 Draft 2				
Scanners and Sequences	Scanner	HDx	HDx	MR750w
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	fgremre (Resoundant-GE)	epimre (Resoundant-GE)	MR-Touch (EPI)
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	FC, ASSET, MultiPhase	FC, ASSET, MultiPhase
Patient Cooperation	(1) Patients fast at least 4-6 hours prior to the exams			
	(2) Patients hold breath at the end of expireation during all MRE scans, as well as during scout scans and parallel imaging calibration scans.			
Slice Positing	 Place 4 axial slices at the largest portion of the liver in corol view, and avoid the heart, the liver dome and the liver bottom tip.			
Patient Inforamation Input	Position	feet-first, supine	feet-first, supine	feet-first, supine
	Weight	Actual Weight	Actual Weight	Actual Weight
	Height			
Coil (note 1)	Coil	Torso	Torso	Torso
Imaging Prameters	Imaging Plane	Axial	Axial	Axial
	No. of slices	4	4	4
	Slice thickness (mm)/gap	10 mm / 0 mm	8 mm / 2 mm	8 mm / 2 mm
	FOV (mm) / Phase FOV (100%)	420/1 (note 4)	420/1 (note 4)	420/1 (note 4)
	Matrix	256 × 64	80 × 80	80 × 80
	TE (msec)	min full (around 15.9, this is close to in-phase TE)	min full(around 55.4) (note 1)	min full(around 55.4) (note 1)
	TR (msec)	50	1000	1000
	Flip Angle (degree)	20	default (90)	default (90)
	NEX, EPI shots	1	1, 1shot	1, 1shot
	Bandwidth (kHz)	31.25	250 (hard coded)	250 (hard coded)
	Freq Encoding Dir	right - left	right - left	right - left
	Phases per Location	4	4	
	Phase Acq. Order	Interleaved	Interleaved	
	Delay After Acq.	Minimum	Minimum	
	Acceleration	ASSET (Note 1)	ASSET (Note 1)	ASSET (Note 1)
	Acceleration factor	2	2	2
	No. of breath holds	4 (note 2)	1	1
	Shimming Volume	Cover the whole body	Cover the whole body	Cover the whole body
	Spectrum Peaks	Water Peak	Water Peak	Water Peak
	Saturation Band	SI	SI	SI
	scan time (note 7)	about 55 s (note 2)	about 16 sec	about 16 sec

GE 3T - Hepatic MRE Protocols - April 2016 Draft 2				
Scanners and Sequences	Scanner	HDx	HDx	MR750w
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	**fgremre (Resoundant-GE)**	**epimre (Resoundant-GE)**	**MR-Touch (EPI)**
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	FC, ASSET, MultiPhase	FC, ASSET, MultiPhase
Driver Parameters (Generic) (note 5)	Driver Power (%)		50	50
	Driver frequency (Hz)	60	60	60
	Driver cycles/ trigger (Duration)	3 (auto-caculated)	Auto-calculated	Auto-calculated
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz) (or Period Mismatch)	80 Hz (0.75)	155	90
	MEG Amplitude (G/cm)	About 3 G/cm with Zoom gradient (75%) (note 3)	Full Scale (note 3)	
	Axis of MEG	4 (Z)	4 (Z)	4 (Z)
User CV or Advanced Table (Specific: epimre -DV16 and DV24) (note 5)	CV0 -Ramp Sampling (1=on, 0=off)		1	
	CV1			
	CV2			
	CV3			
	CV4			
	CV5 -Scale for RF2 Crusher Area		1	
	CV6 -Split MEG (0=L,1/2/3 = L-R in/half/min		2	
	CV7 -Flow Comp. Type for MEG		0	
	CV8 -Driver Frequency Percent Increase		0.5	
	CV9 -Time from Start of MEG1 to MEG2 (-1 = opt, 0=min)		0	
	CV10 -Number of Gradient Pairs		1	
	CV11 -Soft-start Ramp-up Time (sec)		0	
	CV12 -Fraction of Max Gradient Amplitude		1	
	CV13 -Desired MEG Frequency (Hz)		155	
	CV14 -Driver Amp. % (-1 = not V3)		50	
	CV15 -Recon (Def-1912;3D ver =1914;Brain=1915;2D MMDI = 1916)		1916	
	CV16 -Trigger Loc # of Cycles Pre-MEG		4	
	CV17 -MEG Direction (F/P/S=1/2/4, Tetra=8)		4	
	CV18 -Vibration Mode (0=Burst, 1 or 2 = Contin.)		1	
	CV19 - MENC (um per radians)		Don't edit	
	CV20 -# of Motion Periods for Offsets		1	
	CV21 -Frequency of Applied Motion (Hz)		60	
	CV22			
	CV23 -Burst Mode Burst Count		1	

GE 3T - Hepatic MRE Protocols - April 2016 Draft 2				
Scanners and Sequences	Scanner	HDx	HDx	MR750w
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	**fgremre (Resoundant-GE)**	**epimre (Resoundant-GE)**	**MR-Touch (EPI)**
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	FC, ASSET, MultiPhase	FC, ASSET, MultiPhase
	CV24 -Do High-Resolution Recon.?		1	
User CV (Specific: fgremre - DV16) (note 5)	CV 12 -use version3 driver	1		
	CV 13 -Motion Encoding Gradient (MEG) pairs	1		
	CV 14 Motion Frequency - Hz	60		
	CV 15 Scale Max Gradient Amplitude	0.75		
	CV 17 freq=1, phase=2, slice=4	4		
	CV 21 period mismatch	0.75		
	CV 24 driver amplitude	50		
MR-Touch Tab (Specific fgremre-DV22.1, DV24) (note 5)	Temporal Phases	4		
	MEG Frequency (Hz)	80		
	Driver Amplitude (%) (note 6)	50		
	Driver Cycle Per Trigger	3		
	MEG Direction	4 (Z)		
Advanced Tab (Specific fgremre-DV22.1, DV24) (note 5)	CV12 use resoundant	1.00		
MR-Touch Tab (Specific MR-Touch sequence - DV22.1, DV24) (note 5)	Temporal Phases			4
	MEG Frequency (Hz)			90
	Driver frequency (Hz)			60
	Driver Amplitude (%)			50
	MEG Direction			Z
	Driver Cycle Per Trigger			15 (Not for edit)
	MENC um/rad			28.5 (Not for edit)

NOTE: (1) Use body coil instead of torso if paitents cannot fit into the bore with the torso coil; if body coil is used then the ASSET is turned off automatically, scan time is longer (gre) or TE is longer (epi). (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time and breath-hold time. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (420 mm), even for small patients for consistency. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners.(6) Driver Frequencey is 60Hz (default). (7) scan time can be slightly different for different scanners

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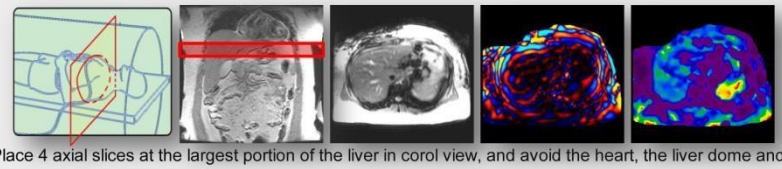
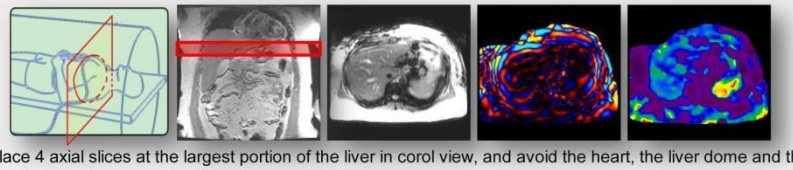
Siemens 1.5T - Hepatic MRE Protocols - April 2016 Draft 2			
Scanners and Sequences	Scanner		
	Software versions		
	Pulse sequence	greMRE	epseMRE(WIP)
	Mode	2D	2D
Patient Cooperation	(1) Patients fast at least 4-6 hours prior to the exams		
	(2) Patients hold breath at the end of expireation during all MRE scans, as well as during scout scans and parallel imaging calibration scans.		
Slice Positing	 Place 4 axial slices at the largest portion of the liver in corol view, and avoid the heart, the liver dome and the liver bottom tip.		
Patient Inforamation Input	Position	head-first, supine	head-first, supine
	Weight	Actual Weight	Actual Weight
	Height	Actual Height	Actual Height
Coil (note 1)	Coil	Torso	Torso
Imaging Prameters	Imaging Plane	Tansversal	Tansversal
	No. of slices	4	4
	Slice thickness (mm)/dist. Factor	10 mm / 0% (0)	8 mm / 25% (2mm)
	FOV (mm) / Phase FOV (100%)	420/1 (note 4)	420/1 (note 4)
	Matrix (Base × Phase)	256 × 25%(64)	128 × 100%(128)
	TE (msec)	min (about ~20 with flow comp off)	min (about 50 with flow comp on)
	TR (msec)	50	1000
	Flip Angle (degree)	20	default (90)
	NEX, EPI shots	1	1, 1shot
	Bandwidth (Hz/Pixel)	260 Hz/pixel	1502 Hz/pixel
	Phase enc.dir.	Anterior-Posterior	Anterior-Posterior
	Acceleration	GRAPPA (note 1)	GRAPPA (note 1)
	Acceleration factor	2	2
	No. of breath holds	4 (each 17sec) (note 2)	1 (each 11 sec)
	Shimming Volume	auto	auto
	Spectrum Peaks	Water Peak	Water Peak
	Saturation Band	SI	SI
	scan time	4 × 17 sec	11 sec
Driver Parameters (Generic) (note 5)	Driver Power (%)	50 (default) (note 6)	50 (default) (note 6)
	Driver frequency (Hz)	60 (default) (note 6)	60 (default) (note 6)
	Driver cycles/ trigger (Duration)	3 (default) (note 6)	3 (default) (note 6)

Siemens 1.5T - Hepatic MRE Protocols - April 2016 Draft 2			
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz)	60 Hz (Hard Coded)	60 Hz (Hard Coded)
	MEG Amplitude	(Hard coded)	30 mT/m (Hard coded)
	Axis of MEG	Slice (Hard Coded)	Slice
	Number of phase	4 (Hard coded)	4 (Hard coded)
Specific Parameters (note 5)	Sequence - Part 1 - Flow Comp	NO	YES
	Sequence - Special - MEG Ampltude (mT/m)	Not available	30
	Sequence - Special - MEG Frequency (mT/m)	Not available	60.0
	Sequence - Special - MEG Waveform	Not available	1-2-1
	Sequence - Special - MEG Direction	Not available	Slice
	System - Tx/Rx - Img. Scale Cor.	2	2
	Resolution - Filter Image - Prescan Normalize	Check	Check

NOTE: (1) Use body coil instead of torso if paitents cannot fit into the bore with the torso coil; if body coil is used then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time and breath-hold time. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (420 mm), even for small patients for consistency. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners. (6) The current implementation of Semiens MRE does not access active driver, those values are default values and can be changed by using a seprate web connection to the active driver (Syngo or Laptop); epseMRE sequences delivers one trigger every 50ms.

Siemens 3T - Hepatic MRE Protocols - April 2016 Draft 2			
Scanners and Sequences	Scanner	Skyra	Skyra
	Software versions	VE11A	VE11A
	Pulse sequence	greMRE	epseMRE(WIP)
	Mode	2D	2D
Patient Cooperation	(1) Patients fast at least 4-6 hours prior to the exams		
	(2) Patients hold breath at the end of expireation during all MRE scans, as well as during scout scans and parallel imaging calibration scans.		
Slice Positing	 Place 4 axial slices at the largest portion of the liver in corol view, and avoid the heart, the liver dome and the liver bottom tip.		
Patient Inforamation Input	Position	head-first, supine	head-first, supine
	Weight	Actual Weight	Actual Weight
	Height	Actual Height	Actual Height
Coil (note 1)	Coil	Torso	Torso
Imaging Prameters	Imaging Plane	Tansversal	Tansversal
	No. of slices	4	4
	Slice thickness (mm)/dist. Factor	10 mm / 0% (0)	8 mm / 25% (2mm)
	FOV (mm) / Phase FOV (100%)	420/1 (note 4)	420/1 (note 4)
	Matrix (Base × Phase)	256 × 25%(64)	128 × 100%(128)
	TE (msec)	min (about ~20 with flow comp off)	min (about 50 with flow comp on)
	TR (msec)	50	1000
	Flip Angle (degree)	20	default (90)
	NEX, EPI shots	1	1, 1shot
	Bandwidth (Hz/Pixel)	260 Hz/pixel	1502 Hz/pixel
	Phase enc.dir.	Anterior-Posterior	Anterior-Posterior
	Acceleration	GRAPPA (note 1)	GRAPPA (note 1)
	Acceleration factor	2	2
	No. of breath holds	4 (each 17sec) (note 2)	1 (each 11 sec)
	Shimming Volume	auto	auto
	Spectrum Peaks	Water Peak	Water Peak
	Saturation Band	SI	SI
	scan time	4 × 17 sec	11 sec
Driver Parameters (Generic) (note 5)	Driver Power (%)	50 (default) (note 6)	50 (default) (note 6)
	Driver frequency (Hz)	60 (default) (note 6)	60 (default) (note 6)
	Driver cycles/ trigger (Duration)	3 (default) (note 6)	3 (default) (note 6)

Siemens 3T - Hepatic MRE Protocols - April 2016 Draft 2			
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz)	60 Hz (Hard Coded)	60 Hz (Hard Coded)
	MEG Amplitude	(Hard coded)	30 mT/m (Hard coded)
	Axis of MEG	Slice (Hard Coded)	Slice
	Number of phase	4 (Hard coded)	4 (Hard coded)
Specific Parameters (note 5)	Sequence - Part 1 - Flow Comp	NO	YES
	Sequence - Special - MEG Ampltude (mT/m)	Not available	30
	Sequence - Special - MEG Frequency (mT/m)	Not available	60.0
	Sequence - Special - MEG Waveform	Not available	1-2-1
	Sequence - Special - MEG Direction	Not available	Slice
	System - Tx/Rx - Img. Scale Cor.	2	2
	Resolution - Filter Image - Prescan Normalize	Check	Check

NOTE: (1) Use body coil instead of torso if paitents cannot fit into the bore with the torso coil; if body coil is used then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time and breath-hold time. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (420 mm), even for small patients for consistency. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners. (6) The current implementation of Semiens MRE does not access active driver, those values are default values and can be changed by using a seprate web connection to the active driver (Syngo or Laptop); epseMRE sequences delivers one trigger every 50ms.

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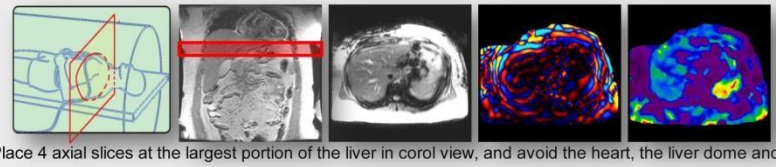
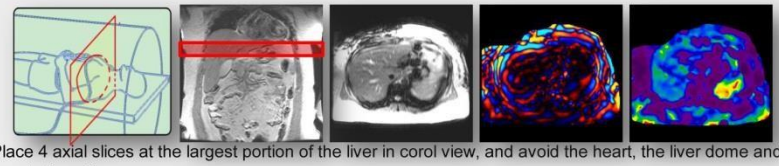
Philips 1.5T - Hepatic MRE Protocols - April 2016 Draft 2			
Scanners and Sequences	Scanner	Ingenia	Ingenia
	Software versions		
	Pulse sequence	GRE MRE	2D SE-EPI MRE
	Mode	2D	2D
Patient Cooperation	(1) Patients fast at least 4-6 hours prior to the exams		
	(2) Patients hold breath at the end of expireation during all MRE scans, as well as during scout scans and parallel imaging calibration scans.		
Slice Positing	 Place 4 axial slices at the largest portion of the liver in corol view, and avoid the heart, the liver dome and the liver bottom tip.		
Patient Inforamation Input	Position	feet-first, supine	feet-first, supine
	Weight	Actual Weight	Actual Weight
	Height		
Coil (note 1)	Coil	Torso	Torso
Imaging Prameters	Imaging Plane	Axial	Axial
	No. of slices	4	4
	Slice thickness (mm)/gap	10 mm / 0 mm	8 mm / 2 mm
	FOV (mm) / Phase FOV (100%)	420/1 (note 4)	420/1 (note 4)
	Matrix	256 × 64	64 × 64
	TE (msec)	20	58
	TR (msec)	50	1000
	Flip Angle (degree)	30	default (90)
	NEX, EPI shots	1	1, 1shot
	Bandwidth (Hz/Pixel)	288 Hz/pixel	88 Hz/pixel
	Freq Encoding Dir	right - left	right - left
	Acceleration	SENSE (note 1)	SENSE (note 1)
	Acceleration factor	2	2
	No. of breath holds	4 (note 2)	1
	Shimming Volume	Cover the whole body	Cover the whole body
	Spectrum Peaks	Water Peak	Water Peak
	Saturation Band	SI	SI
	scan time	60 s (note 2)	19 sec
Driver Parameters (Generic) (note 5)	Driver Power (%)	50	50
	Driver frequency (Hz)	60	60
	Driver cycles/ trigger (Duration)	3 (auto-caculated)	Auto-calculated

Philips 1.5T - Hepatic MRE Protocols - April 2016 Draft 2			
Scanners and Sequences	Scanner	Ingenia	Ingenia
	Software versions		
	Pulse sequence	**GRE MRE**	**2D SE-EPI MRE**
	Mode	2D	2D
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz) (or Period Mismatch)	60 Hz	60 Hz
	MEG Amplitude (G/cm)	note 3	note 3
	Axis of MEG	4 (Z)	4 (Z)
	Number of phase	4	4
Specific Parameters (To be specified)			

NOTE: (1) Use body coil instead of torso if paitents cannot fit into the bore with the torso coil; if body coil is used then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time and breath-hold time. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (420 mm), even for small patients for consistency. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners.

Philips 3T - Hepatic MRE Protocols - April 2016 Draft 2			
Scanners and Sequences	Scanner	Ingenia	Ingenia
	Software versions		
	Pulse sequence	GRE MRE	2D SE-EPI MRE
	Mode	2D	2D
Patient Cooperation	(1) Patients fast at least 4-6 hours prior to the exams		
	(2) Patients hold breath at the end of expireation during all MRE scans, as well as during scout scans and parallel imaging calibration scans.		
Slice Positing	 Place 4 axial slices at the largest portion of the liver in corol view, and avoid the heart, the liver dome and the liver bottom tip.		
Patient Inforamation Input	Position	feet-first, supine	feet-first, supine
	Weight	Actual Weight	Actual Weight
	Height		
Coil (note 1)	Coil	Torso	Torso
Imaging Prameters	Imaging Plane	Axial	Axial
	No. of slices	4	4
	Slice thickness (mm)/gap	10 mm / 0 mm	8 mm / 2 mm
	FOV (mm) / Phase FOV (100%)	420/1 (note 4)	420/1 (note 4)
	Matrix	256 × 64	64 × 64
	TE (msec)	20	58
	TR (msec)	50	1000
	Flip Angle (degree)	30	default (90)
	NEX, EPI shots	1	1, 1shot
	Bandwidth (Hz/Pixel)	288 Hz/pixel	88 Hz/pixel
	Freq Encoding Dir	right - left	right - left
	Acceleration	SENSE (note 1)	SENSE (note 1)
	Acceleration factor	2	2
	No. of breath holds	4 (note 2)	1
	Shimming Volume	Cover the whole body	Cover the whole body
	Spectrum Peaks	Water Peak	Water Peak
	Saturation Band	SI	SI
	scan time	60 s (note 2)	19 sec
Driver Parameters (Generic) (note 5)	Driver Power (%)	50	50
	Driver frequency (Hz)	60	60
	Driver cycles/ trigger (Duration)	3 (auto-caculated)	Auto-calculated

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Philips 3T - Hepatic MRE Protocols - April 2016 Draft 2			
Scanners and Sequences	Scanner	Ingenia	Ingenia
	Software versions		
	Pulse sequence	**GRE MRE**	**2D SE-EPI MRE**
	Mode	2D	2D
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz) (or Period Mismatch)	60 Hz	60 Hz
	MEG Amplitude (G/cm)	note 3	note 3
	Axis of MEG	4 (Z)	4 (Z)
	Number of phase	4	4
Specific Parameters (To be specified)			

NOTE: (1) Use body coil instead of torso if paitents cannot fit into the bore with the torso coil; if body coil is used then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time and breath-hold time. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (420 mm), even for small patients for consistency. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners.

GE 1.5T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c				
Scanners and Sequences	Scanner	HDx	HDx	MR450w (Tentative)
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	**fgremre (Resoundant-GE)**	**epimre (Resoundant-GE)**	**MR-Touch (GRE)**
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	ASSET, MultiPhase	Fast, ASSET, MultiPhase
Phantom Setup	Place the 16-cm diameter cylinder phantom vertically in the torso coil, place the liver driver (facing down) on the top of the phantom and secure them with the liver MRE elastic belt tightly.			
Slice Positing	Place one coronal slice at the center of the height of the phantom, with a fixed squared FOV (200 mm). 			
Information Input (Pretent Patient)	Position	feet-first, supine	feet-first, supine	feet-first, supine
	Weight	150 Lbs	150 Lbs	150 Lbs
	Height			
Coil (note 1)	Coil	Torso	Torso	Torso
Imaging Prameters	Imaging Plane	coronal	coronal	coronal
	No. of slices	1	1	1
	Slice thickness (mm)/gap	10 mm / 0 mm	8 mm / 2 mm	10 mm / 0 mm
	FOV (mm) / Phase FOV (100%)	20cm/1 (note 4)	20cm/1 (note 4)	20cm/1 (note 4)
	Matrix	256 × 64	64 × 64	256 × 64
	TE (msec)	in-phase TE (about 18.2) (note 7)	min full TE (note 1)	min full TE (type a value colse to 18.2 if possible)
	TR (msec)	50	250	50
	Flip Angle (degree)	25	default (90)	25
	NEX, EPI shots	1	8, 4shot	1
	Bandwidth (kHz)	31.25	250 (hard coded)	31.25
	Freq Encoding Dir	Superior-Inferior	Superior-Inferior	Superior-Inferior
	Phases per Location	4	4	
	Phase Acq. Order	Interleaved	Interleaved	
	Delay After Acq.	Minimum	Minimum	
	Acceleration	ASSET (Note 1)	ASSET (Note 1)	ASSET (Note 1)
	Acceleration factor	1	1	1
	No. of breath holds			

	Shimming Volume	Cover the whole phantom	Cover the whole phantom	Cover the whole phantom
	Spectrum Peaks	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)
	Saturation Band	SI	SI	SI
	scan time	about 28 s (note 2)	about 1 min 13 sec	about 28 sec (note 2)
Driver Parameters (Generic) (note 5)	Driver Power (%)	10	10	10
	Driver frequency (Hz)	60	60	60

GE 1.5T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c				
Scanners and Sequences	Scanner	HDx	HDx	MR450w (Tentative)
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	**fgremre (Resoundant-GE)**	**epimre (Resoundant-GE)**	**MR-Touch (GRE)**
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	ASSET, MultiPhase	Fast, ASSET, MultiPhase
	Driver cycles/ trigger (Duration)	3 (auto-caculated)	Auto-calculated	Auto-caculated
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz) (or Period Mismatch)	75 Hz (0.8)	155	75
	MEG Amplitude (G/cm)	About 3 G/cm with Zoom gradient (75%) (note 3)	Full Scale (note 3)	
	Axis of MEG	4 (Z)	4 (Z)	4 (Z)
User CV or Advanced Table (Specific: epimre -DV16 and DV24) (note 5)	CV0 -Ramp Sampling (1=on, 0=off)		1	
	CV1			
	CV2			
	CV3			
	CV4			
	CV5 -Scale for RF2 Crusher Area		1	
	CV6 -Split MEG (0=L,1/2/3 = L-R in/half/min		2	
	CV7 -Flow Comp. Type for MEG		0	
	CV8 -Driver Frequency Percent Increase		0.5	
	CV9 -Time from Start of MEG1 to MEG2 (-1 = opt, 0=min)		0	
	CV10 -Number of Gradient Pairs		1	
	CV11 -Soft-start Ramp-up Time (sec)		0	
	CV12 -Fraction of Max Gradient Amplitude		1	
	CV13 -Desired MEG Frequency (Hz)		155	
	CV14 -Driver Amp. % (-1 = not V3)		10	
	CV15 -Recon (Def-1912;3D ver =1914;Brain=1915;2D MMDI = 1916)		1916	
	CV16 -Trigger Loc # of Cycles Pre-MEG		4	

	CV17 -MEG Direction (F/P/S=1/2/4, Tetra=8)		4	
	CV18 -Vibration Mode (0=Burst, 1 or 2 = Contin.)		2	
	CV19 - MENC (um per radians)		Don't edit	
	CV20 -# of Motion Periods for Offsets		1	
	CV21 -Frequency of Applied Motion (Hz)		60	
	CV22			
	CV23 -Burst Mode Burst Count		1	
	CV24 -Do High-Resolution Recon.?		1	
	CV 12 -use version3 driver	1		
	CV 13 -Motion Encoding Gradient (MEG) pairs	1		
	CV 14 Motion Frequency - Hz	60		

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GE 1.5T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c				
Scanners and Sequences	Scanner	HDx	HDx	MR450w (Tentative)
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24
	Pulse sequence	**fgremre (Resoundant-GE)**	**epimre (Resoundant-GE)**	**MR-Touch (GRE)**
	Mode	2D, zoom gradient	2D, zoom gradient	2D
	Options	Fast, ASSET, MultiPhase	ASSET, MultiPhase	Fast, ASSET, MultiPhase
User CV (Specific: fgremre DV16) (note 5)	CV 15 Scale Max Gradient Amplitude	0.75		
	CV 17 freq=1, phase=2, slice=4	4		
	CV 21 period mismatch	0.8		
	CV 24 driver amplitude	10		
MR-Touch Tab (Specific fgremre-DV22.1, DV24) (note 5)	Temporal Phases	4		
	MEG Frequency (Hz)	75		
	Driver Amplitude (%) (note 6)	10		
	Driver Cycle Per Trigger	3		
	MEG Direction	4 (Z)		
Advanced Tab (Specific fgremre-DV22.1, DV24) (note 5)	CV12 use resoundant	1.00		
MR-Touch Tab (Specific MR-Touch sequence -DV22.1, DV24) (note 5)	Temporal Phases			4
	MEG Frequency (Hz)			75
	Driver Amplitude (%) (note 6)			10
	Driver Cycle Per Trigger			3
	MEG Direction			4 (Z)

NOTE: (1) Always use torso coil (multi-channel), add pads around the phantom to support the top part of the torsol coil, which should not contact the phantom; if other coils that do not support parallel imaging is used, then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time; however, do not do this for the phantom. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (200 mm), even for this 16-cm diameter cylinder phantom. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters; overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners.(6) Driver Frequencey is 60Hz (default).
(7) FC is not supported with F/W in phase TE, FC should be turned off; if this causes trouble, then Try min full TE.

GE 3T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c					
Scanners and Sequences	Scanner	HDx	HDx	MR750w	3T (MR750W)
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24	DV22.1 and 24
	Pulse sequence	**fgremre (Resoundant-GE)**	**epimre (Resoundant-GE)**	**MR-Touch (EPI) - Clinical Mode**	**MR-Touch (EPI) - Research Mode**
	Mode	2D, zoom gradient	2D, zoom gradient	2D	2D
	Options	Fast, ASSET, MultiPhase	ASSET, MultiPhase	ASSET, FC	ASSET, FC
Phantom Setup	Place the 16-cm diameter cylinder phantom vertically in the torso coil, place the liver driver (facing down) on the top of the phantom and secure them with the liver MRE elastic belt tightly.				
Slice Positing	Place one coronal slice at the center of the height of the phantom, with a fixed squared FOV (200 mm). 				
Information Input (Pretent Patient)	Position	feet-first, supine	feet-first, supine	feet-first, supine	feet-first, supine
	Weight	150 Lbs	150 Lbs	150 Lbs	150 Lbs
	Height				
Coil (note 1)	Coil	Torso	Torso	Torso	Torso
Imaging Prameters	Imaging Plane	coronal	coronal	coronal	coronal
	No. of slices	1	1	1	1
	Slice thickness (mm)/gap	10 mm / 0 mm	8 mm / 2 mm	8 mm / 2 mm	8 mm / 2 mm
	FOV (cm) / Phase FOV (100%)	20cm/1 (note 4)	20cm/1 (note 4)	20cm/1 (note 4)	20cm/1 (note 4)
	Matrix	256 × 64	64 × 64	32 × 32	64 × 64
	TE (msec)	min full (around 15.9, this is close to inphase TE)	min full(around 31 msec) (note 1)	min full(around 57.6 msec) (note 1)	min full (note 1)
	TR (msec)	50	250	250	248 (display CV -> act_tr = 248000)
	Flip Angle (degree)	20	default (90)	default (90)	default (90)
	NEX, EPI shots	1	8, 4shot	1, 1shot	1, 8-shot (display CV -> touch_maxshots = 8))
	Bandwidth (kHz)	31.25	250 (hard coded)	250 (hard coded)	250 (hard coded)
	Freq Encoding Dir	Superior-Inferior	Superior-Inferior	Superior-Inferior	Superior-Inferior
	Phases per Location	4	4		
	Phase Acq. Order	Interleaved	Interleaved		
	Delay After Acq.	Minimum	Minimum		
	Acceleration	ASSET (Note 1)	ASSET (Note 1)	ASSET (Note 1) (Note 2)	ASSET
	Acceleration factor	1	1	2	1
	No. of breath holds				
	Shimming Volume	Cover the whole phantom	Cover the whole phantom	Cover the whole phantom	Cover the whole phantom
	Spectrum Peaks	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)
	Saturation Band				
	scan time	28 s (note 2)	1 min 13 sec	10 sec	24 sec

Driver Parameters (Generic) (note 5)	Driver Power (%)	10	10	10	10
	Driver frequency (Hz)	60	60	60	60
	Driver cycles/ trigger (Duration)	3 (auto-caculated)	Auto-calculated	Auto-calculated	Auto-calculated
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz) (or Period Mismatch)	80 Hz (0.75)	155	90	90
	MEG Amplitude (G/cm)	About 1.7 G/cm with whole gradient (75%) (note 3)	Full Scale (note 3)		
	Axis of MEG	4 (Z)	4 (Z)	4 (Z)	4 (Z)
	CV0 -Ramp Sampling (1=on, 0=off)		1		
	CV1				

GE 3T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c					
Scanners and Sequences	Scanner	HDx	HDx	MR750w	3T (MR750W)
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24	DV22.1 and 24
	Pulse sequence	fgremre (Resoundant-GE)	epimre (Resoundant-GE)	MR-Touch (EPI) - Clinical Mode	MR-Touch (EPI) - Research Mode
	Mode	2D, zoom gradient	2D, zoom gradient	2D	2D
	Options	Fast, ASSET, MultiPhase	ASSET, MultiPhase	ASSET, FC	ASSET, FC
User CV or Advanced Table (Specific: epimre -DV16 and DV24) (note 5)	CV2				
	CV3				
	CV4				
	CV5 -Scale for RF2 Crusher Area		1		
	CV6 -Split MEG (0=L,1/2/3 = L-R in/half/min		2		
	CV7 -Flow Comp. Type for MEG		0		
	CV8 -Driver Frequency Percent Increase		0.5		
	CV9 -Time from Start of MEG1 to MEG2 (-1 = opt, 0=min)		0		
	CV10 -Number of Gradient Pairs		1		
	CV11 -Soft-start Ramp-up Time (sec)		0		
	CV12 -Fraction of Max Gradient Amplitude		1		
	CV13 -Desired MEG Frequency (Hz)		155		
	CV14 -Driver Amp. % (-1 = not V3)		10		
	CV15 -Recon (Def-1912;3D ver =1914;Brain=1915;2D MMDI = 1916)		1916		
	CV16 -Trigger Loc # of Cycles Pre-MEG		4		
	CV17 -MEG Direction (F/P/S=1/2/4, Tetra=8)		4		
	CV18 -Vibration Mode (0=Burst, 1 or 2 = Contin.)		2		
	CV19 - MENC (um per radians)		Don't edit		
	CV20 -# of Motion Periods for Offsets		1		
	CV21 -Frequency of Applied Motion (Hz)		60		
	CV22				
	CV23 -Burst Mode Burst Count		1		
	CV24 -Do High-Resolution Recon.?		1		
User CV (Specific: fgremre - DV16) (note 5)	CV 12 -use version3 driver	1			
	CV 13 -Motion Encoding Gradient (MEG) pairs	1			
	CV 14 Motion Frequency - Hz	60			
	CV 15 Scale Max Gradient Amplitude	0.75			
	CV 17 freq=1, phase=2, slice=4	4			
	CV 21 period mismatch	0.75			
	CV 24 driver amplitude	10			
MR-Touch Tab (Specific fgremre-DV22.1, DV24) (note 5)	Temporal Phases	4			
	MEG Frequency (Hz)	80			
	Driver Amplitude (%) (note 6)	10			
	Driver Cycle Per Trigger	3			
	MEG Direction	4 (Z)			
Advanced Tab (Specific fgremre-DV22.1, DV24) (note 5)	CV12 use resoundant	1.00			
	Temporal Phases			4	4

GE 3T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c					
Scanners and Sequences	Scanner	HDx	HDx	MR750w	3T (MR750W)
	Software versions	DV16 and DV22.1 and 24	DV16 and DV22.1 and 24	DV22.1 and 24	DV22.1 and 24
	Pulse sequence	**fgremre (Resoundant-GE)**	**epimre (Resoundant-GE)**	**MR-Touch (EPI) - Clinical Mode**	**MR-Touch (EPI) - Research Mode**
	Mode	2D, zoom gradient	2D, zoom gradient	2D	2D
	Options	Fast, ASSET, MultiPhase	ASSET, MultiPhase	ASSET, FC	ASSET, FC
MR-Touch Tab (Specific MR-Touch sequence -DV22.1, DV24) (note 5)	MEG Frequency (Hz)			90	90
	Driver frequency (Hz)			60	60
	Driver Amplitude (%)			10	10
	MEG Direction			Z	Z
	Driver Cycle Per Trigger			15 (Not for edit)	15 (Not for edit)
	MENC um/rad			28.5 (Not for edit)	28.5 (Not for edit) (Note 3)

NOTE: (1) Always use torso coil (multi-channel), add pads around the phantom to support the top part of the torsol coil, which should not contact the phantom; if other coils that do not support parallel imaging is used, then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time; however, do not do this for the phantom. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (200 mm), even for this 16-cm diameter cylinder phantom. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters; overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners.(6) Driver Frequencey is 60Hz (default).

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Siemens 1.5T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c			
Scanners and Sequences	Scanner		
	Software versions		
	Pulse sequence	**greMRE**	**epseMRE(WIP)**
	Mode	2D	2D
Phantom Setup	Place the 16-cm diameter cylinder phantom vertically in the torso coil, place the liver driver (facing down) on the top of the phantom and secure them with the liver MRE elastic belt tightly.		
Slice Positing	Place one coronal slice at the center of the height of the phantom, with a fixed squared FOV (200 mm). 		
Information Input (Pretent Patient)	Position	head-first, supine	head-first, supine
	Weight	150 Lbs	150 Lbs
	Height	5 ft	5 ft
Coil (note 1)	Coil	Torso	Torso
Imaging Prameters	Imaging Plane	Coronal	Coronal
	No. of slices	1	1
	Slice thickness (mm)/dist. Factor	10 mm / 0% (0)	8 mm / 25% (2mm)
	FOV (mm) / Phase FOV (100%)	200mm/1 (note 4)	200mm/1 (note 4)
	Matrix (Base × Phase)	256 × 25%(64)	128 × 100%(128)
	TE (msec)	min (about ~20 with flow comp off)	min
	TR (msec)	50	1000

	Flip Angle (degree)	25	default (90)
	NEX, EPI shots	1	1, 1shot
	Bandwidth (Hz/Pixel)	260 Hz/pixel	1502 Hz/pixel
	Phase enc.dir.	Right-Left	Right-Left
	Acceleration	GRAPPA (note 1)	GRAPPA (note 1)
	Acceleration factor	1	1
	No. of breath holds	NA	NA

Siemens 1.5T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c			
Scanners and Sequences	Scanner		
	Software versions		
	Pulse sequence	**greMRE**	**epseMRE(WIP)**
	Mode	2D	2D
	Shimming Volume	auto	auto
	Spectrum Peaks	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)
	Saturation Band		
	scan time	34 sec	11 sec
Driver Parameters (Generic) (note 5)	Driver Power (%)	10 (default) (note 6)	10 (default) (note 6)
	Driver frequency (Hz)	60 (default) (note 6)	60 (default) (note 6)
	Driver cycles/ trigger (Duration)	3 (default) (note 6)	3 (default) (note 6)
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz)	60 Hz (Hard Coded)	60 Hz (Hard Coded)
	MEG Amplitude	(Hard coded)	30 mT/m (Hard coded)
	Axis of MEG	Slice (Hard Coded)	Slice
	Number of phase	4 (Hard coded)	4 (Hard coded)
Specific Parameters (note 5)	Sequence - Part 1 - Flow Comp	NO	YES
	Sequence - Special - MEG Ampltude (mT/m)	Not available	30

	Sequence - Special - MEG Frequency (Hz)	Not available	60.0
	Sequence - Special - MEG Waveform	Not available	1-2-1
	Sequence - Special - MEG Direction	Not available	Slice
	System - Tx/Rx - Img. Scale Cor.	1	1
	Resolution - Filter Image - Prescan Normalize	Check	Check
NOTE: (1) Always use torso coil (multi-channel), add pads around the phantom to support the top part of the torsol coil, which should not contact the phantom; if other coils that do not support parallel imaging is used, then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time; however, do not do this for the phantom. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (200 mm), even for this 16-cm diameter cylinder phantom. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners. (6) The current implementation of Semiens MRE does not access active driver, those values are default values and can be changed by using a seprate web connection to the active driver (Syngo or Laptop); epseMRE sequences delivers one trigger every 50ms.			

Siemens 3T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c			
Scanners and Sequences	Scanner	Skyra	Skyra
	Software versions	VE11A	VE11A
	Pulse sequence	**greMRE**	**epseMRE(WIP)**
	Mode	2D	2D
Phantom Setup	Place the 16-cm diameter cylinder phantom vertically in the torso coil, place the liver driver (facing down) on the top of the phantom and secure them with the liver MRE elastic belt tightly.		
Slice Positing	Place one coronal slice at the center of the height of the phantom, with a fixed squared FOV (200 mm). 		
Information Input (Pretent Patient)	Position	head-first, supine	head-first, supine
	Weight	150 Lbs	150 Lbs
	Height	5 ft	5 ft

Coil (note 1)	Coil	Torso	Torso
Imaging Prameters	Imaging Plane	Coronal	Coronal
	No. of slices	1	1
	Slice thickness (mm)/dist. Factor	10 mm / 0% (0)	8 mm / 25% (2mm)
	FOV (mm) / Phase FOV (100%)	200mm/1 (note 4)	200mm/1 (note 4)
	Matrix (Base × Phase)	256 × 25%(64)	128 × 100%(128)
	TE (msec)	min (about ~20 with flow comp off)	min
	TR (msec)	50	1000
	Flip Angle (degree)	20	default (90)
	NEX, EPI shots	1	1, 1shot
	Bandwidth (Hz/Pixel)	260 Hz/pixel	1502 Hz/pixel
	Phase enc.dir.	Right-Left	Right-Left
	Acceleration	GRAPPA (note 1)	GRAPPA (note 1)
	Acceleration factor	1	1
	No. of breath holds	NA	NA

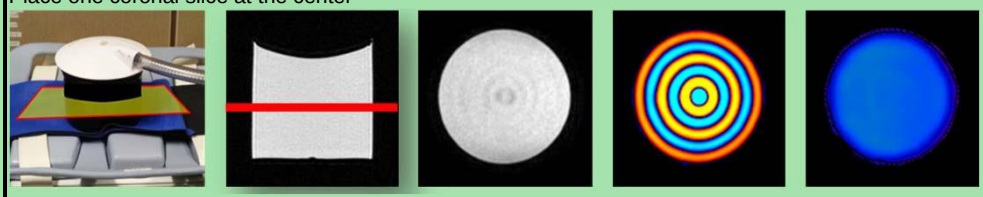
Siemens 3T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c			
Scanners and Sequences	Scanner	Skyra	Skyra
	Software versions	VE11A	VE11A
	Pulse sequence	**greMRE**	**epseMRE(WIP)**
	Mode	2D	2D
	Shimming Volume	auto	auto
	Spectrum Peaks	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)
	Saturation Band		

	scan time	34 sec	11 sec
Driver Parameters (Generic) (note 5)	Driver Power (%)	10 (default) (note 6)	10 (default) (note 6)
	Driver frequency (Hz)	60 (default) (note 6)	60 (default) (note 6)
	Driver cycles/ trigger (Duration)	3 (default) (note 6)	3 (default) (note 6)
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz)	60 Hz (Hard Coded)	60 Hz (Hard Coded)
	MEG Amplitude	(Hard coded)	30 mT/m (Hard coded)
	Axis of MEG	Slice (Hard Coded)	Slice
	Number of phase	4 (Hard coded)	4 (Hard coded)
Specific Parameters (note 5)	Sequence - Part 1 - Flow Comp	NO	YES
	Sequence - Special - MEG Ampltude (mT/m)	Not available	30
	Sequence - Special - MEG Frequency (Hz)	Not available	60.0
	Sequence - Special - MEG Waveform	Not available	1-2-1
	Sequence - Special - MEG Direction	Not available	Slice
	System - Tx/Rx - Img. Scale Cor.	1	1
	Resolution - Filter Image - Prescan Normalize	Check	Check

NOTE: (1) Always use torso coil (multi-channel), add pads around the phantom to support the top part of the torsol coil, which should not contact the phantom; if other coils that do not support parallel imaging is used, then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time; however, do not do this for the phantom. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (200 mm), even for this 16-cm diameter cylinder phantom. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners. (6) The current implementation of Semiens MRE does not access active driver, those values are default values and can be changed by using a seprate web connection to the active driver (Syngo or Laptop); epseMRE sequences delivers one trigger every 50ms.

Philips 1.5T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c

Scanners and Sequences	Scanner	Ingenia	Ingenia
	Software versions		
	Pulse sequence	**GRE MRE**	**2D SE-EPI MRE**
	Mode	2D	2D

Phantom Setup	Place the 16-cm diameter cylinder phantom vertically in the torso coil, place the liver driver (facing down) on the top of the phantom and secure them with the liver MRE elastic belt tightly.		
Slice Positing	Place one coronal slice at the center  of the height of the phantom, with a fixed squared FOV (200 mm).		
Information Input (Pretent Patient)	Position	feet-first, supine	feet-first, supine
	Weight	150 Lbs	150 Lbs
	Height		
Coil (note 1)	Coil	Torso	Torso
Imaging Prameters	Imaging Plane	Coronal	Coronal
	No. of slices	1	1
	Slice thickness (mm)/gap	10 mm / 0 mm	8 mm / 2 mm
	FOV (mm) / Phase FOV (100%)	200/1 (note 4)	200/1 (note 4)
	Matrix	256 × 64	64 × 64
	TE (msec)	min or 20	min or 58
	TR (msec)	50	1000
	Flip Angle (degree)	25	default (90)
	NEX, EPI shots	1	1, 1shot
	Bandwidth (Hz/Pixel)	288 Hz/pixel	88 Hz/pixel
	Freq Encoding Dir	Superior-Inferior	Superior-Inferior
	Acceleration	SENSE (note 1)	SENSE (note 1)
	Acceleration factor	1	1

	No. of breath holds	4 (note 2)	1

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Philips 1.5T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c			
Scanners and Sequences	Scanner	Ingenia	Ingenia
	Software versions		
	Pulse sequence	**GRE MRE**	**2D SE-EPI MRE**
	Mode	2D	2D
	Shimming Volume	Cover the whole body	Cover the whole body
	Spectrum Peaks	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)
	Saturation Band		
	scan time	30 s (note 2)	19 sec
Driver Parameters (Generic) (note 5)	Driver Power (%)	50	50
	Driver frequency (Hz)	60	60
	Driver cycles/ trigger (Duration)	3 (auto-caculated)	Auto-calculated
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz) (or Period Mismatch)	60 Hz	60 Hz
	MEG Amplitude (G/cm)	note 3	note 3
	Axis of MEG	4 (Z)	4 (Z)
	Number of phase	4	4
Specific Parameters (To be specified)			
NOTE: (1) Always use torso coil (multi-channel), add pads around the phantom to support the top part of the torsol coil, which should not contact the phantom; if other coils that do not support parallel imaging is used, then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time; however, do not do this for the phantom. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (200 mm), even for this 16-cm diameter cylinder phantom. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners.			

Philips 3T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c			
Scanners and Sequences	Scanner	Ingenia	Ingenia

	Software versions		
	Pulse sequence	**GRE MRE**	**2D SE-EPI MRE**
	Mode	2D	2D
Phantom Setup	Place the 16-cm diameter cylinder phantom vertically in the torso coil, place the liver driver (facing down) on the top of the phantom and secure them with the liver MRE elastic belt tightly.		
Slice Positing	Place one coronal slice at the center of the height of the phantom, with a fixed squared FOV (200 mm). 		
Information Input (Pretent Patient)	Position	feet-first, supine	feet-first, supine
	Weight	150 Lbs	150 Lbs
	Height		
Coil (note 1)	Coil	Torso	Torso
Imaging Prameters	Imaging Plane	Coronal	Coronal
	No. of slices	1	1
	Slice thickness (mm)/gap	10 mm / 0 mm	8 mm / 2 mm
	FOV (mm) / Phase FOV (100%)	400/1 (note 4)	200/1 (note 4)
	Matrix	256 × 64	64 × 64
	TE (msec)	min or 20	min or 58
	TR (msec)	50	1000
	Flip Angle (degree)	20	default (90)
	NEX, EPI shots	1	1, 1shot
	Bandwidth (Hz/Pixel)	288 Hz/pixel	88 Hz/pixel

	Freq Encoding Dir	Superior-Inferior	Superior-Inferior
	Acceleration	SENSE (note 1)	SENSE (note 1)
	Acceleration factor	1	1
	No. of breath holds	4 (note 2)	1

Philips 3T - Phantom 2DMRE Parameter Recommendations - Sep 2016 Draft 1c			
Scanners and Sequences	Scanner	Ingenia	Ingenia
	Software versions		
	Pulse sequence	**GRE MRE**	**2D SE-EPI MRE**
	Mode	2D	2D
	Shimming Volume	Cover the whole phantom	Cover the whole phantom
	Spectrum Peaks	Peak with middle freq (there are 3 peaks)	Peak with middle freq (there are 3 peaks)
	Saturation Band		
	scan time	30 s (note 2)	19 sec
Driver Parameters (Generic) (note 5)	Driver Power (%)	10	10
	Driver frequency (Hz)	60	60
	Driver cycles/ trigger (Duration)	3 (auto-caculated)	Auto-calculated
Motion Encoding Gradients (Generic) (note 5)	MEG frequency (Hz) (or Period Mismatch)	60 Hz	60 Hz
	MEG Amplitude (G/cm)	note 3	note 3
	Axis of MEG	4 (Z)	4 (Z)
	Number of phase	4	4
Specific Parameters (To be specified)			

NOTE: (1) Always use torso coil (multi-channel), add pads around the phantom to support the top part of the torsol coil, which should not contact the phantom; if other coils that do not support parallel imaging is used, then the ASSET is turned off automatically, scan time is longer. (2) For GREMRE, scan time can vary depending on the FOV (in phase dir) setup - decreasing phase FOV can slightly decrease scan time; however, do not do this for the phantom. (3) Depending on your gradient hardware peformance, the absolute gradient strenth could be differnet. (4) FOV is recommendated to be a fixed value (200 mm), even for this 16-cm diameter cylinder phantom. (5) The specific tab and parameters can be different for different software versions and MRE sequences; the generic MRE parameters for driver and motion encoding gradients are the guidline to those specific tab and parameters (MRE-related); overall, this recommendation is conservative so that it can be successfully performmed at all software versions and scanners.

Appendix E: Sample Phantom QA Protocol

This activity describes MRE system Quality Assurance (QA) method using MRE QA phantoms, including the phantom setup, phantom imaging parameters and region of interest (ROI) for measuring phantom stiffness, as well as a QA schedule and pass criteria.

QA PHANTOM

The MRE system QA phantom is made of Polyvinyl Chloride (PVC) in a 12.5cm × Ø15.5cm cylinder container with 0.15 cm wall thickness. It should be handled carefully when being transferred from on location to another to avoid dropping.

Figure 1. MRE QA Phantom

PHANTOM SETUP:

The MRE system QA phantoms setup uses the patient liver MRE driver, the patient elastic belt, a phantom specific friction cloth, and the patient torso RF coil. There are 10 steps for a typical QA phantom setup; the goal of the setup is to make sure the phantom is sitting on the table vertically and stably:

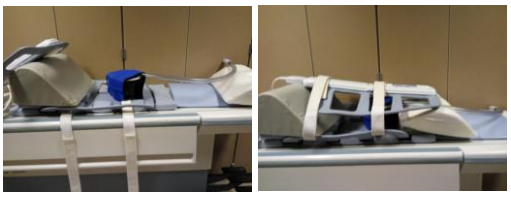
Figure 2. MRE QA Phantom Setup

1) **Position the bottom part of the patient torso coil on the patient table**
2) **Put the patient elastic belt on the bottom coil**
3) **Put the MRE standard phantom on the elastic belt vertically**
4) **Put the friction cloth on the top of the phantom**
5) **Put the patient liver driver on the friction cloth**
6) **Wrap the phantom, friction cloth and driver with the elastic belt tightly**
7) **Put some cushions around the MRE Phantom to support the top part of the torso coil, which should not contact the phantom**
8) **Put the top part of the torso coil on the cushions**
9) **Connect the liver driver to the tube of MRE active driver**
10) **Advance to scan**

PHANTOM IMAGING PARAMETERS

Patient MRE sequences are used for the MRE system QA, but with different imaging parameters. Phantom imaging parameters have been optimized according to its T1 and T2 relaxation time, chemical spectrum and geometry, which are very different from the patients. Detailed parameters for GRE MRE and EPI MRE sequences at both 1.5-T and 3-T platforms of the three vendors (GE, Siemens and Philips) are attached (Phantom 2DMRE Parameters - Hepatic Driver - Sept 2016 Draft 1c.pdf).

REGION OF INTEREST (ROI) FOR MEASURING PHANTOM STIFFNESS

Position a circular ROI in the middle of the phantom with half of the phantom diameter on the elastogram (with or without confidence mask). A high quality phantom exam should have the majority of phantom uncovered with the confidence mask. Phantom edges should be avoided from the ROI due to the edge effect. Mean and standard deviation of the pixel values in the ROI are reported as the

phantom stiffness (in the unit of Pa or kPa).

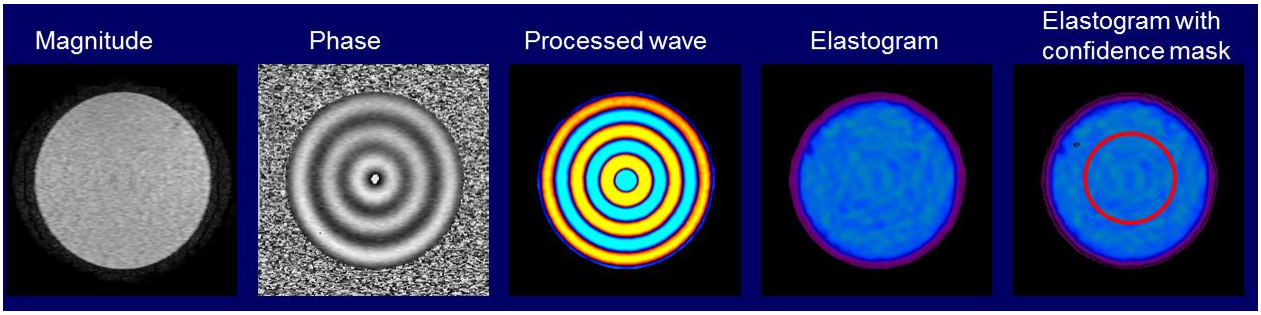

Figure 3. ROI for measuring phantom stiffness (mean ± sd, Pa or kPa)

QA SCHEDULE AND PASS CRITERIA

The MRE system QA phantom exams should be scheduled on site every six months. The current mean stiffness measurement (E_current) of the phantom should be compared to the average of the current and the previous measurement (E_previous); measurement difference = 2 × abs (E_current-E_previous)/(E_current + E_previous). Pass criteria for the current exam: measurement difference ≤ 10%.

Table 1: MRE QA Schedule and Criteria

Date	Phantom Mean Stiffness (kPa)	Phantom SD Stiffness (kPa)	Stiffness Measurement Difference	Pass Criteria (Expected Stiffness Measurement Difference)
First Scan	E0	SD0	NA	NA
6 months	E1	SD1	2 × abs (E1-E0)/(E1+E0)	≤ 10%
Next 6 months	E2	SD2	2 × abs (E2-E1)/(E2+E1)	≤ 10%
⋮	⋮	⋮	⋮	⋮

1. Ellis EL, Mann DA. Clinical evidence for the regression of liver fibrosis. Journal of Hepatology. 2012;56(5):1171-80.

2. Snowdon VK, Fallowfield JA. Models and mechanisms of fibrosis resolution. Alcohol Clin Exp Res. 2011;35(5):794-9.

3. Yin M, Glaser KJ, Talwalkar JA, Chen J, Manduca A, Ehman RL. Hepatic MR Elastography: Clinical Performance in a Series of 1377 Consecutive Examinations. Radiology. 2016;278(1):114-24.

4. Yin M, Woollard J, Wang X, et al. Quantitative assessment of hepatic fibrosis in an animal

model with magnetic resonance elastography. Magn Reson Med. 2007;58(2):346-53.

5. Shire NJ, Yin M, Chen J, et al. Test-retest repeatability of MR elastography for noninvasive liver fibrosis assessment in Hepatitis C. Journal of Magnetic Resonance Imaging. 2011;34:947-55.

6. Yasar TK, Wagner M, Bane O, et al. Interplatform reproducibility of liver and spleen stiffness measured with MR elastography. J Magn Reson Imaging. 2016;43(5):1064-72.

7. Hines CDG, Bley TA, Lindstrom MJ, Reeder SB. Repeatability of magnetic resonance elastography for quantification of hepatic stiffness. Journal of Magnetic Resonance Imaging. 2010;31:725-31.

8. Repeatability of Magnetic Resonance Elastography of Liver - A Meta-Analysis. Radiology (In Review).

9. Arunachalam SP, Rossman PJ, Arani A, et al. Quantitative 3D magnetic resonance elastography: Comparison with dynamic mechanical analysis. Magnet Reson Med. 2016.

10. Chen Q, Ringleb SI, Hulshizer T, An KN. Identification of the testing parameters in high frequency dynamic shear measurement on agarose gels. J Biomech. 2005;38(4):959-63.

11. Okamoto RJ, Clayton EH, Bayly PV. Viscoelastic properties of soft gels: comparison of magnetic resonance elastography and dynamic shear testing in the shear wave regime. Phys Med Biol. 2011;56(19):6379-400.

12. Sahebjavaher RS, Nir G, Gagnon LO, et al. MR elastography and diffusion-weighted imaging of ex vivo prostate cancer: quantitative comparison to histopathology. NMR Biomed. 2015;28(1):89-100.

13. Samani A, Zubovits J, Plewes D. Elastic moduli of normal and pathological human breast tissues: an inversion-technique-based investigation of 169 samples. Phys Med Biol. 2007;52(6):1565-76.

14. Mederacke I, Wursthorn K, Kirschner J, et al. Food intake increases liver stiffness in patients with chronic or resolved hepatitis C virus infection. Liver Int. 2009;29(10):1500-6.

15. Yin M, Talwalkar JA, Glaser KJ, et al. Dynamic postprandial hepatic stiffness augmentation assessed with MR elastography in patients with chronic liver disease. American Journal of Roentgenology. 2011;197:64-70.

16. Venkatesh SK, Ehman RL. Magnetic Resonance Elastography of Abdomen. Abdom Imaging. 2015;40(4):745-59.

17. Venkatesh SK, Yin M, Ehman RL. Magnetic resonance elastography of liver: technique, analysis, and clinical applications. J Magn Reson Imaging. 2013;37(3):544-55.

18. Dzyubak B, Venkatesh SK, Manduca A, Glaser KJ, Ehman RL. Automated liver elasticity calculation for MR elastography. Journal of Magnetic Resonance Imaging. 2016;43(5):1055-63.